Physics 1

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Resonance



Resonance











Impart energy





Impart energy

EM radiation at Larmor





Impart energy

EM radiation at Larmor

63 MHz - radio waves





Impart energy

EM radiation at Larmor

63 MHz - radio waves

Why is this useful





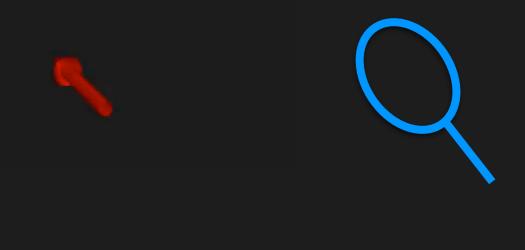


Impart energy

EM radiation at Larmor

63 MHz - radio waves

Why is this useful



Induces current in antenna



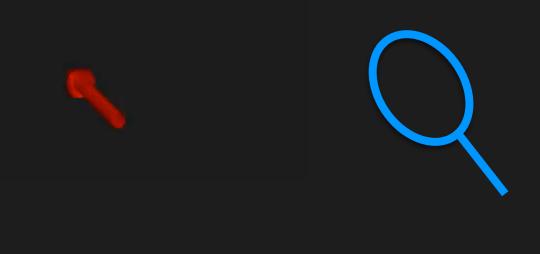


Impart energy

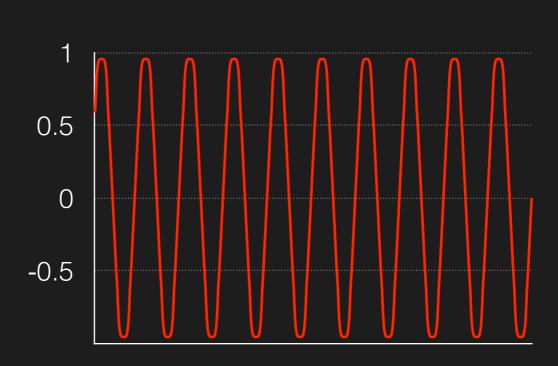
EM radiation at Larmor

63 MHz - radio waves

Why is this useful



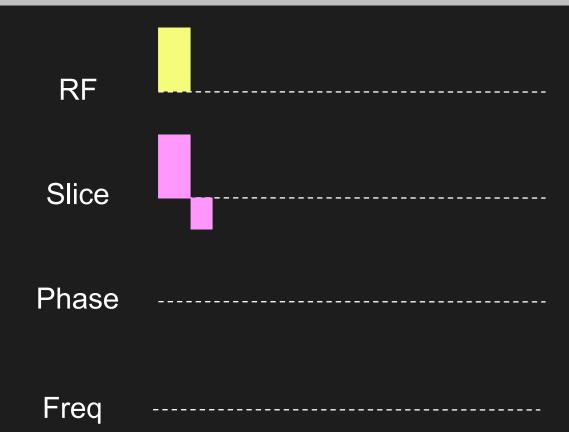
Induces current in antenna





RF	
Slice	
Phase	
Freq	









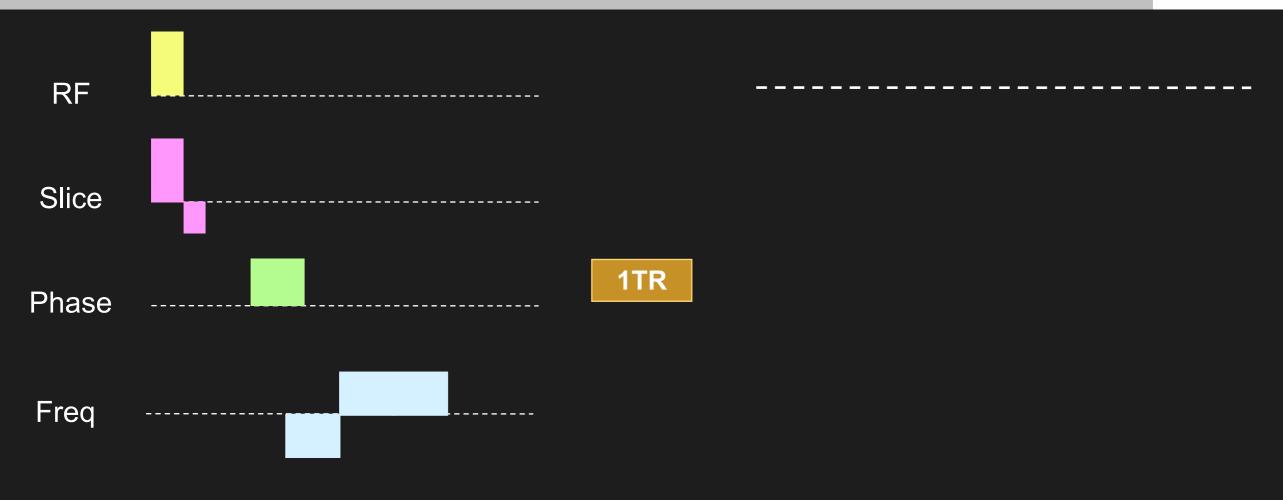




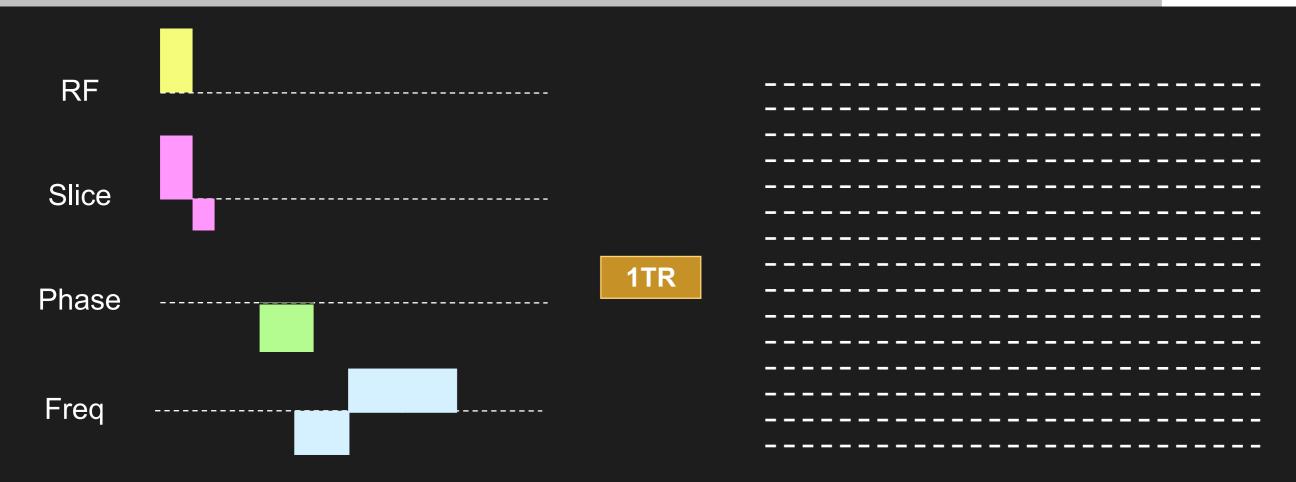




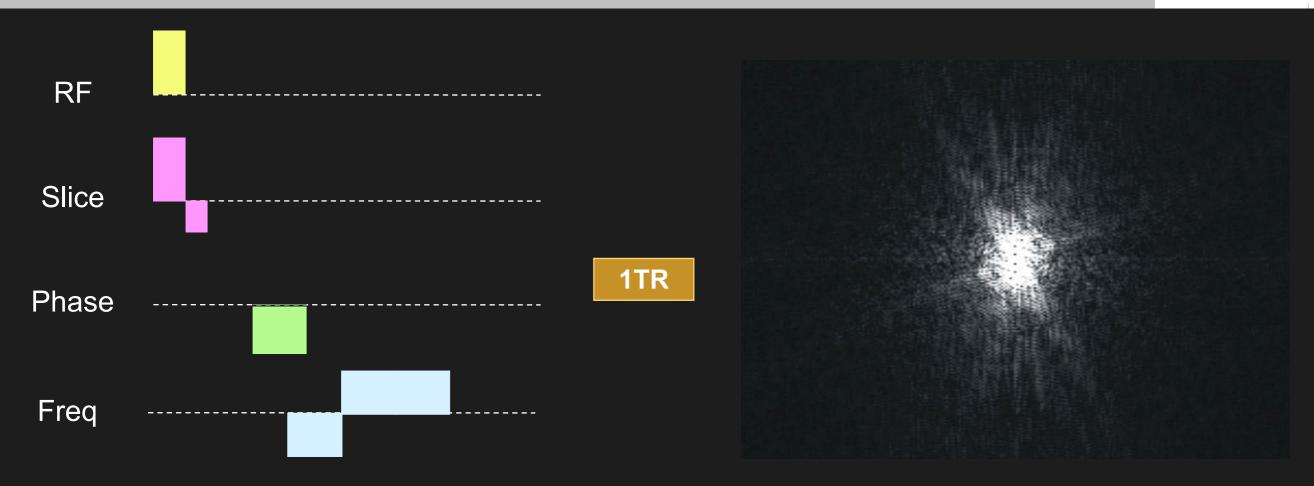




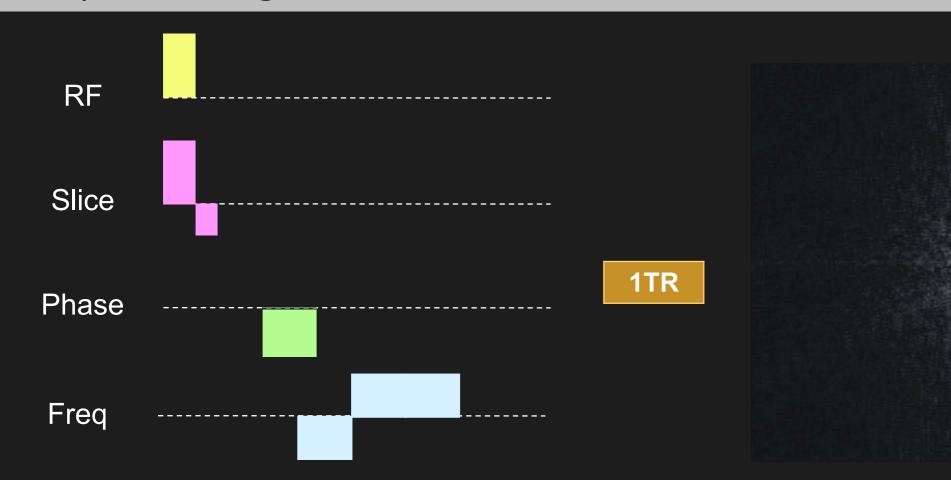


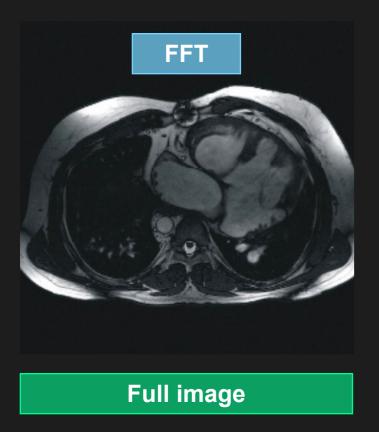




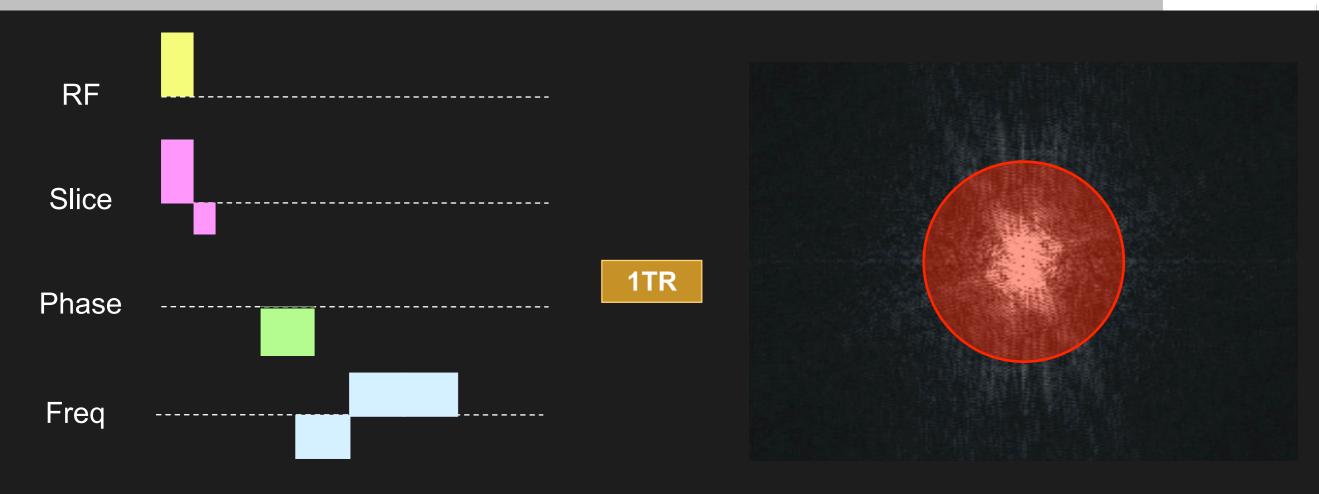


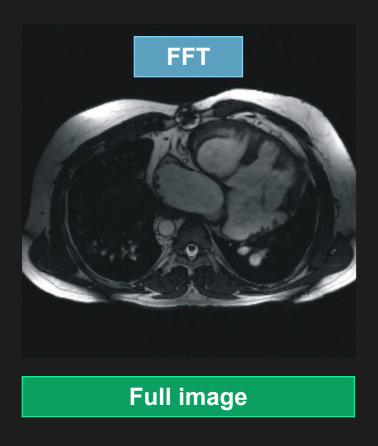




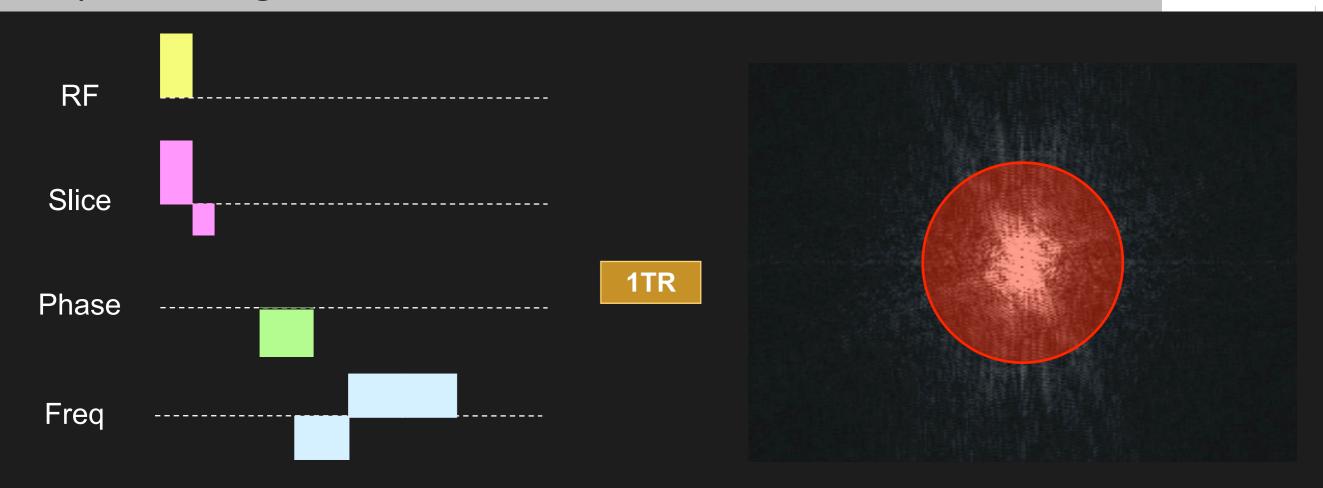


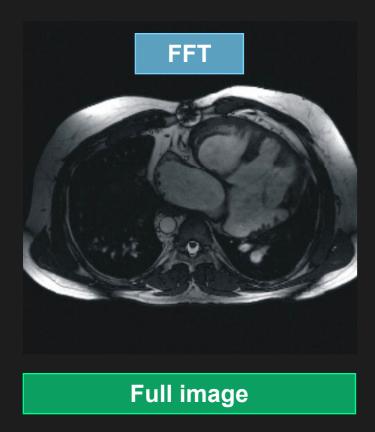


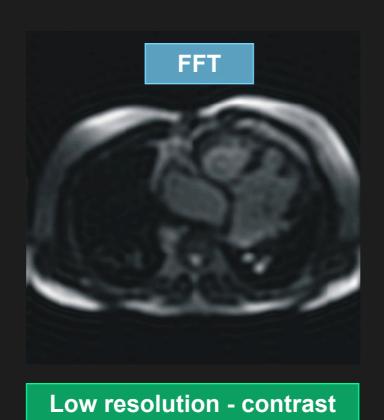




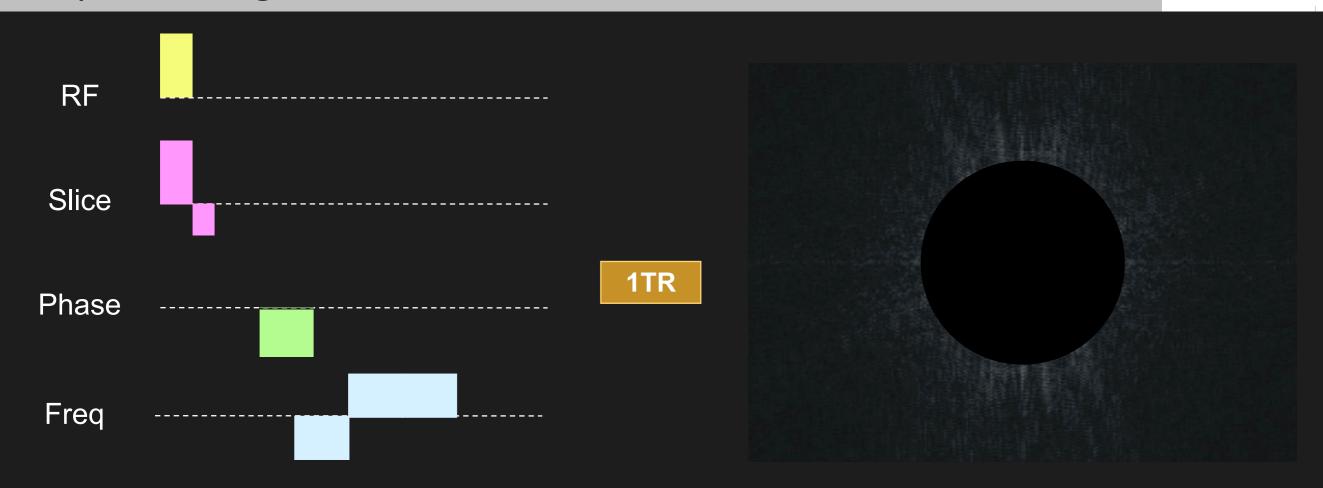


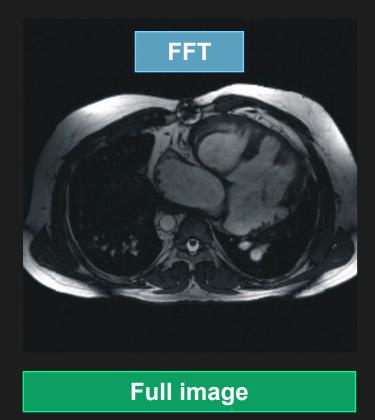


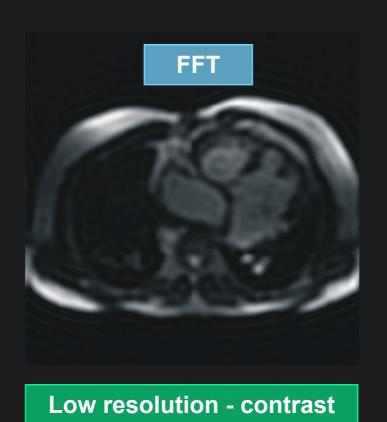




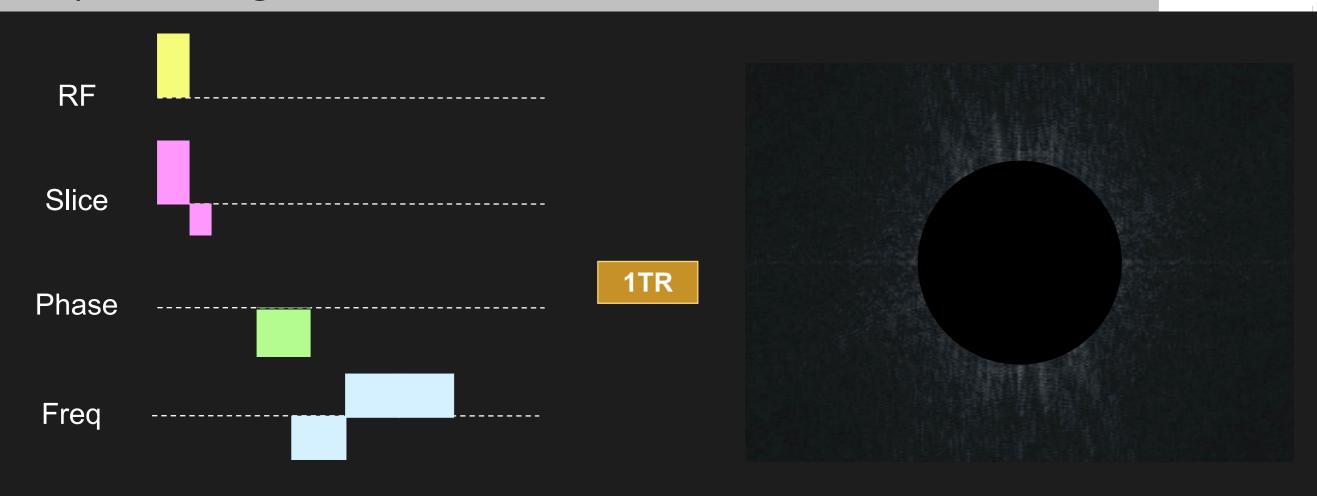


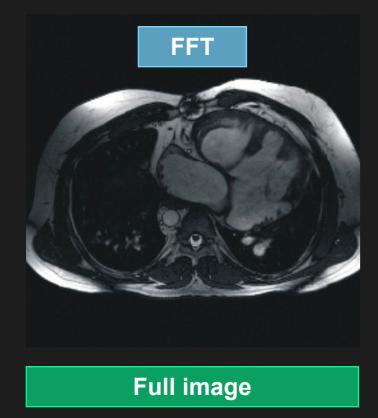






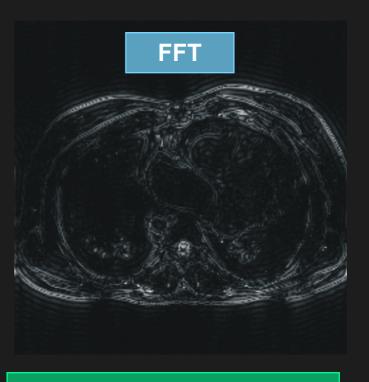








FFT

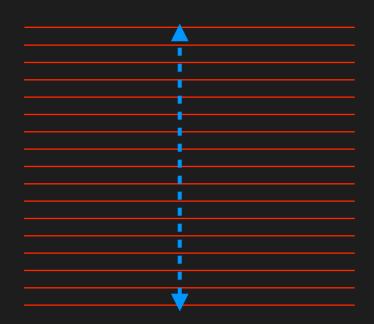


High resolution - edges









Resolution - size of K-space



Resolution - size of K-space

Increase line spacing





Resolution - size of K-space

Increase line spacing







Resolution - size of K-space

Increase line spacing



Resolution - size of K-space

Increase line spacing



Resolution - size of K-space

Increase line spacing



Resolution - size of K-space

Increase line spacing



Larger gradient more dephasing

Resolution - size of K-space

Increase line spacing



Larger gradient more dephasing

Resolution - size of K-space

Increase line spacing



Larger gradient more dephasing Limited by aliasing - 360 phase **Resolution - size of K-space**

Increase line spacing



Resolution - size of K-space

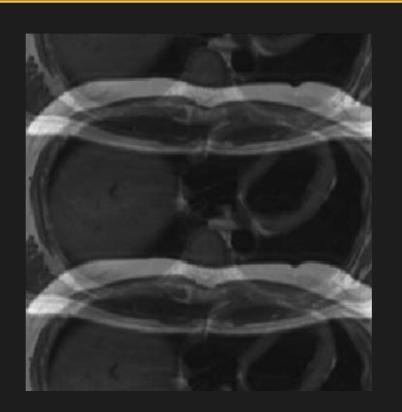
Increase line spacing

How do we do that?



Larger gradient more dephasing

Limited by aliasing - 360 phase



Resolution - FOV



Resolution - size of K-space

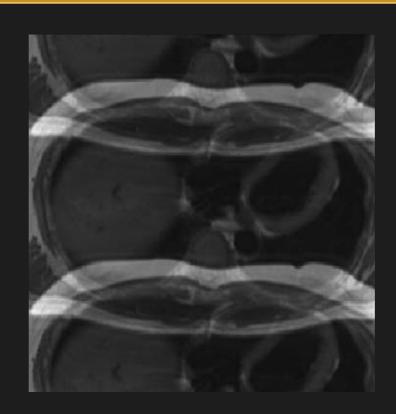
Increase line spacing

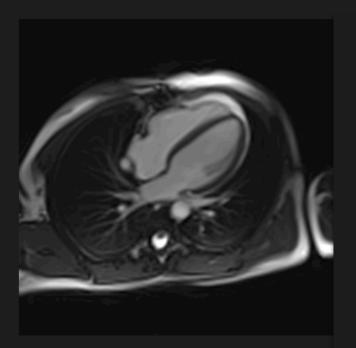
How do we do that?



Larger gradient more dephasing

Limited by aliasing - 360 phase

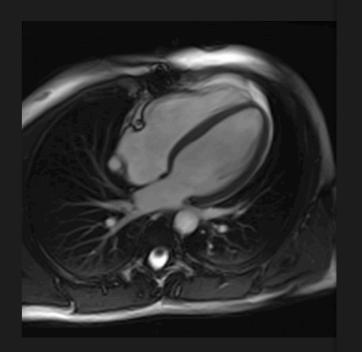




FOV = 500mm

Matrix = 176*176

Scan time = 15s



FOV = 300mm

Matrix = 176*176

Scan time = 15s







Resolution - size of K-space



Resolution - size of K-space

Increase number of lines



Resolution - size of K-space

Increase number of lines

How do we do that?



Increase matrix

Resolution - size of K-space

Increase number of lines

How do we do that?



Increase matrix

Increased time

Resolution - size of K-space

Increase number of lines

How do we do that?



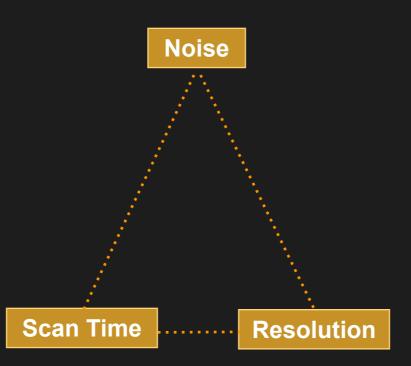
Resolution - size of K-space

Increase number of lines

How do we do that?

Increase matrix

Increased time





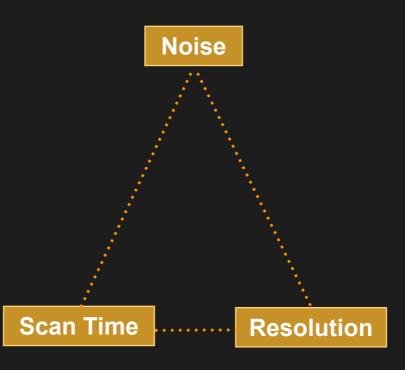
Resolution - size of K-space

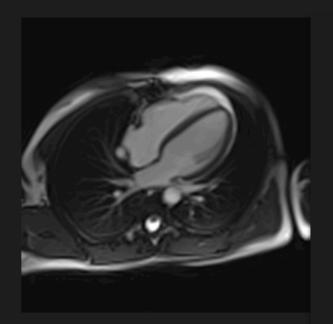
Increase number of lines

How do we do that?

Increase matrix

Increased time





FOV = 500mm Matrix = 176*176 Scan time = 15s



FOV = 500mm Matrix = 240*240Scan time = 20s

Resolution - RFOV



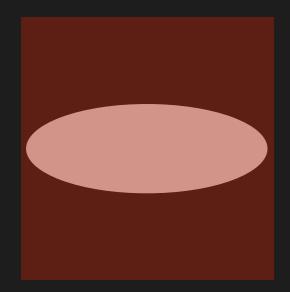
Resolution - RFOV



Resolution - RFOV





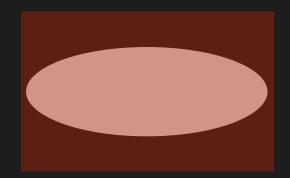






Smaller FOV - PE direction

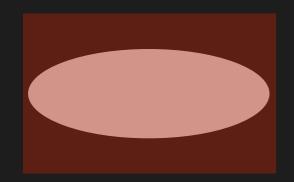




Smaller FOV - PE direction

Increase resolution



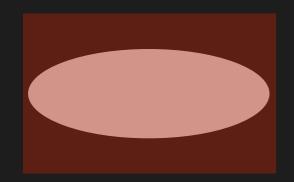


Smaller FOV - PE direction

Increase resolution

Lose lines





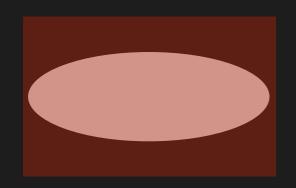
Smaller FOV - PE direction

Increase resolution

Lose lines

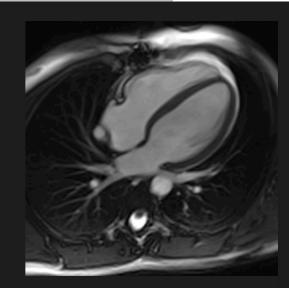
Same resolution





Smaller FOV - PE direction

Increase resolution



FOV = 350mm

Matrix = 192*192

Scan time = 16s

Lose lines

Same resolution

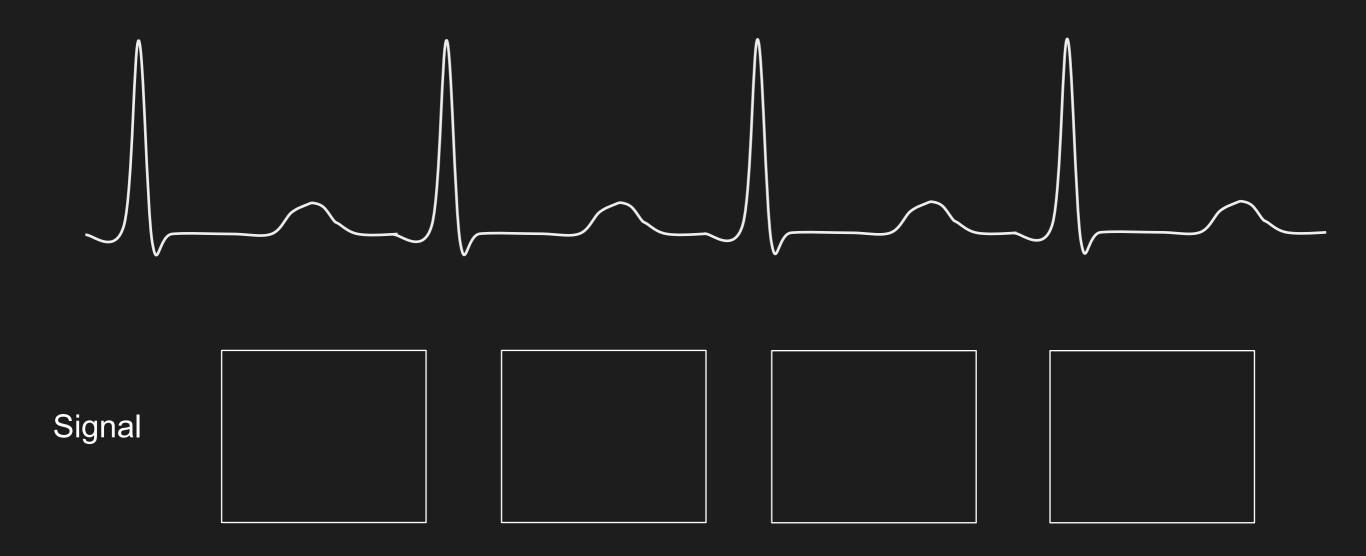
Shorter time - loss of SNR



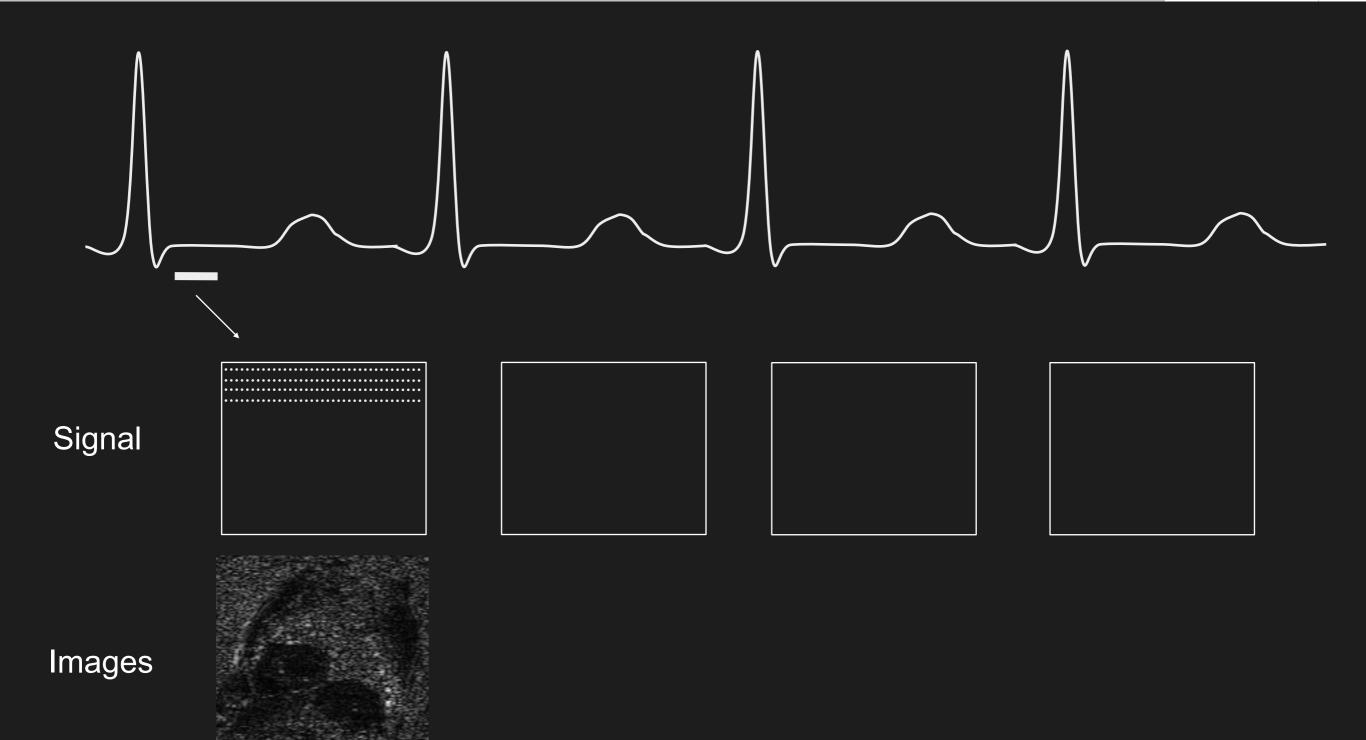
FOV = 350mm

Matrix = 144*192

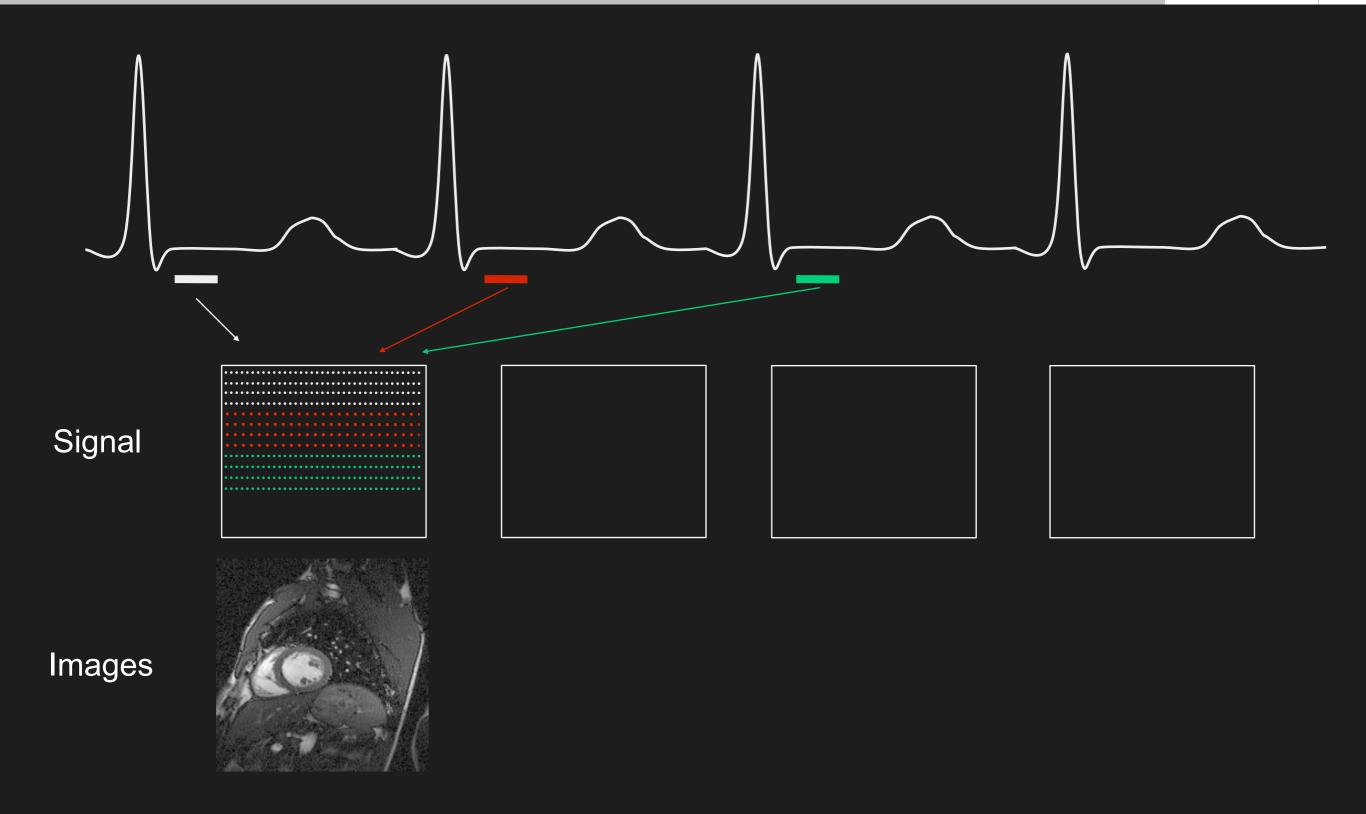
Scan time = 12s

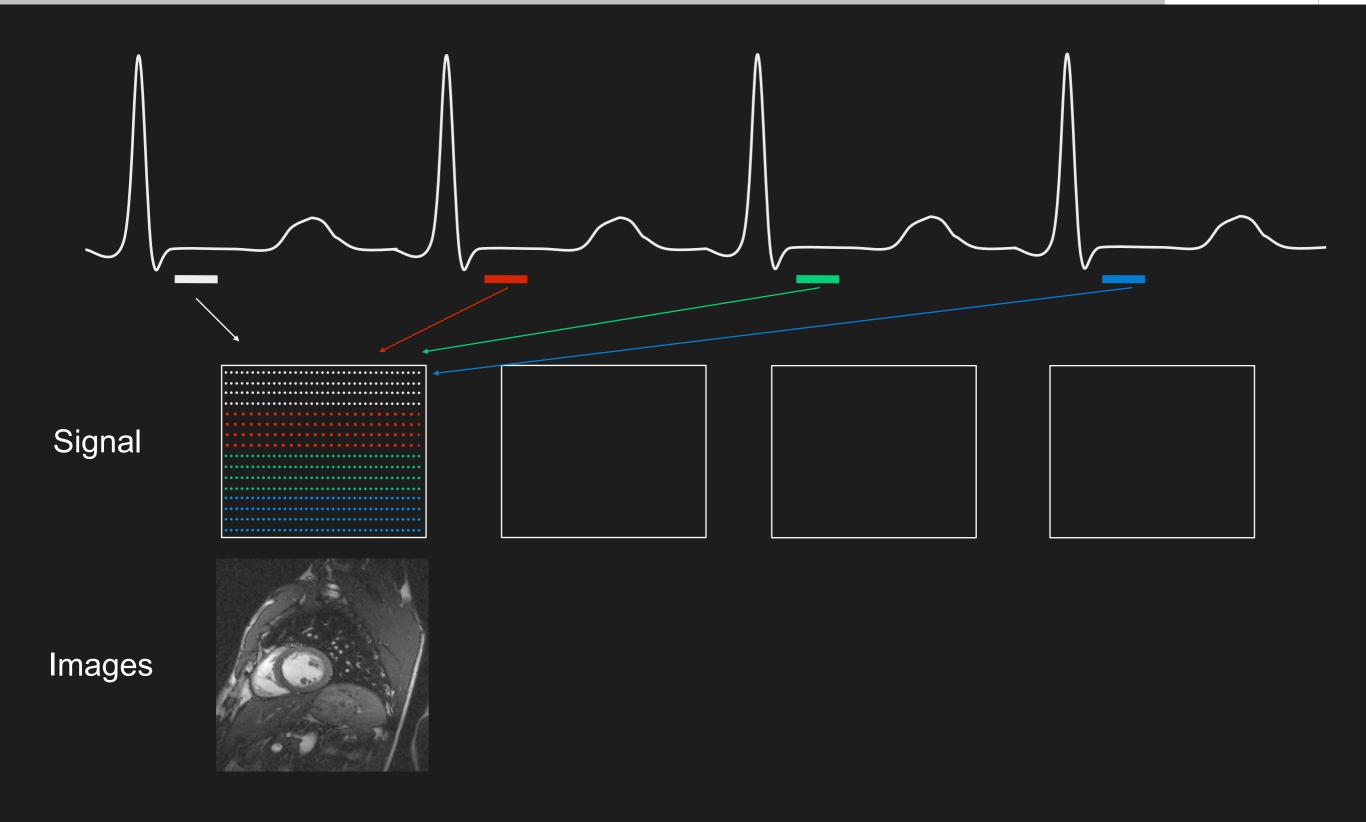


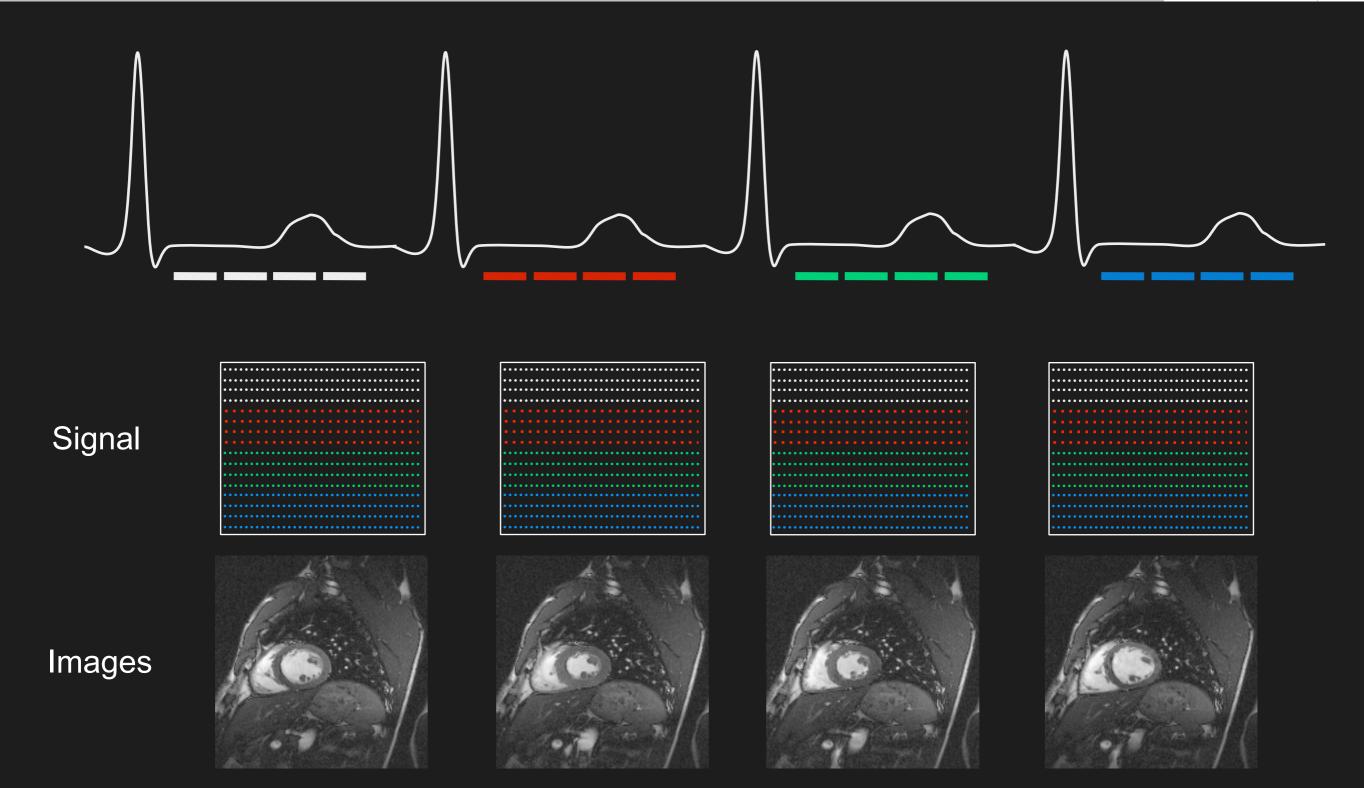
Images





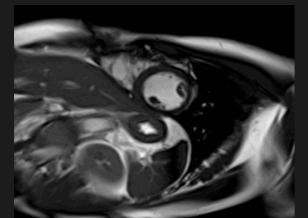


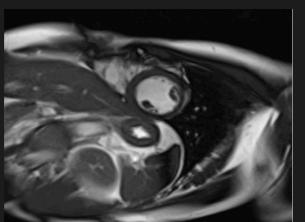


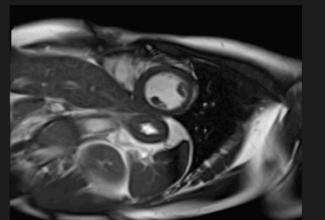


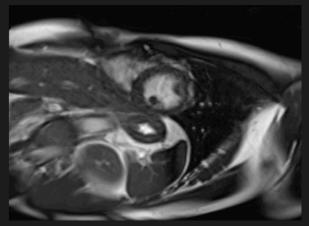


100 fps 50 fps 10 fps 5 fps



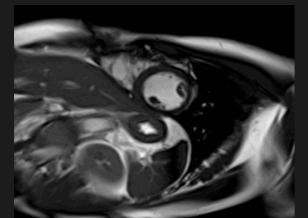


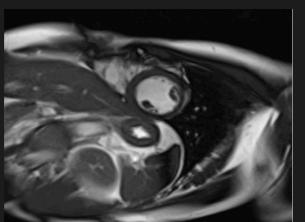


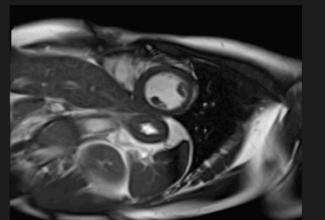


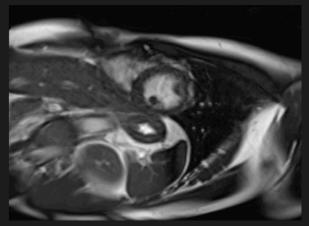


100 fps 50 fps 10 fps 5 fps

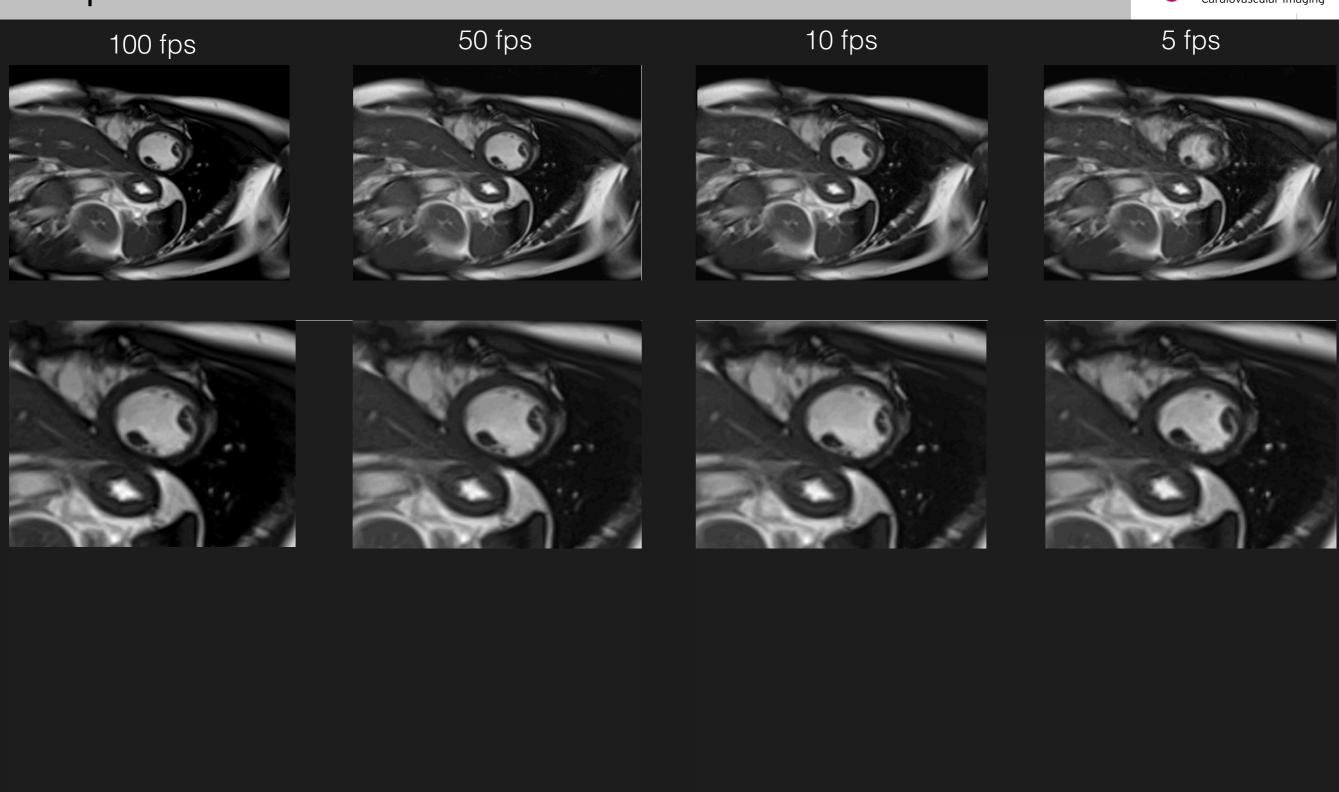




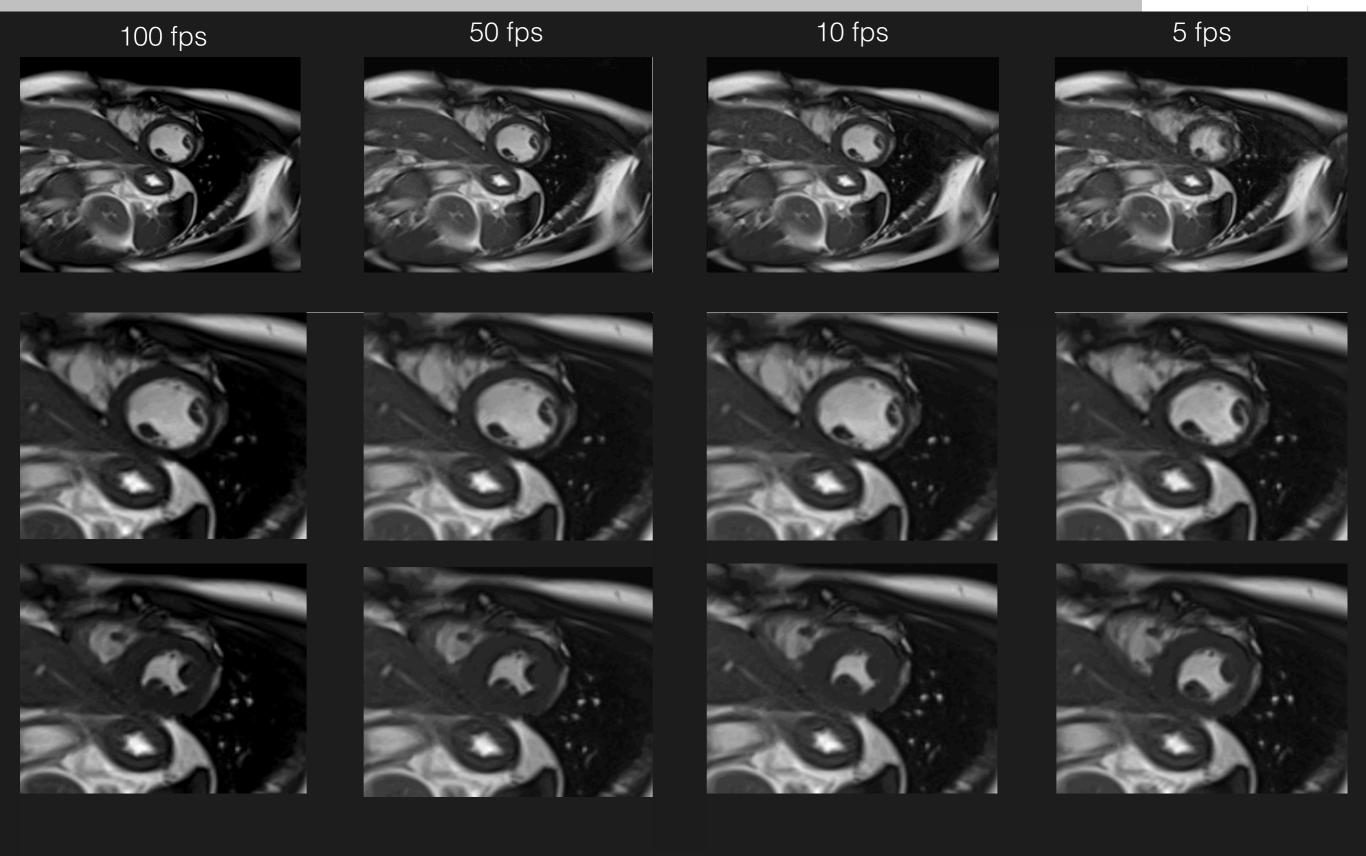




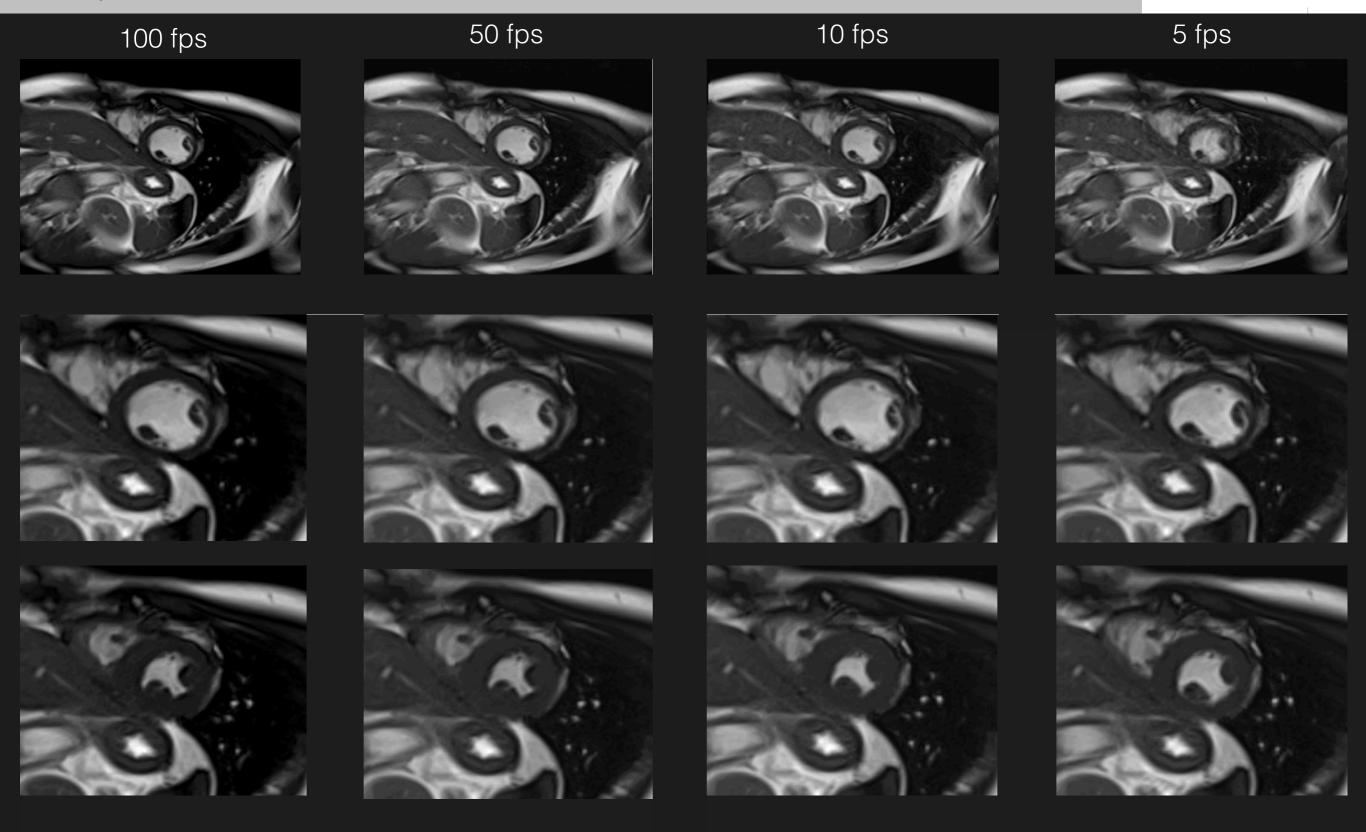






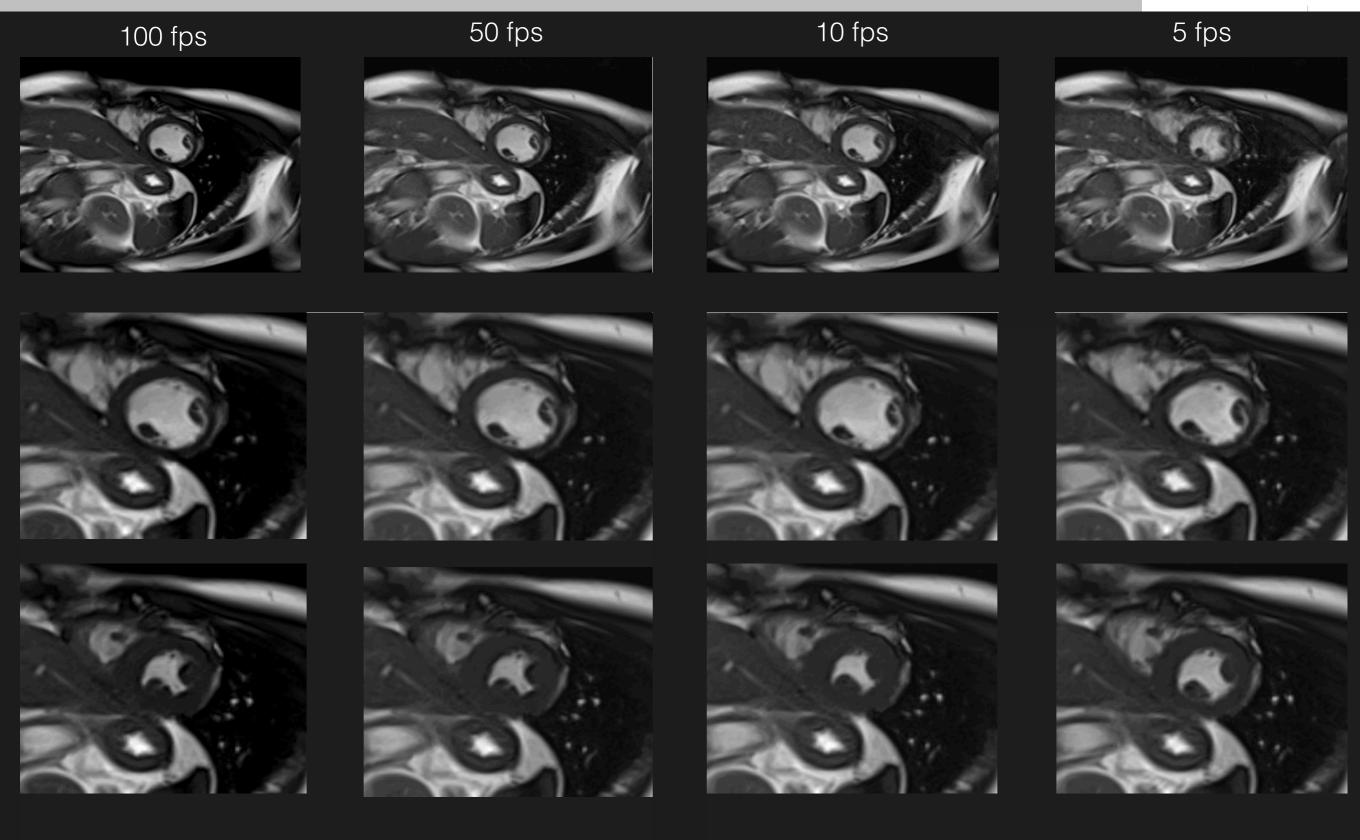






Overestimate ESV

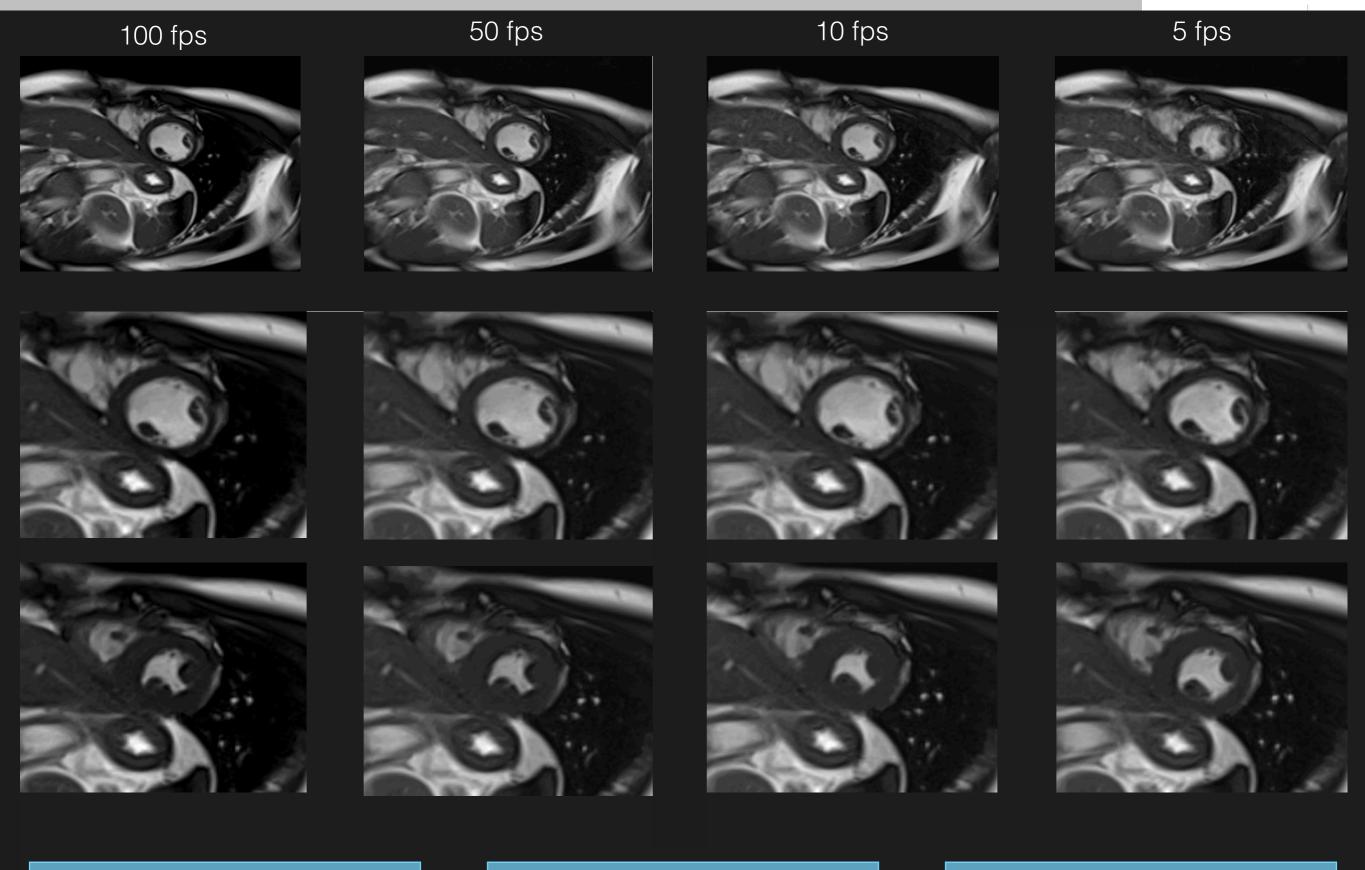




Overestimate ESV

Underestimate EF





Overestimate ESV

Underestimate EF

20-30 true phases





TR = 3ms



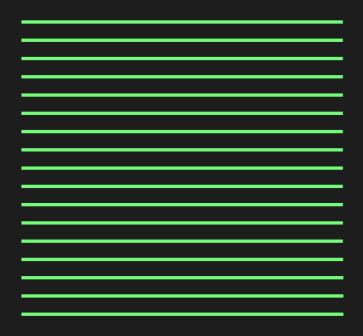
TR = 3ms

NoPE = 200









Temporal resolution

TR = 3ms

NoPE = 200

LPS = 10

HR = **75bpm**



Temporal resolution

TR * LPS



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75bpm**



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75**bpm

No of segments/ beats



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75**bpm

No of segments/ beats NoPE/ LPS



Temporal resolution

beats

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75bpm**

No of segments/

NoPE/ LPS

20 beats



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75bpm**

No of segments/ beats NoPE/ LPS

20 beats

Breath hold time



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75bpm**

No of segments/ beats NoPE/ LPS

20 beats

Breath hold time

Beats * RR int



Temporal resolution

TR * LPS

30ms

TR = 3ms

NoPE = 200

LPS = 10

HR = **75**bpm

No of segments/ beats NoPE/ LPS

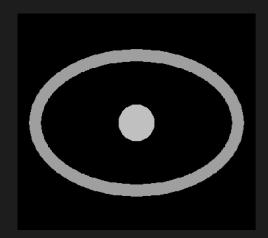
20 beats

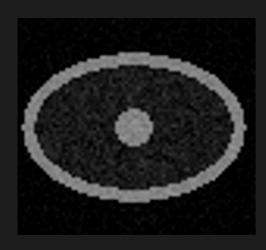
Breath hold time

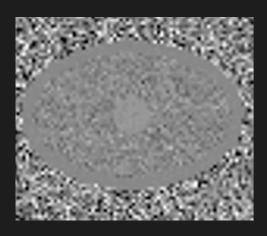
Beats * RR int

16s

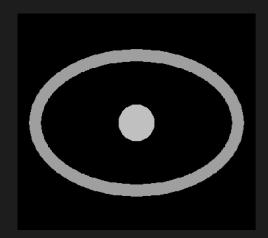


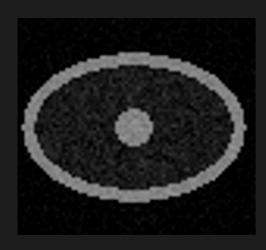


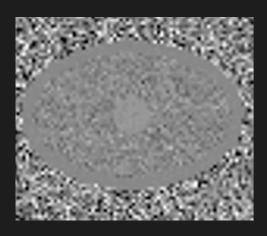




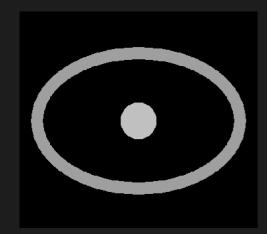


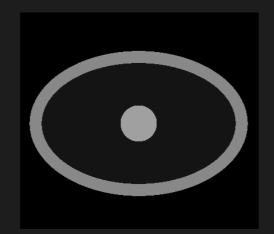


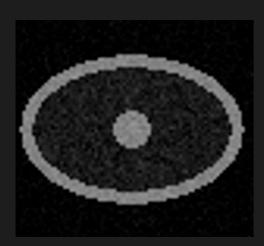


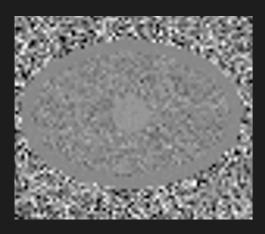




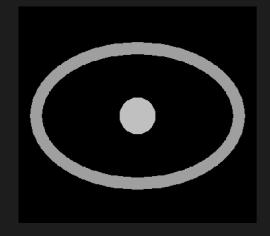




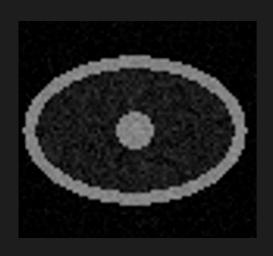


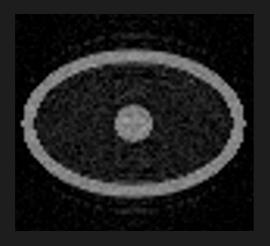


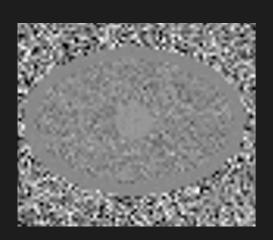


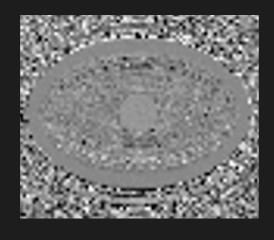






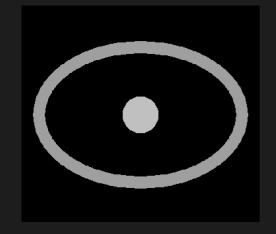


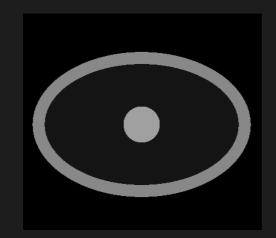


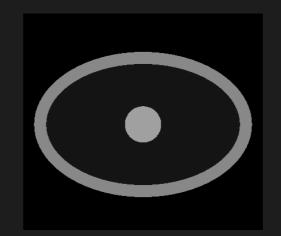


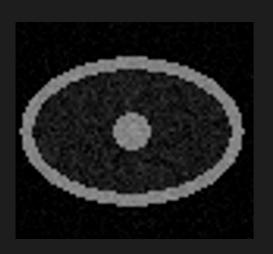
Ghosting

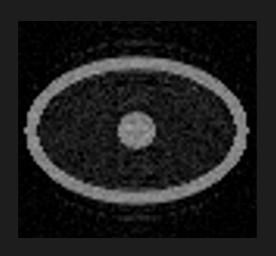


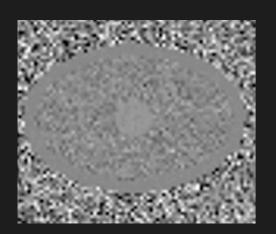


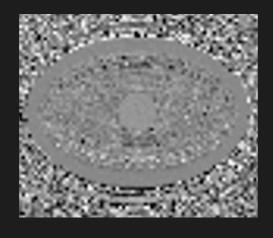






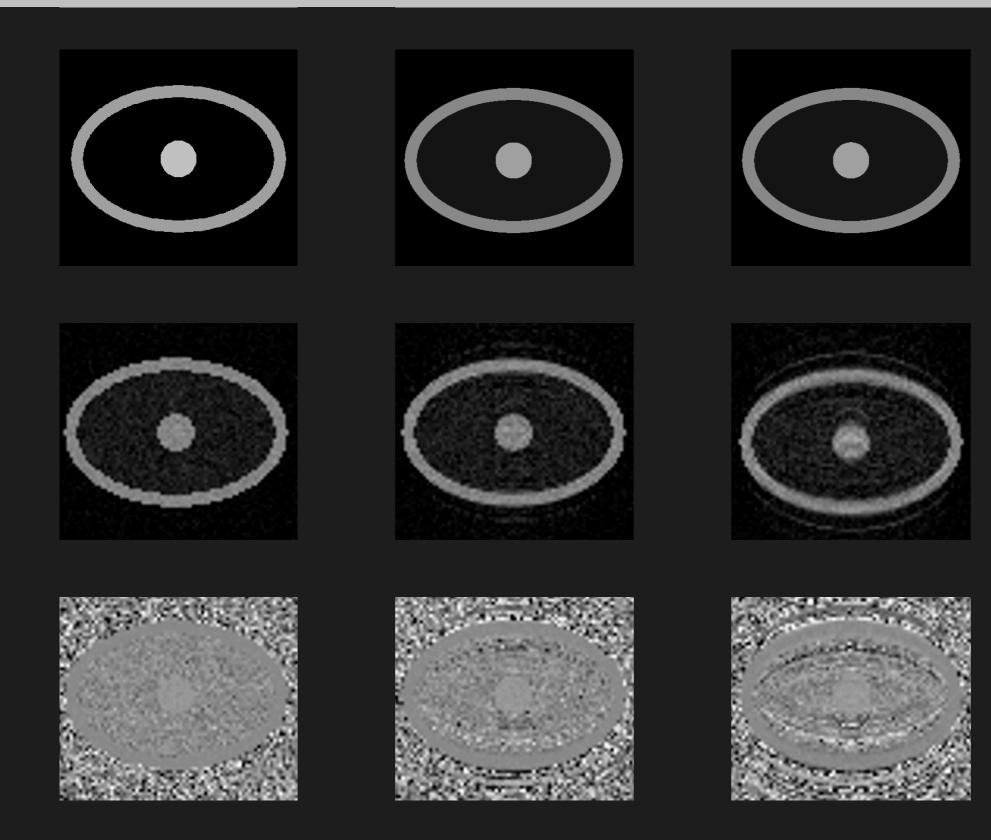






Ghosting

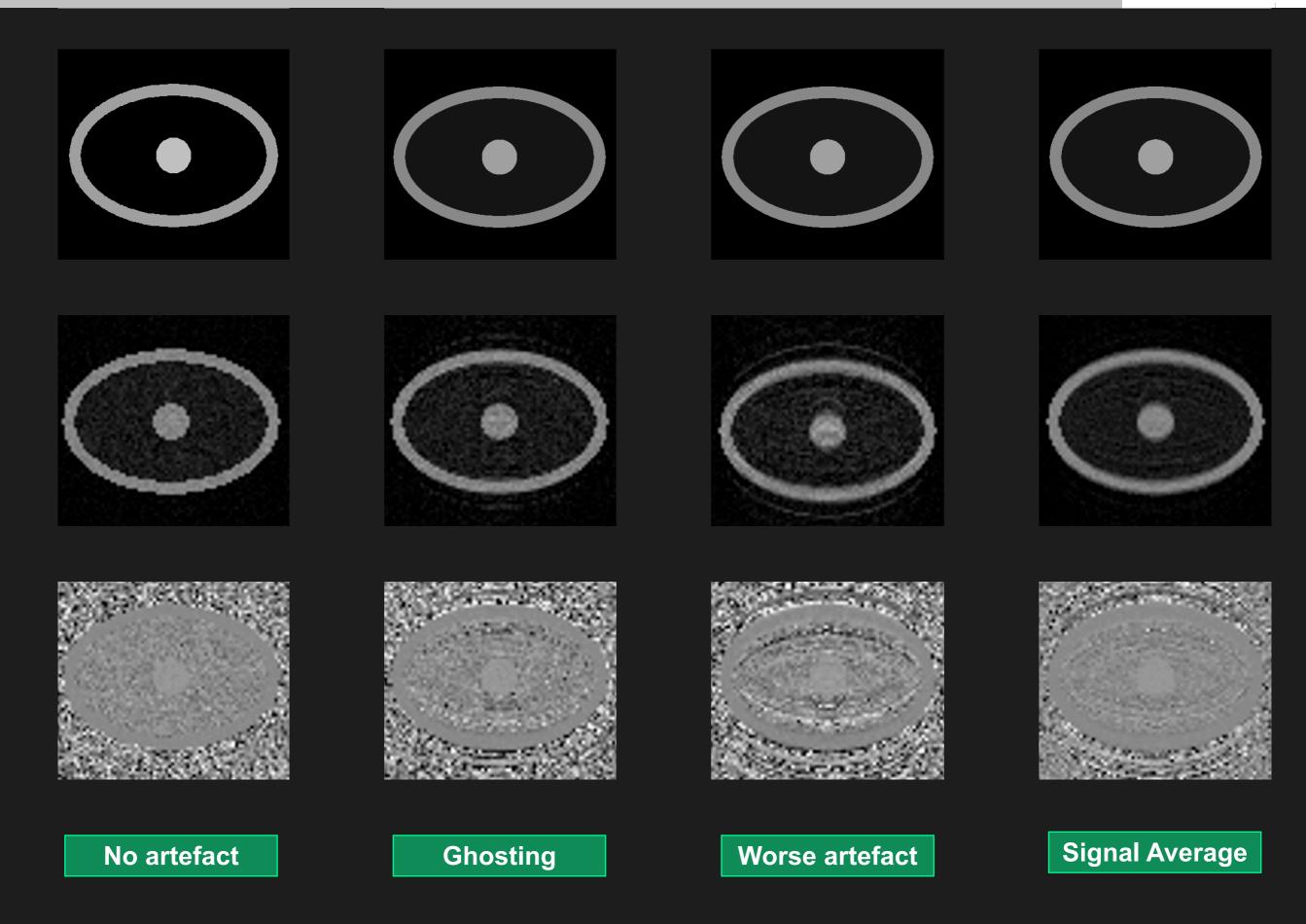




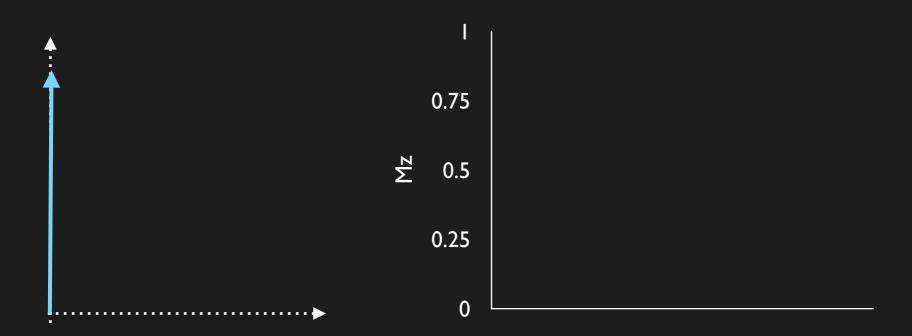
Ghosting

Worse artefact

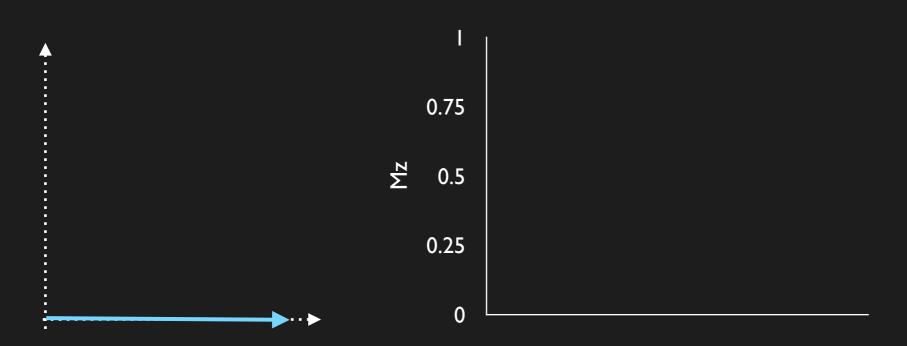




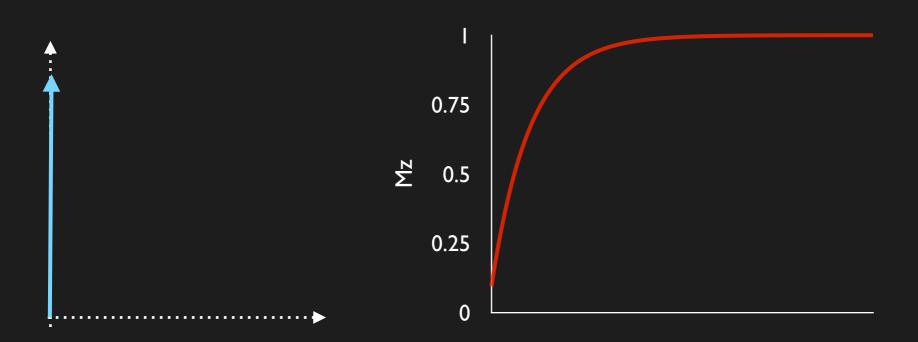






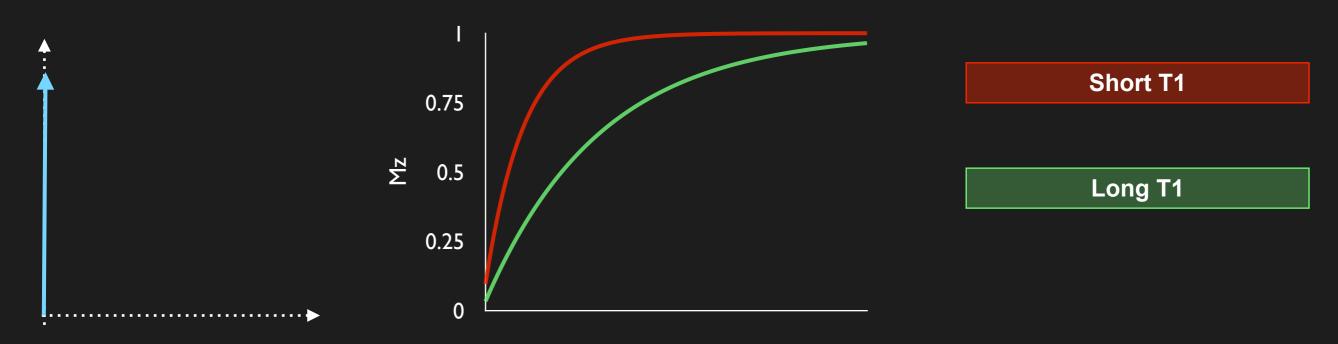




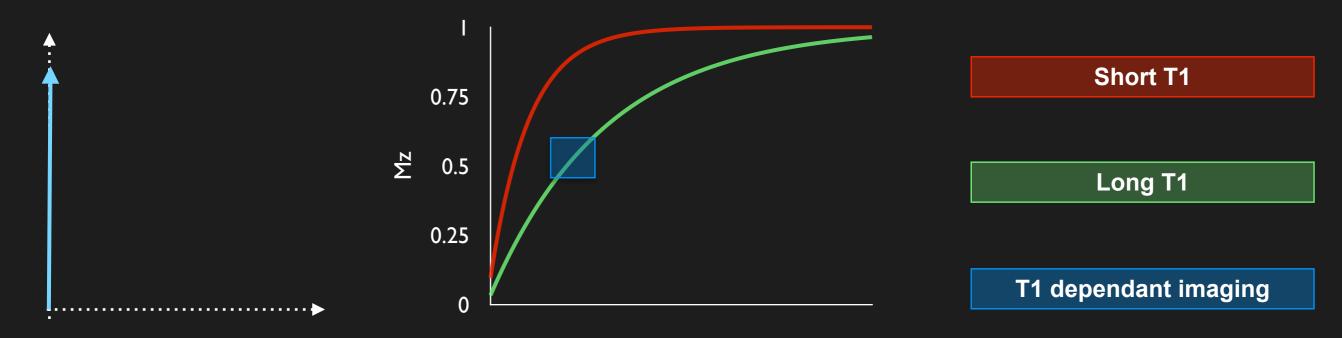


Short T1

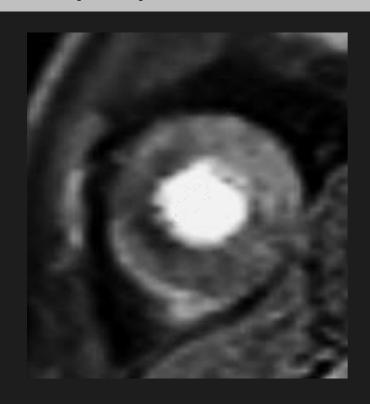


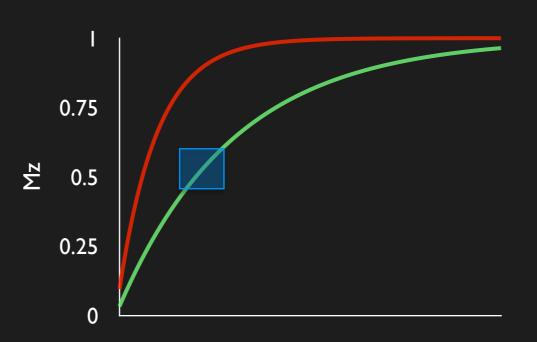










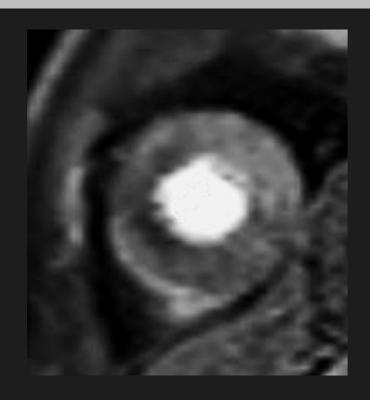


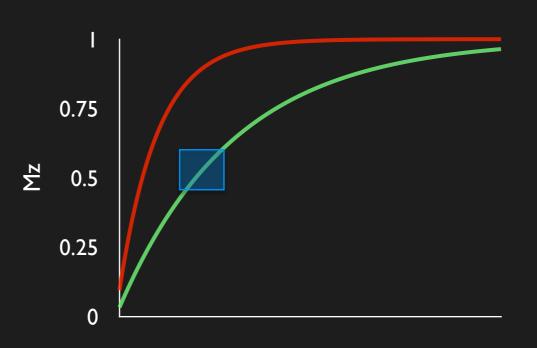
Short T1

Long T1

T1 dependant imaging



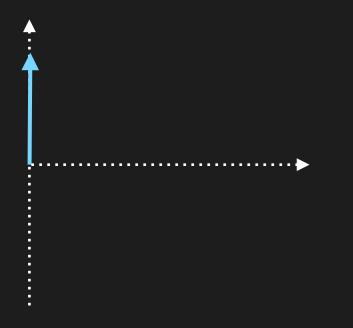




Short T1

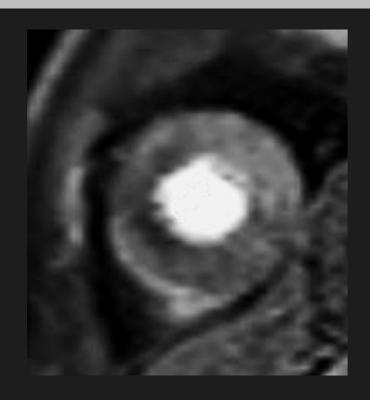
Long T1

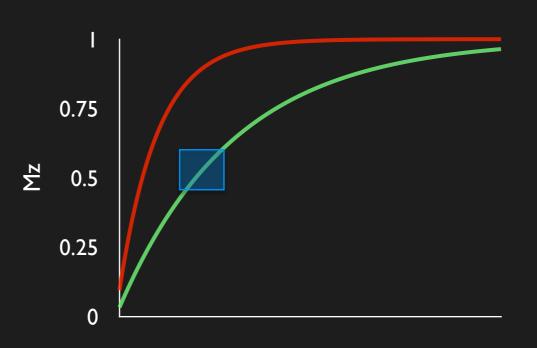
T1 dependant imaging







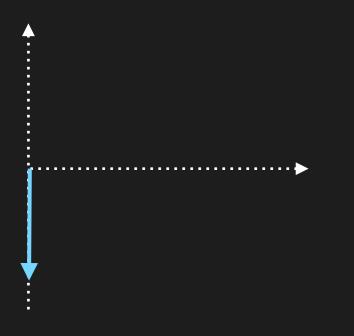




Short T1

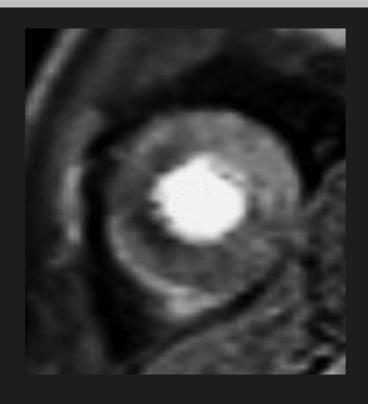
Long T1

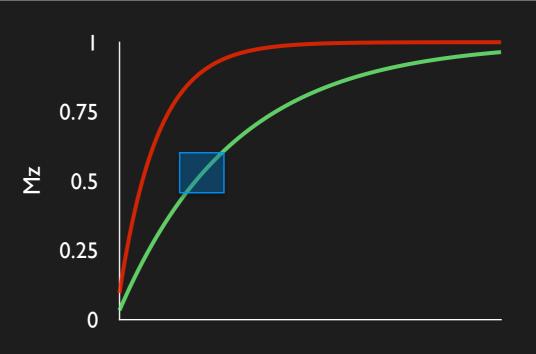
T1 dependant imaging







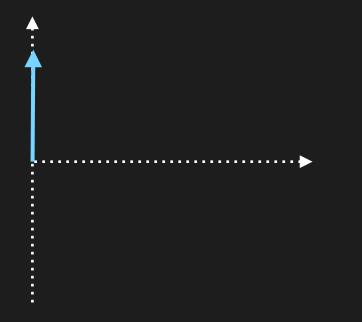


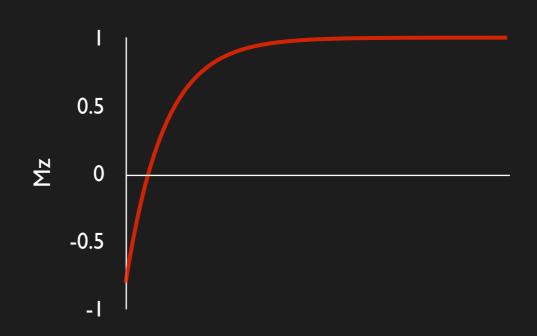


Short T1

Long T1

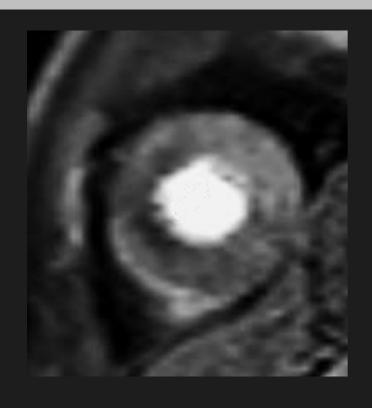
T1 dependant imaging

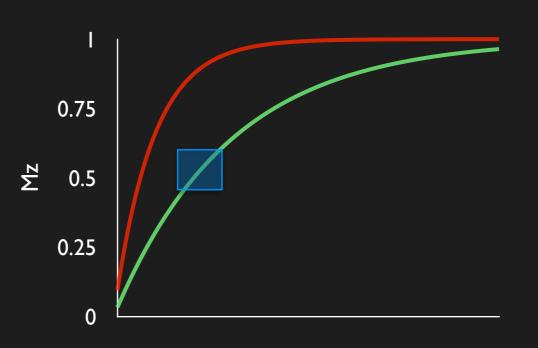




Null point at 0.693*T1



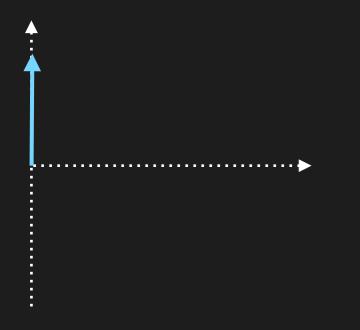


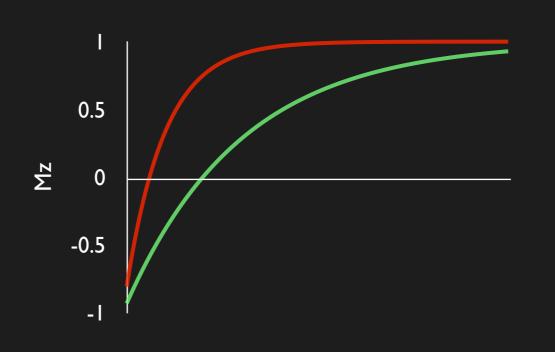


Short T1

Long T1

T1 dependant imaging

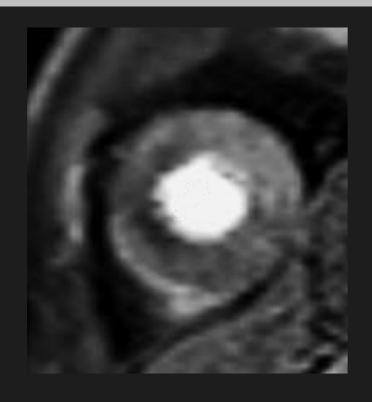


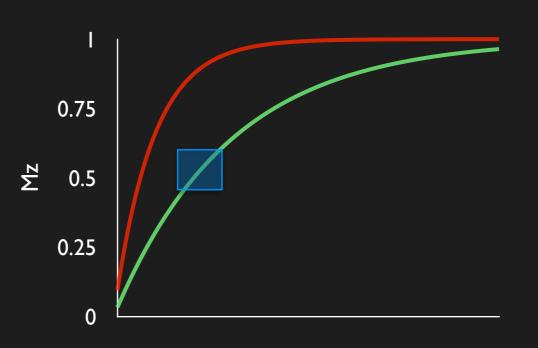


Null point at 0.693*T1

Longer T1



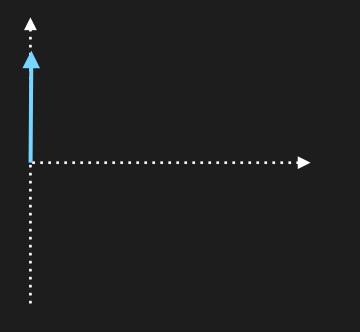


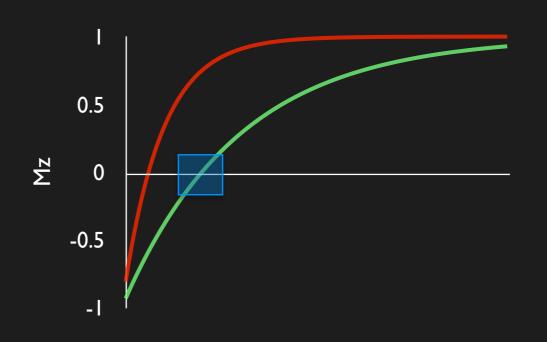




Long T1

T1 dependant imaging



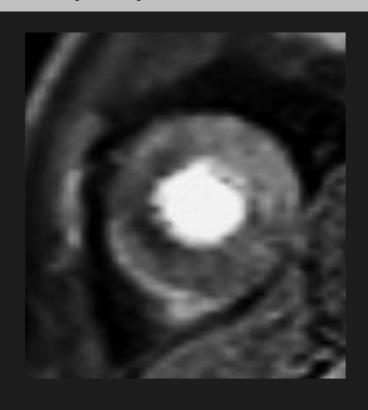


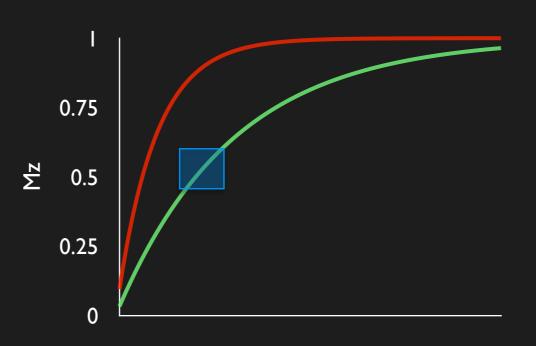
Null point at 0.693*T1

Longer T1

High contrast





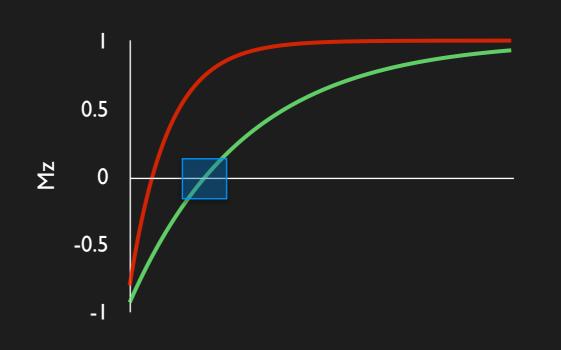


Short T1

Long T1

T1 dependant imaging



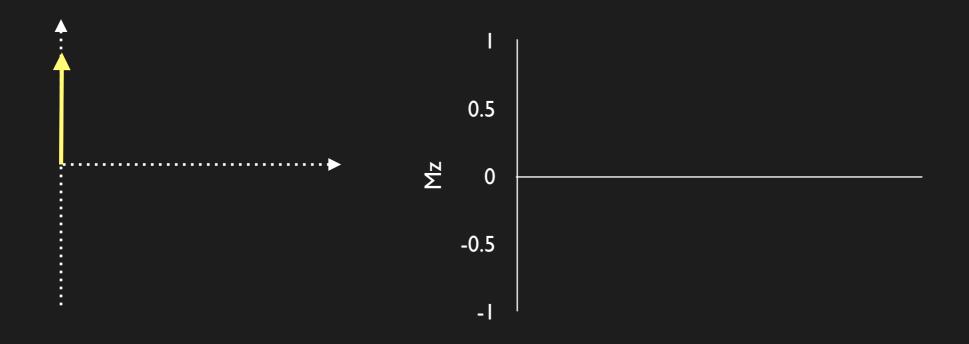


Null point at 0.693*T1

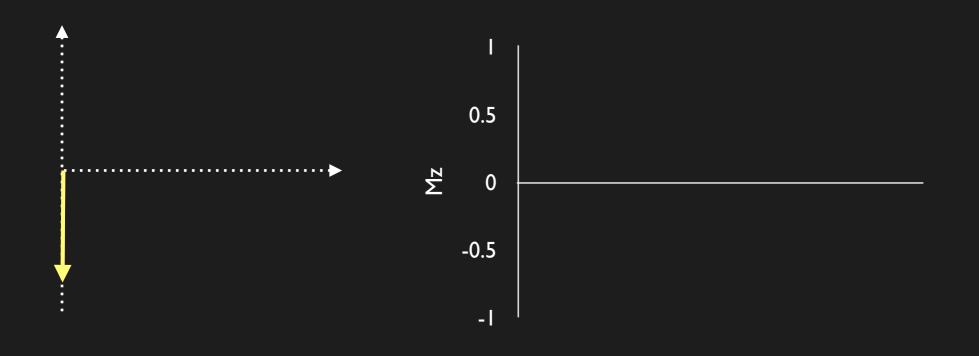
Longer T1

High contrast



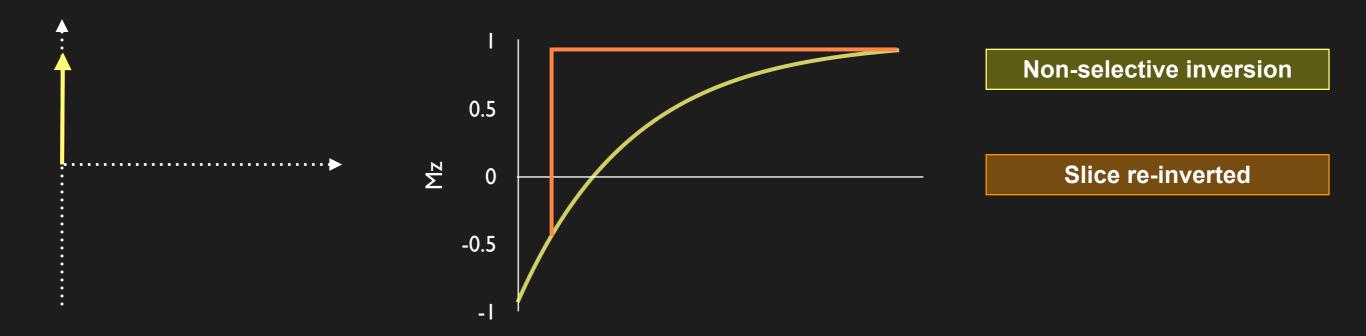




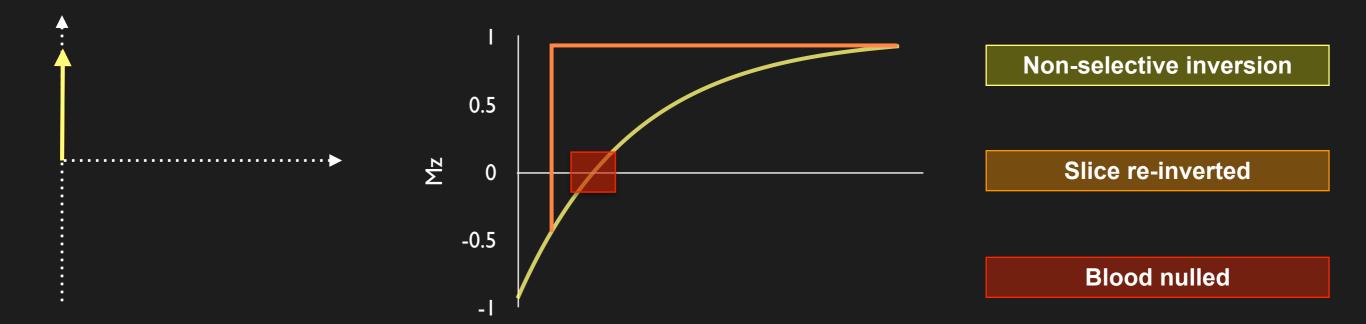


Non-selective inversion

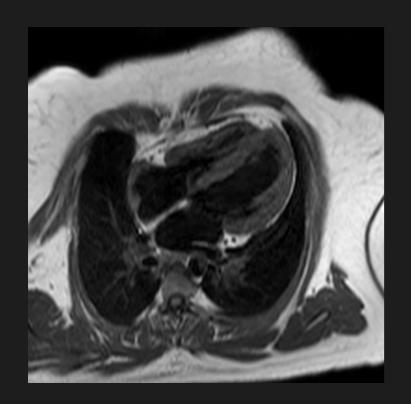


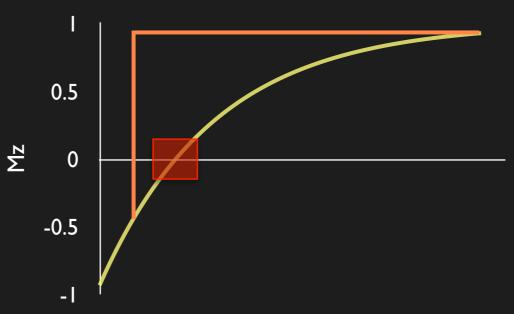










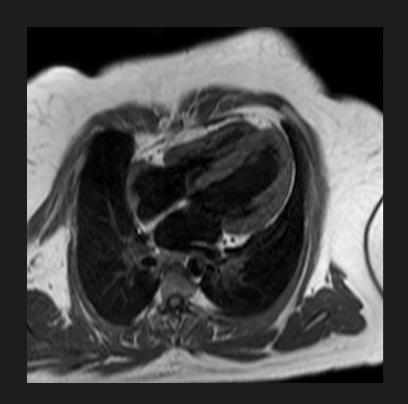


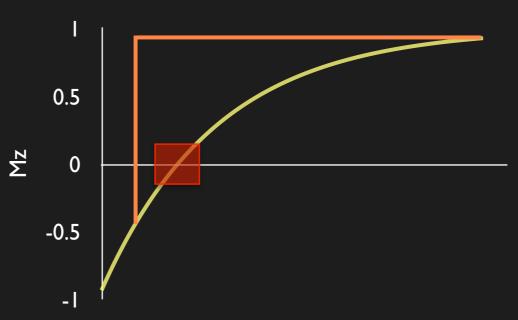
Non-selective inversion

Slice re-inverted

Blood nulled



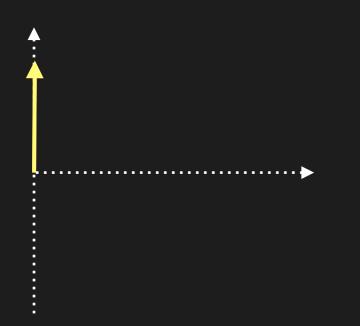




Non-selective inversion

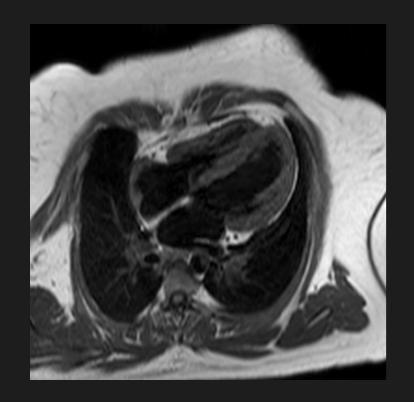
Slice re-inverted

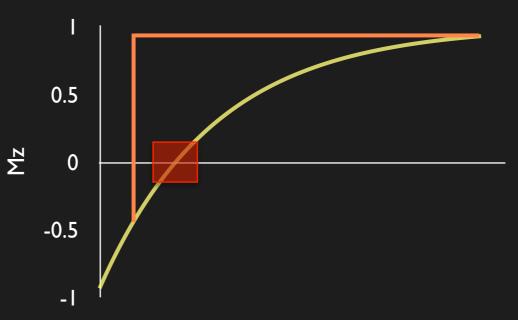
Blood nulled







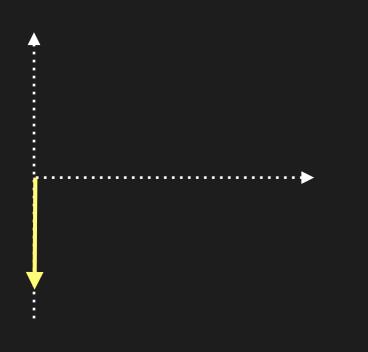




Non-selective inversion

Slice re-inverted

Blood nulled

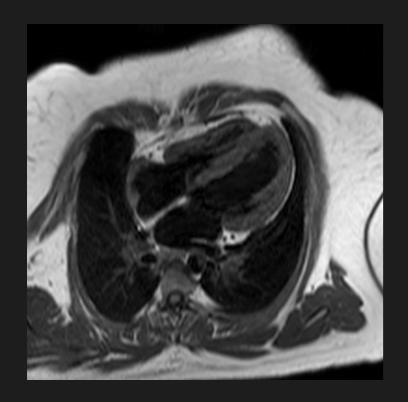


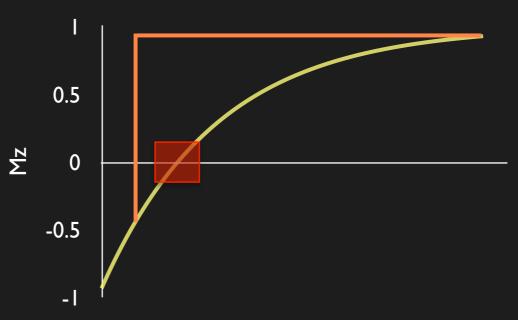


Non-selective inversion

More inversion recovery - DIR and TIR



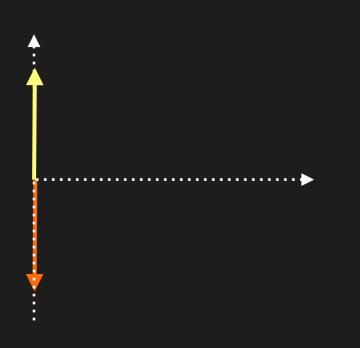


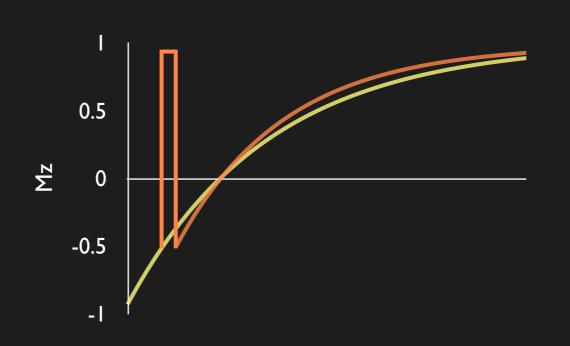


Non-selective inversion

Slice re-inverted

Blood nulled



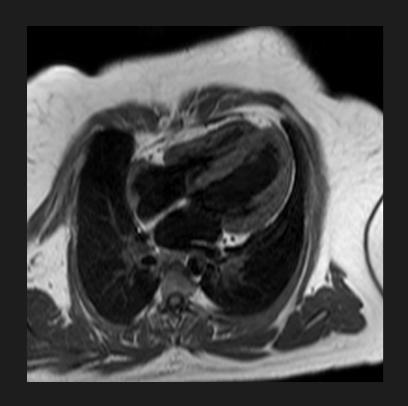


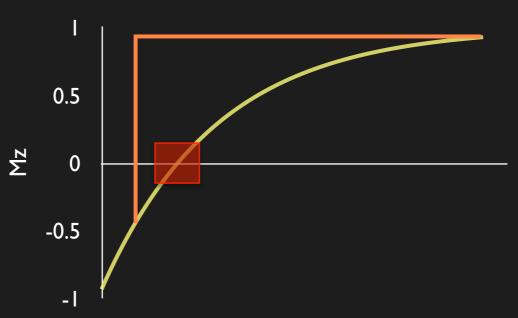
Non-selective inversion

Slice re-inverted x 2

More inversion recovery - DIR and TIR



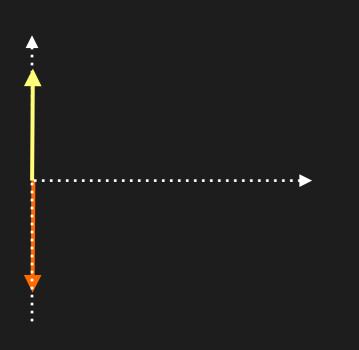


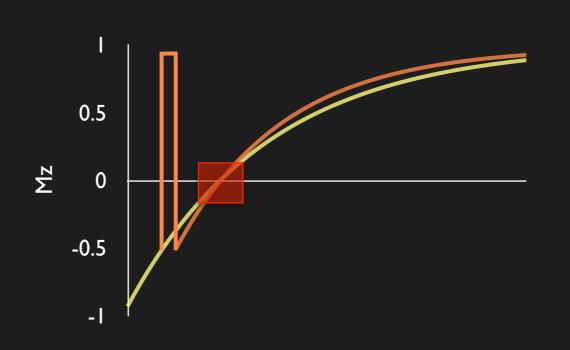


Non-selective inversion

Slice re-inverted

Blood nulled





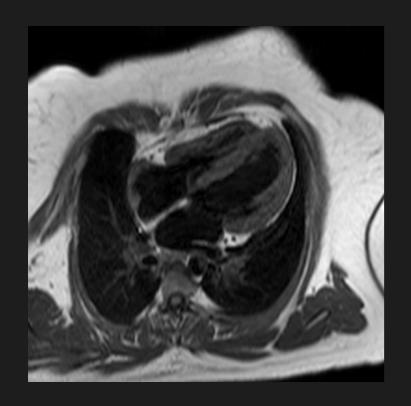
Non-selective inversion

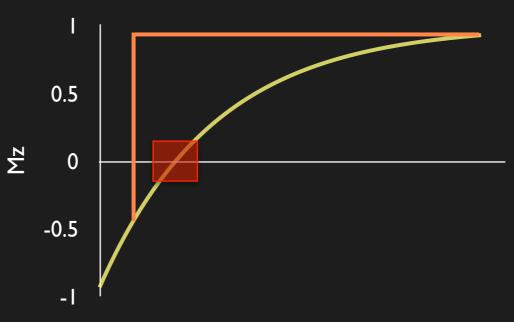
Slice re-inverted x 2

Blood and fat inverted

More inversion recovery - DIR and TIR





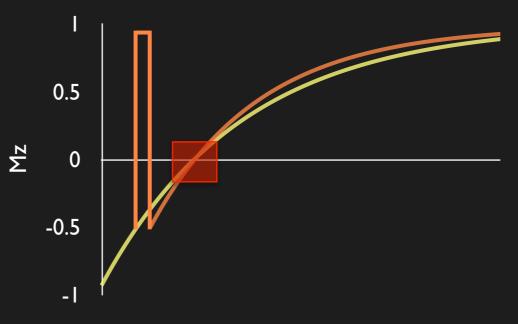


Non-selective inversion

Slice re-inverted

Blood nulled





Non-selective inversion

Slice re-inverted x 2

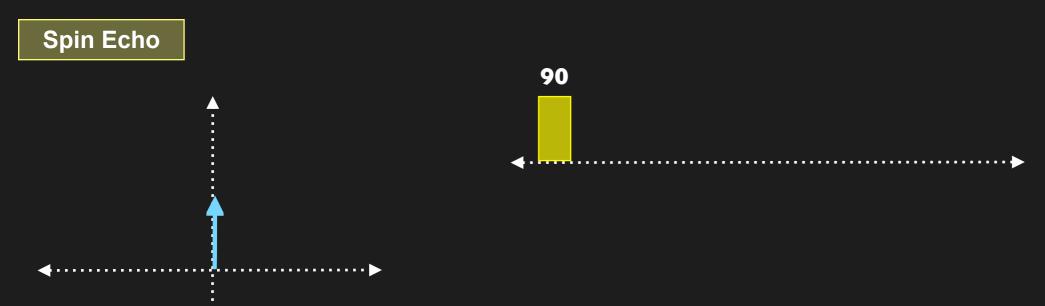
Blood and fat inverted



4.....

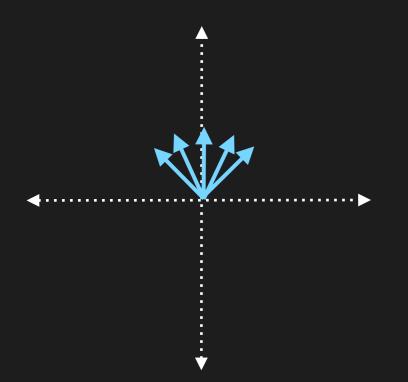
Spin Echo

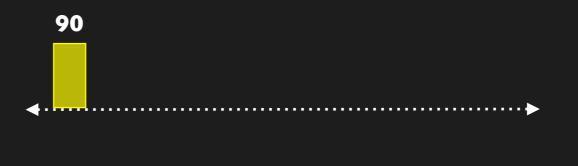






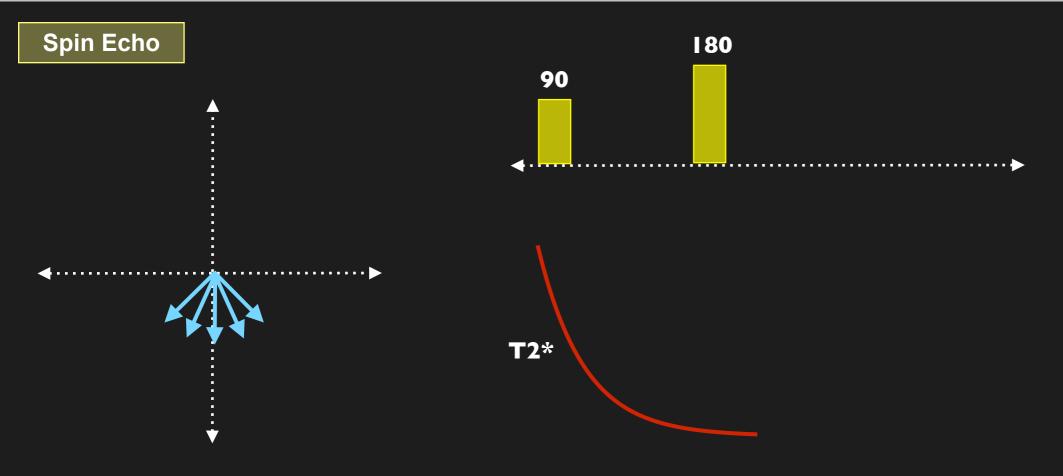




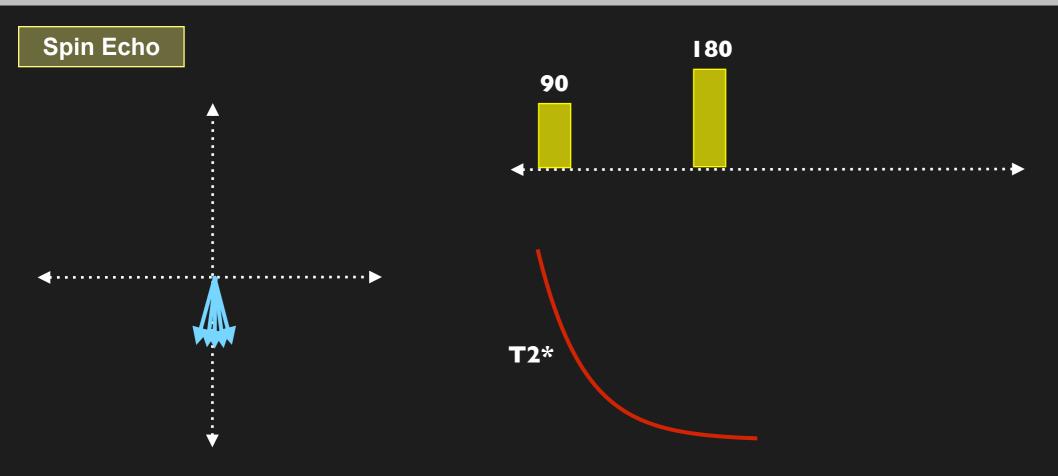




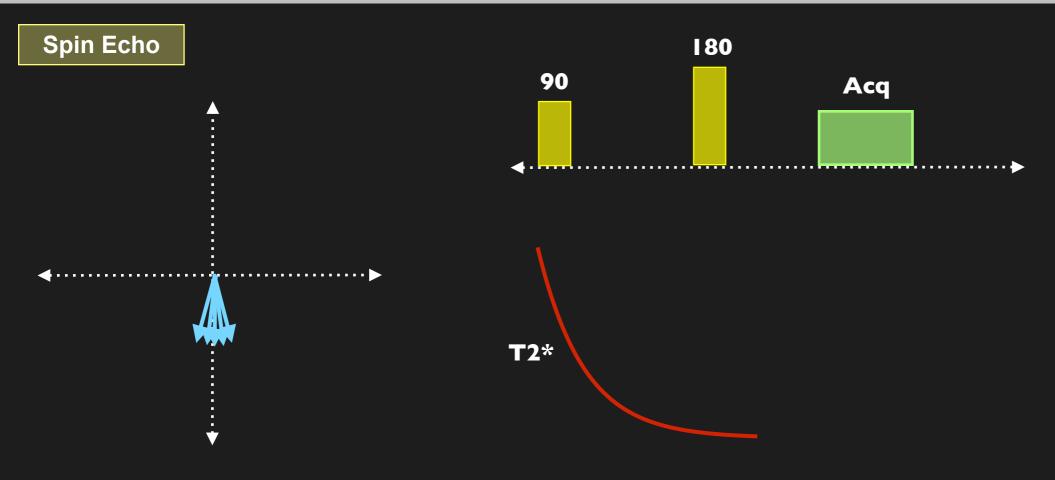




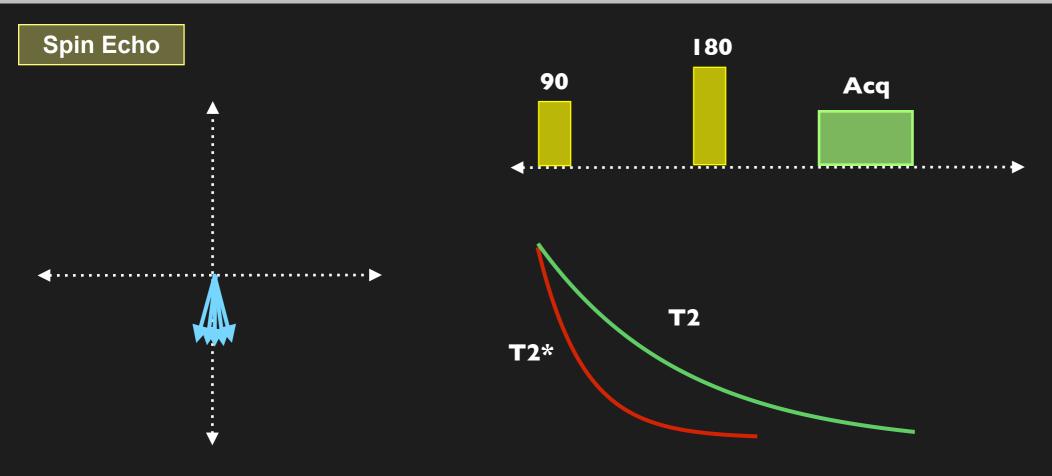


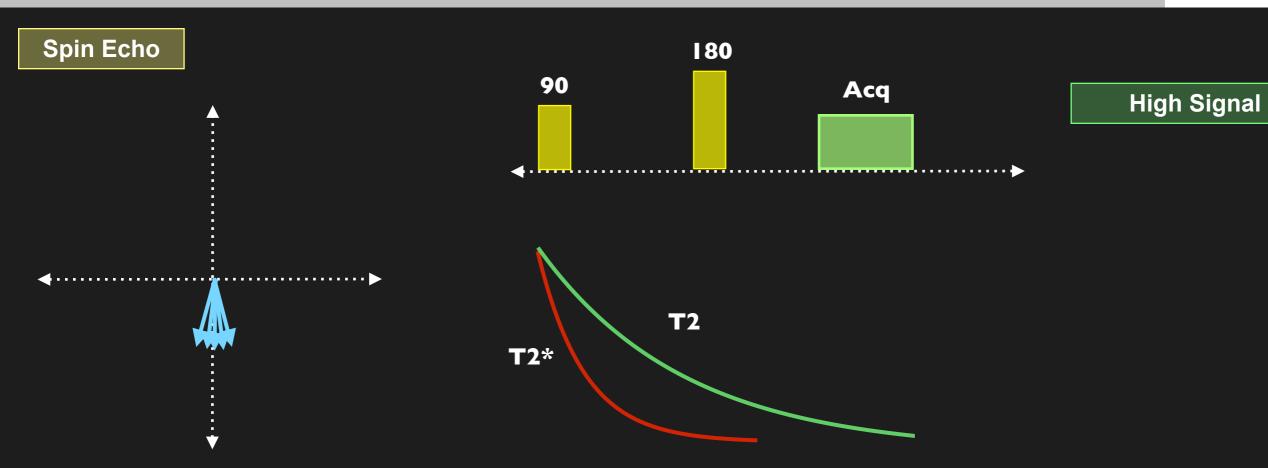




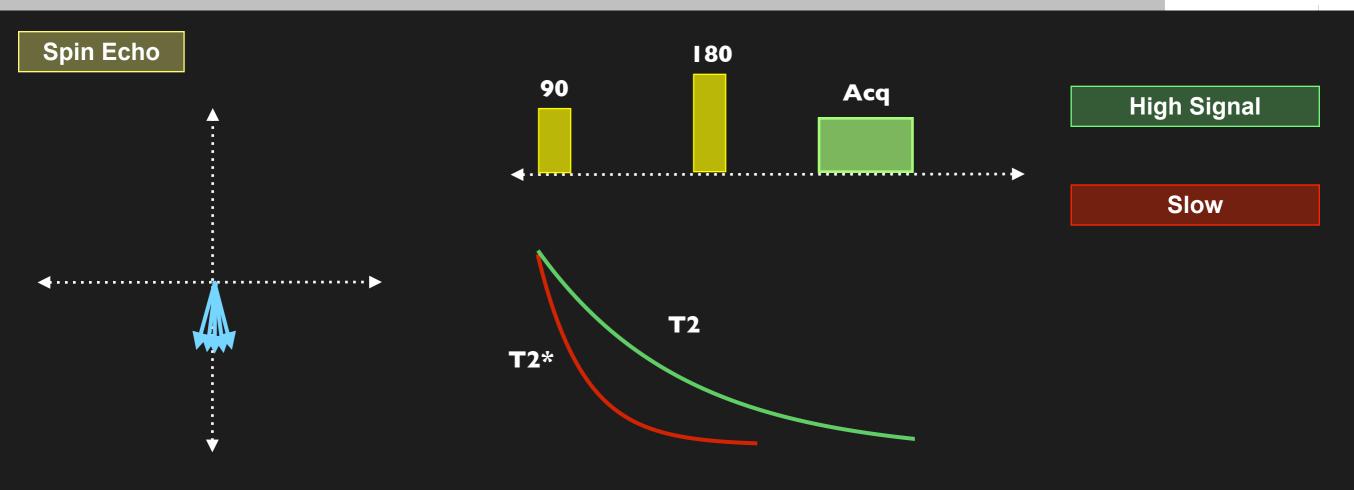




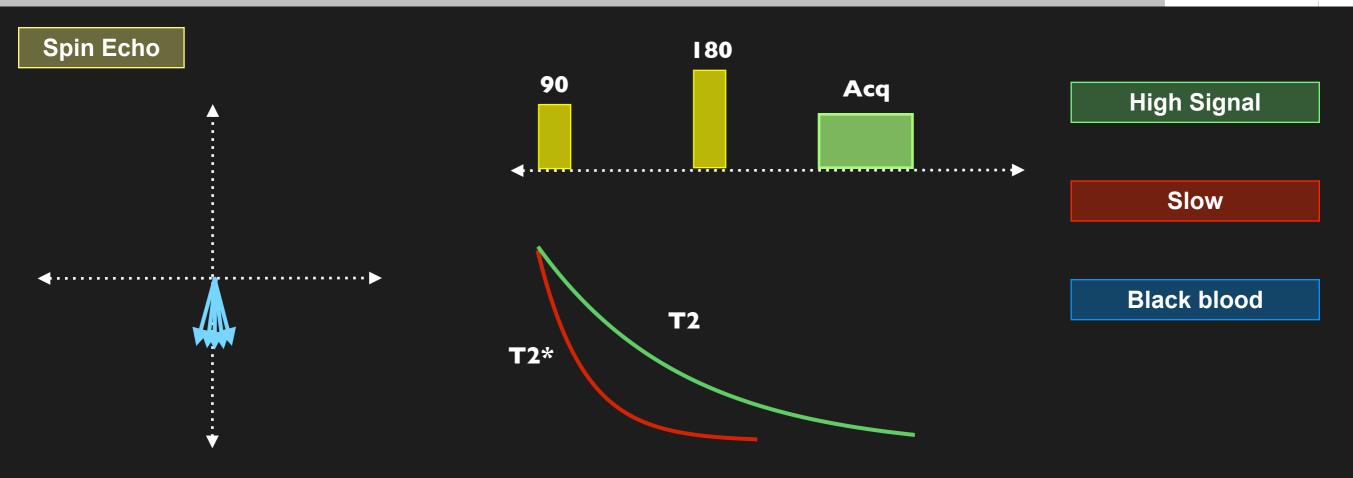




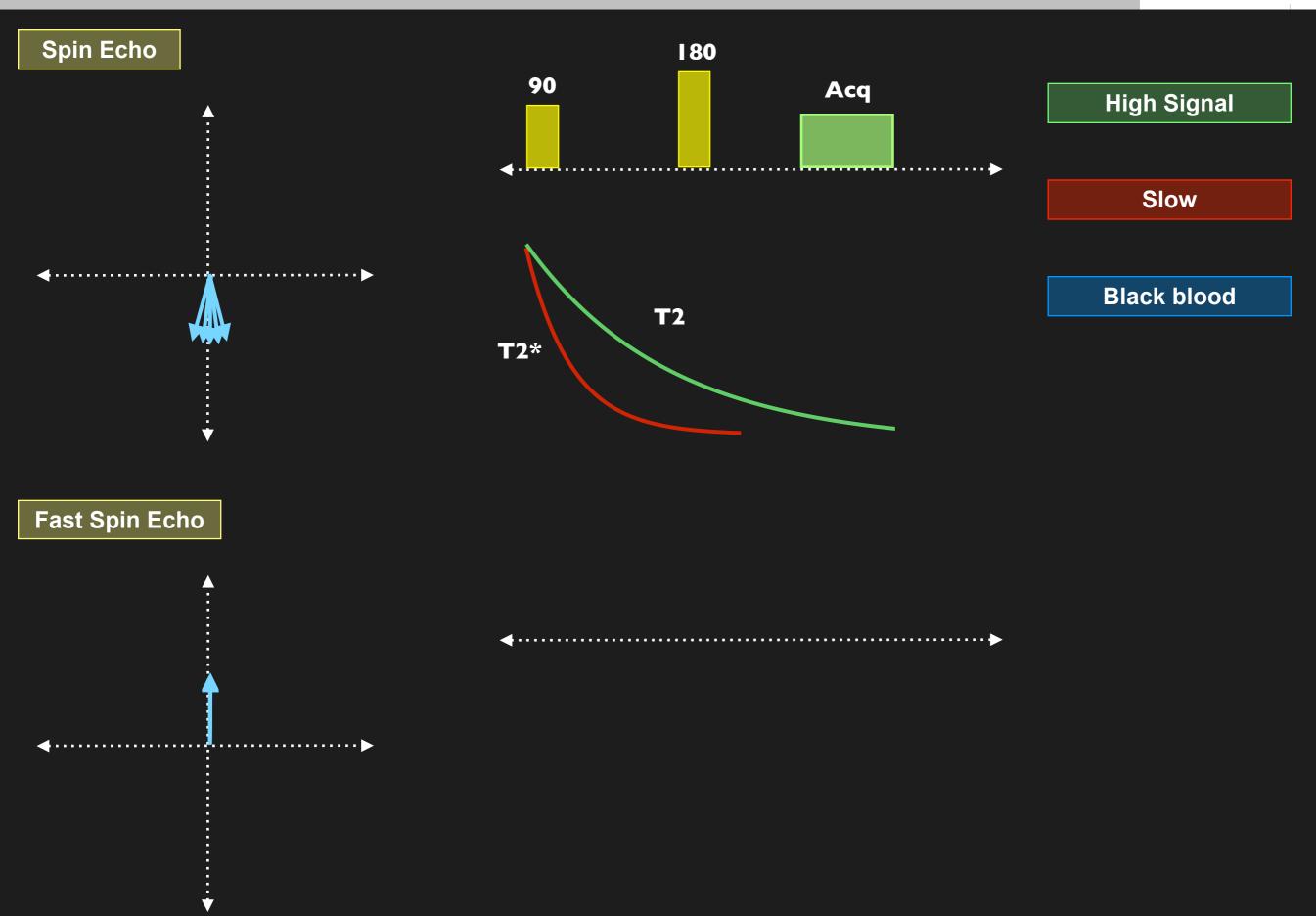




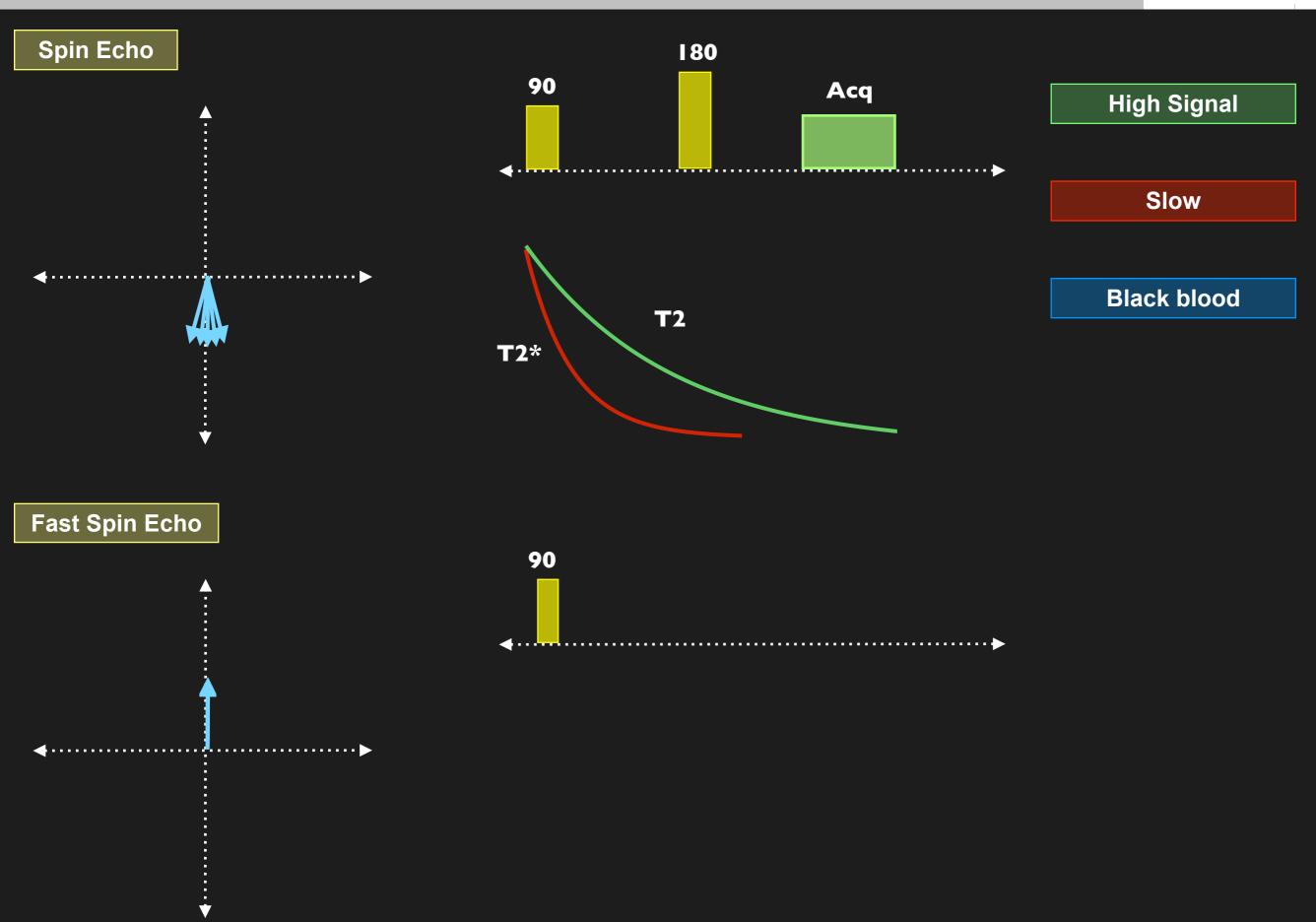




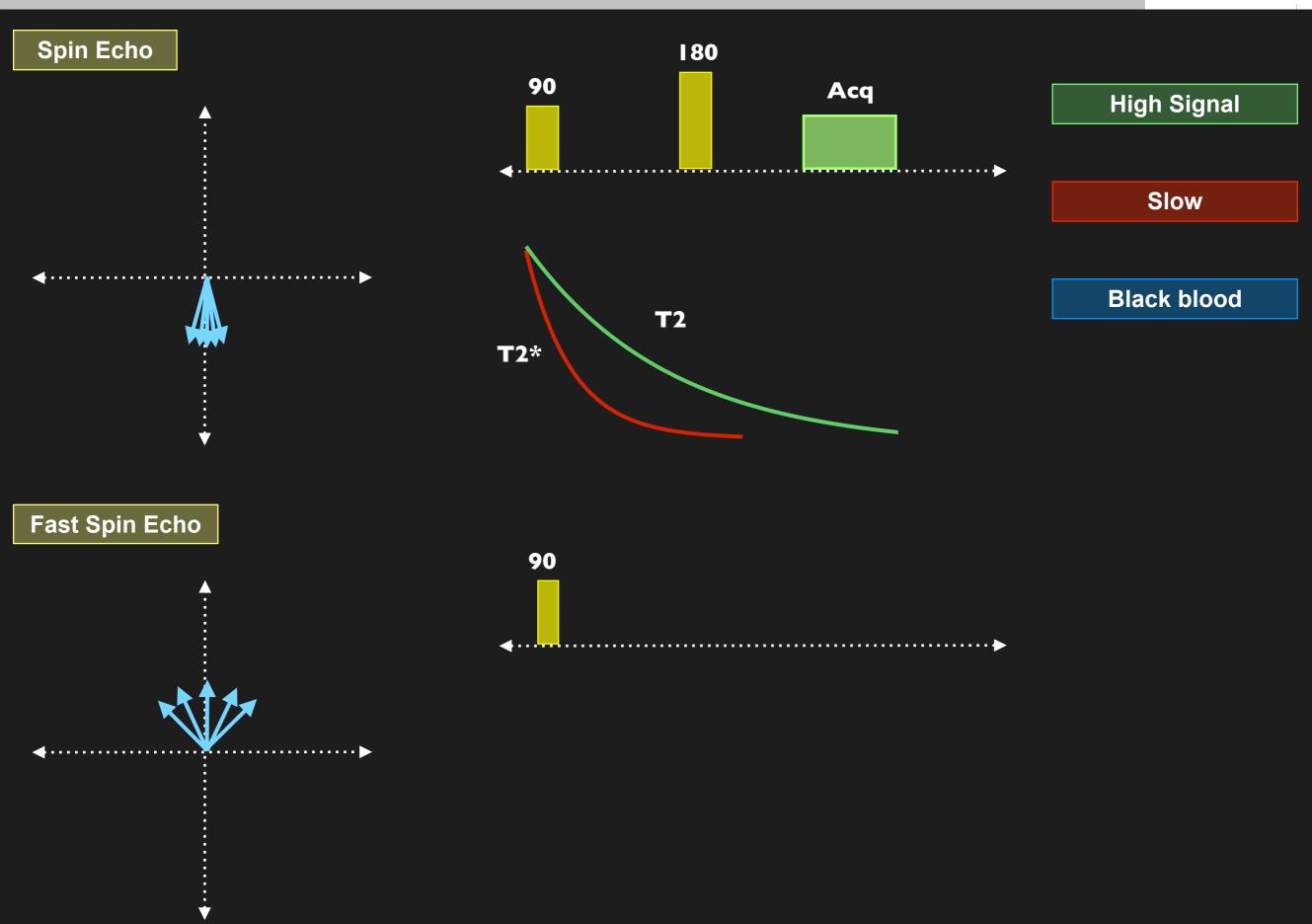


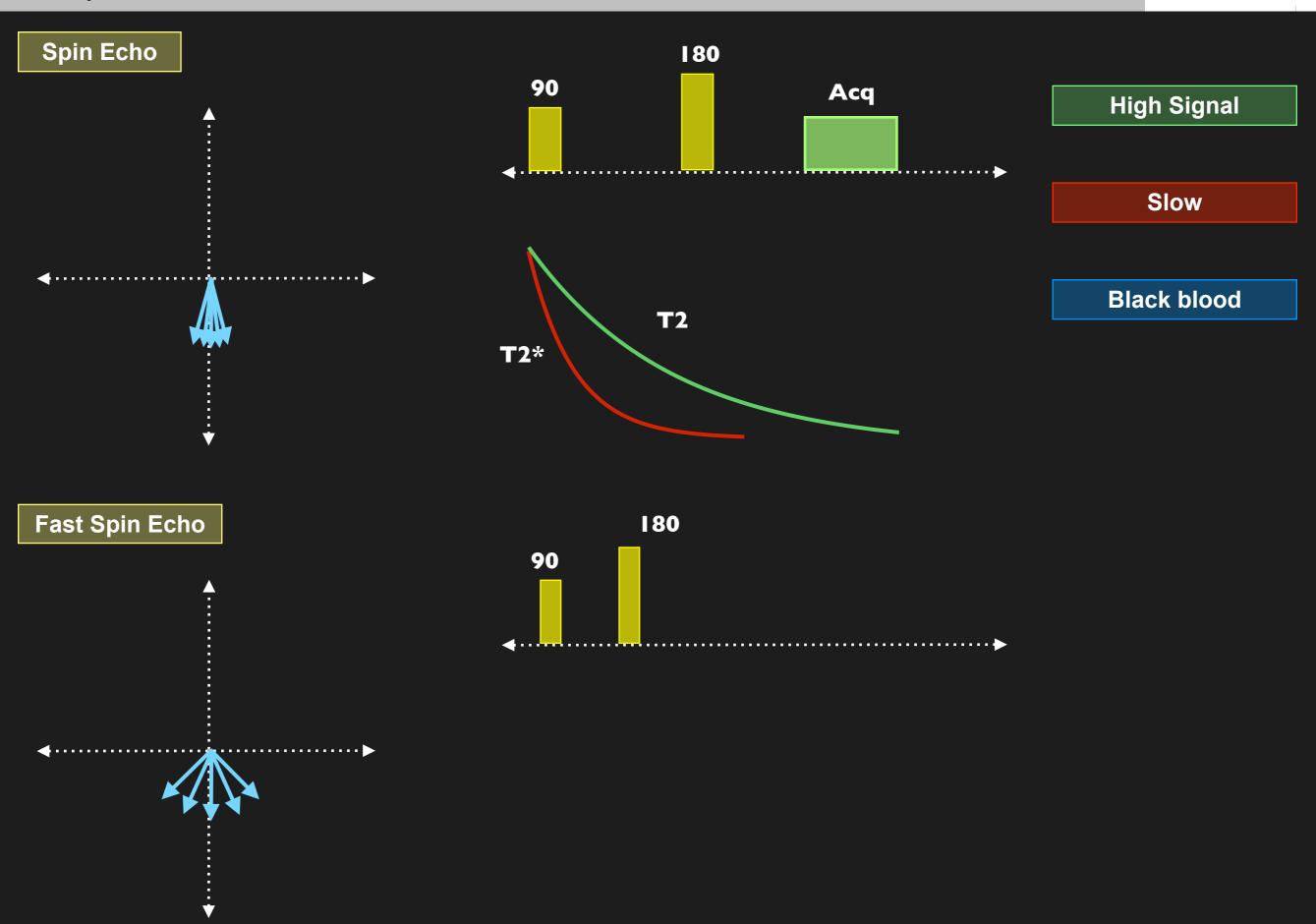


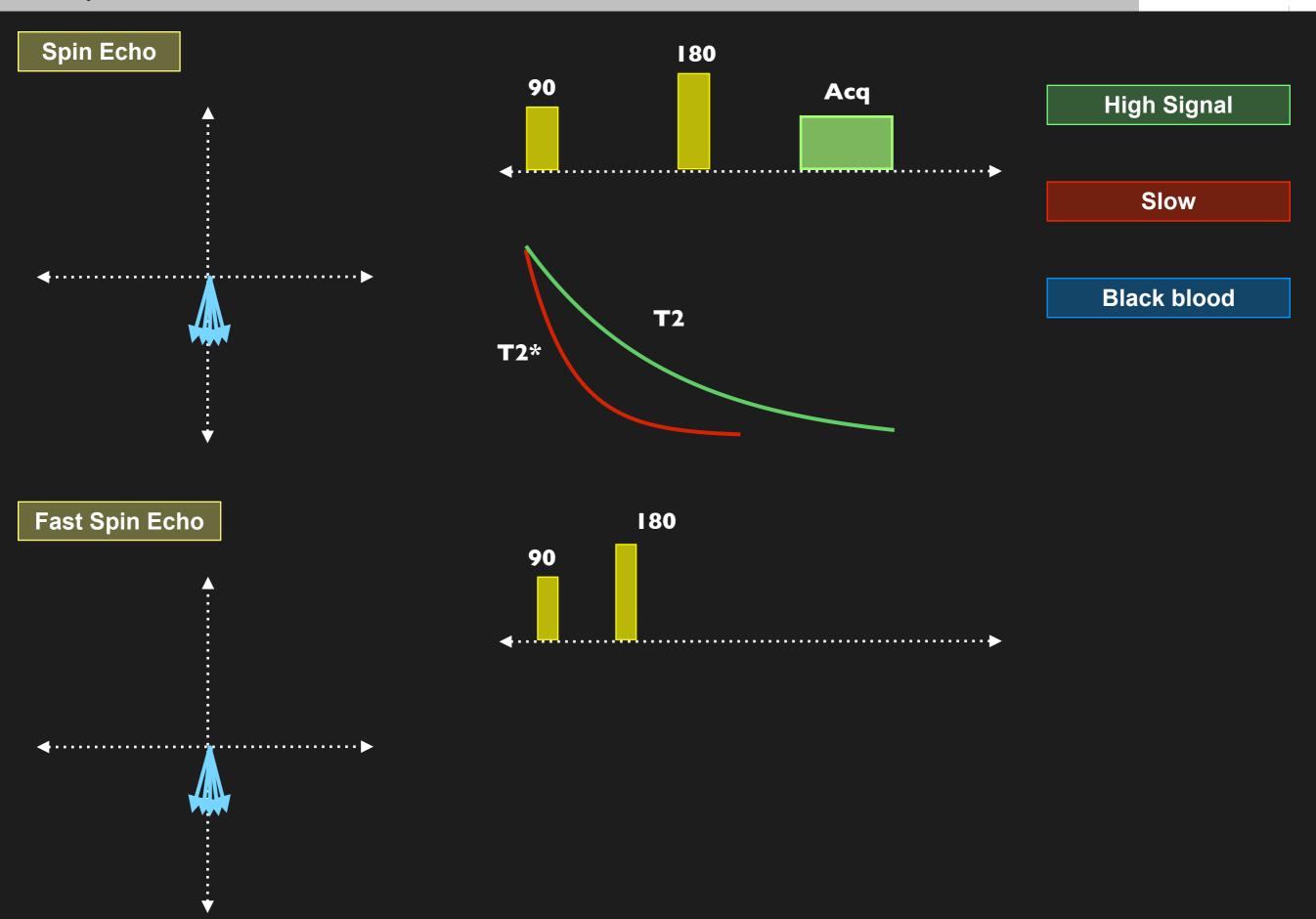


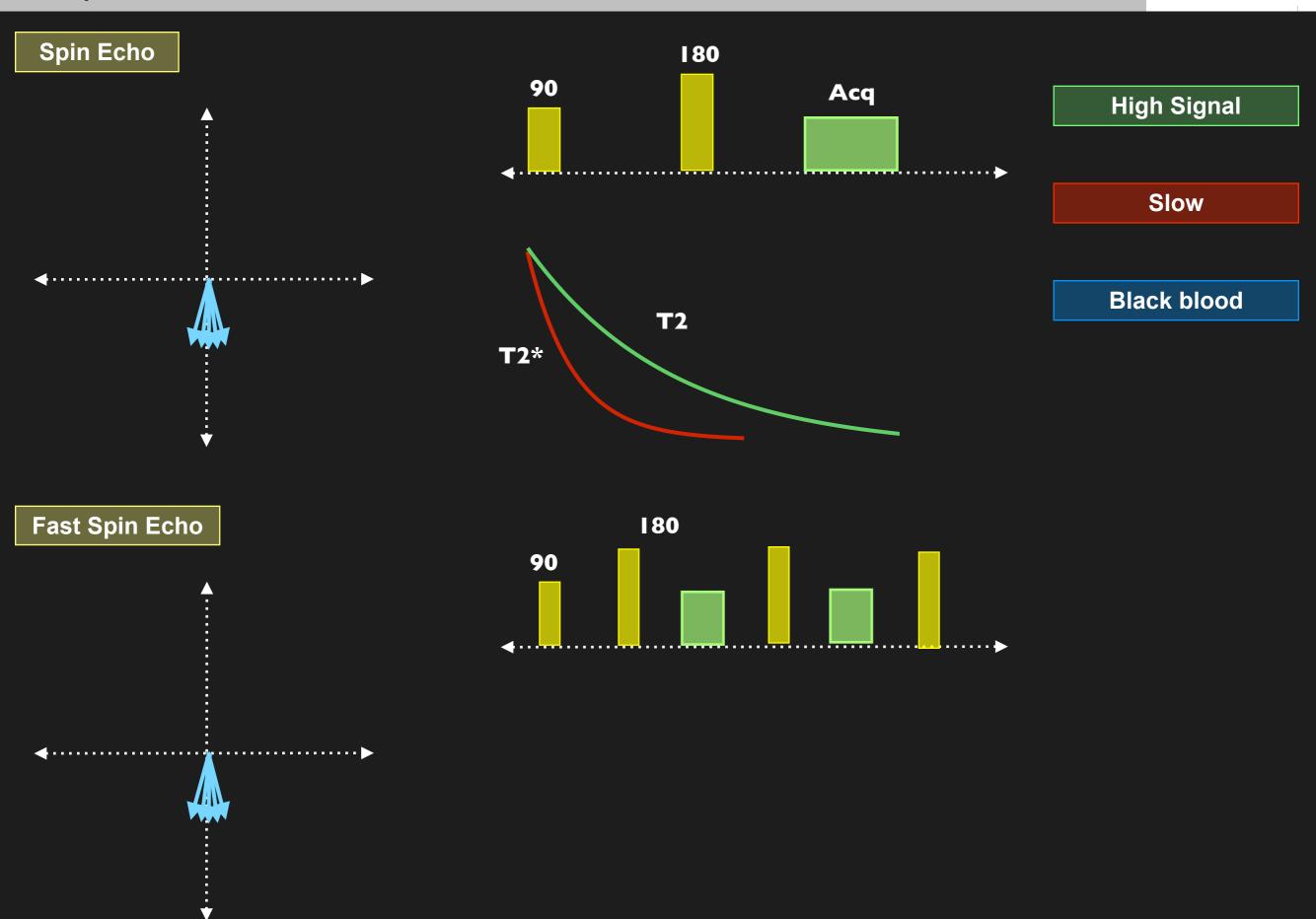




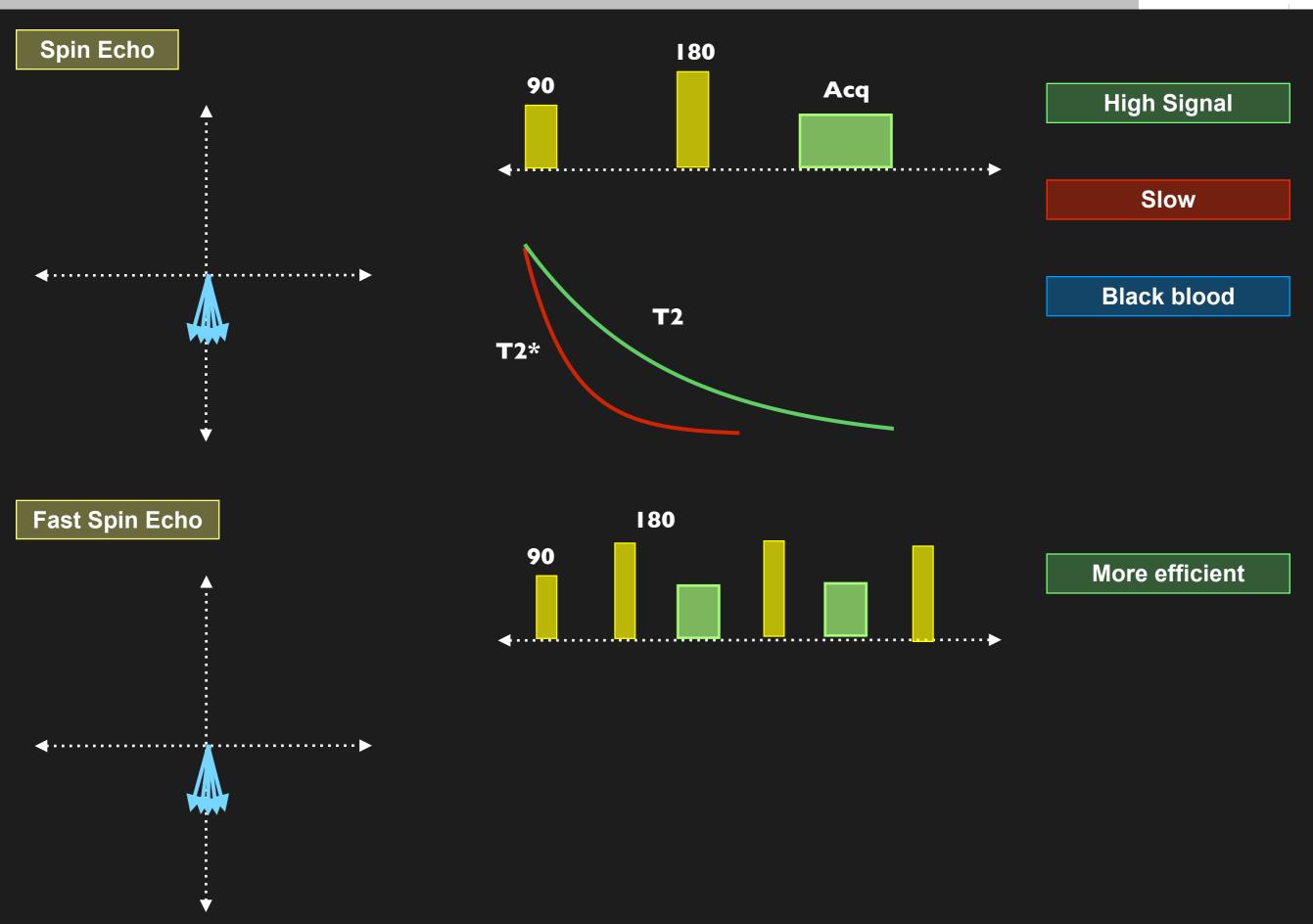


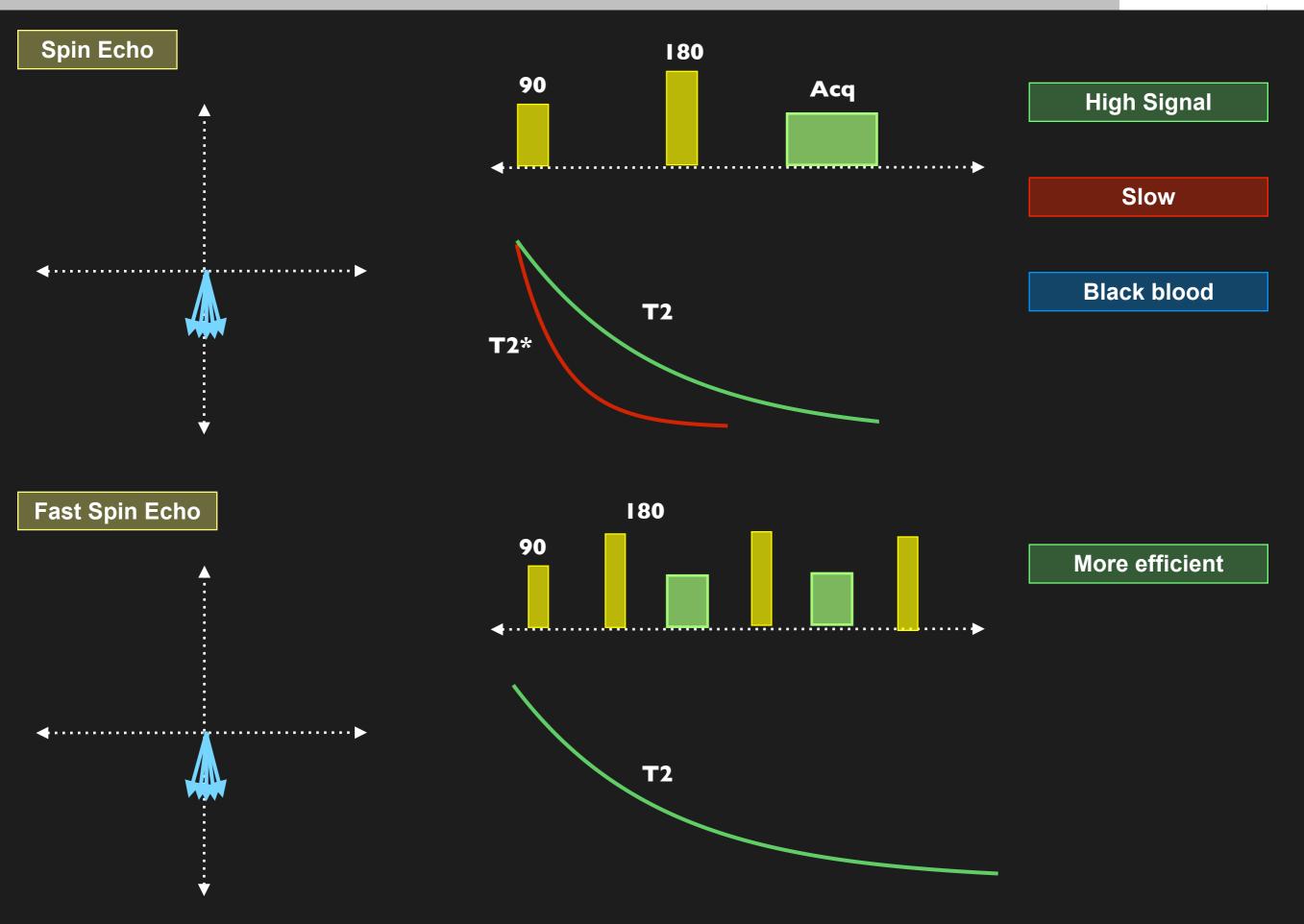


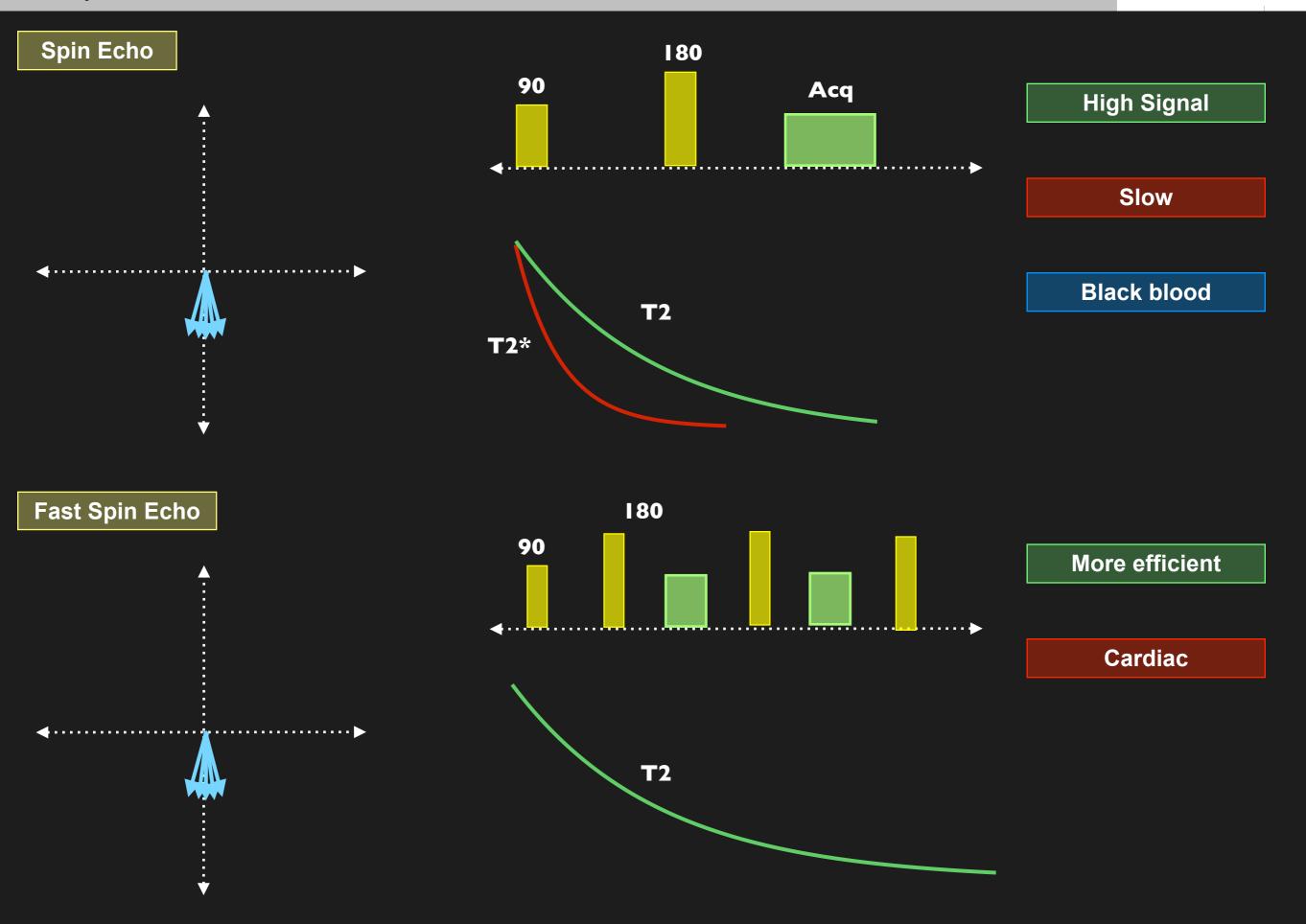




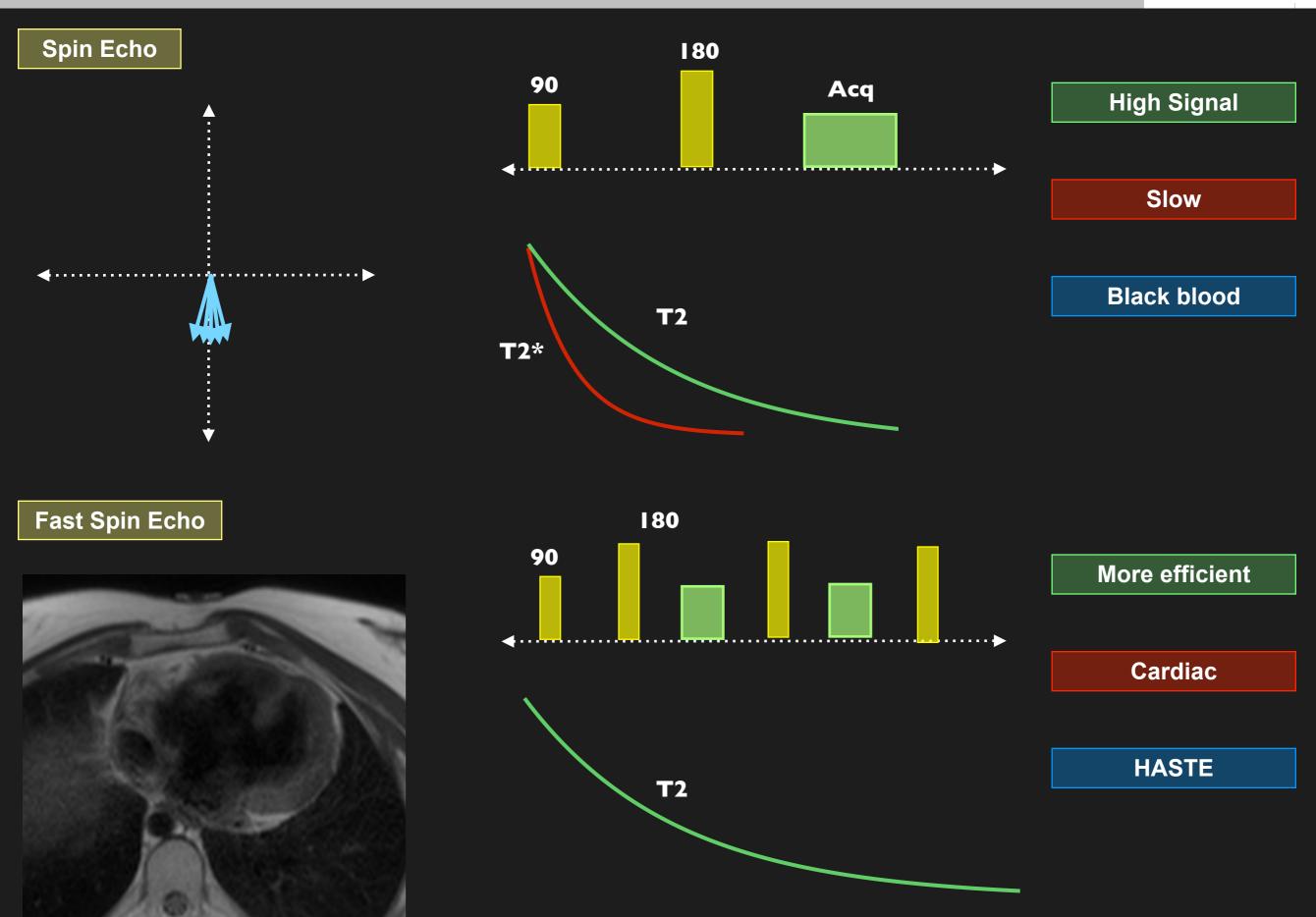










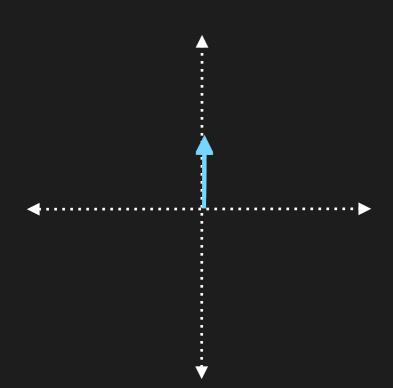






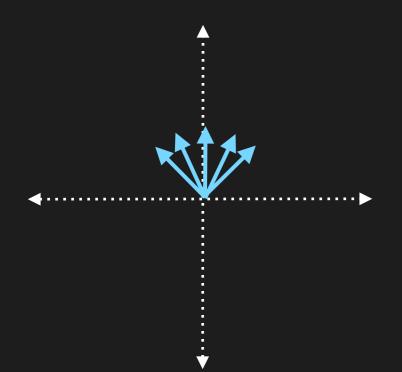




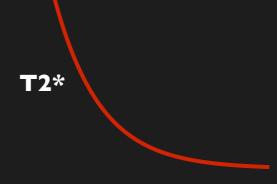




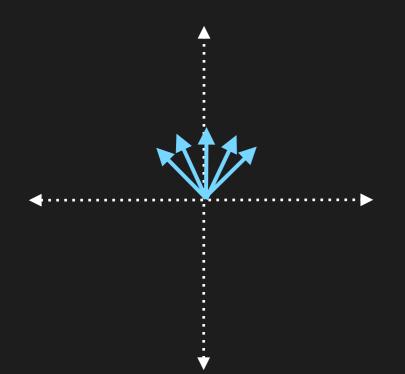


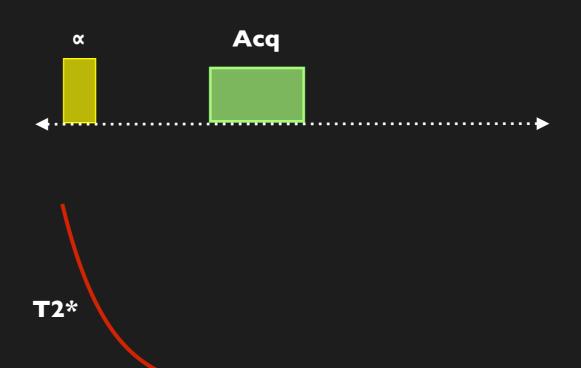






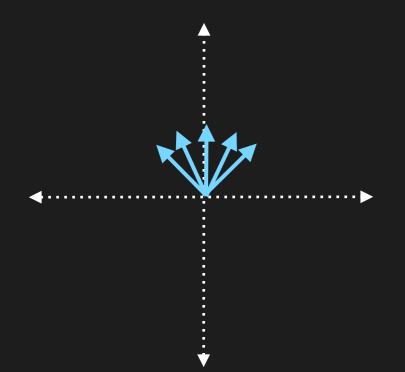


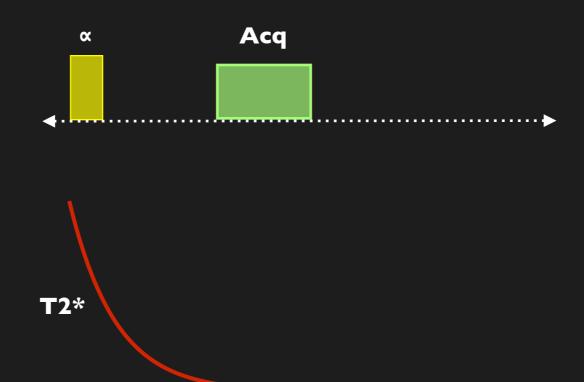




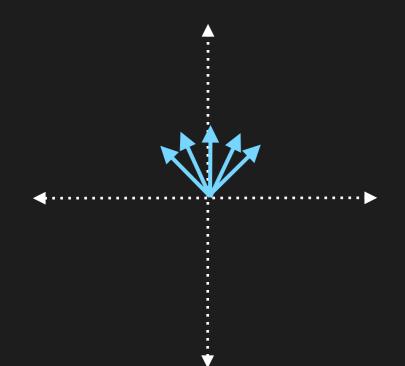








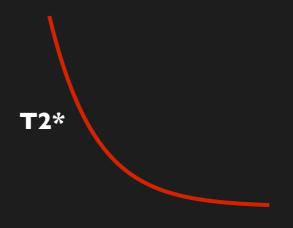
T2* not **T2**



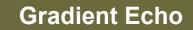


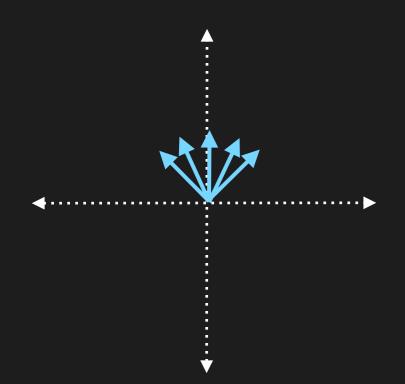
T2* not **T2**

Fast - cardiac

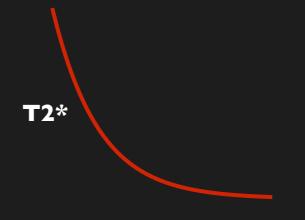








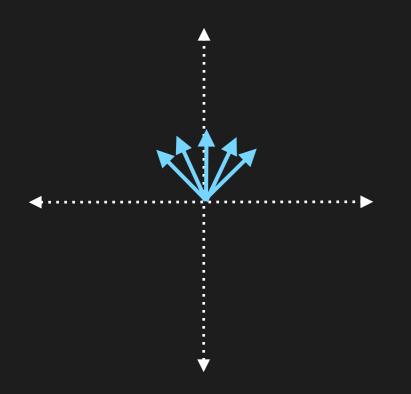


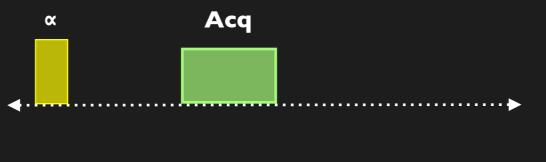


T2* not **T2**

Fast - cardiac

Bright blood





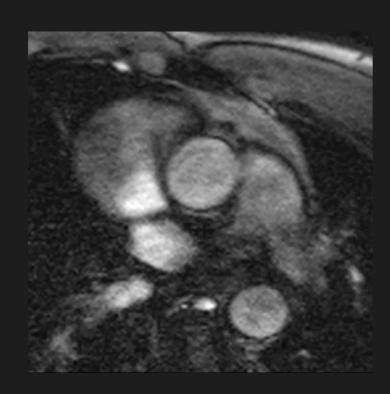
T2*

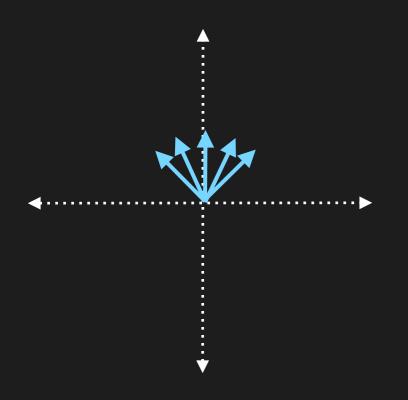




Fast - cardiac

Bright blood



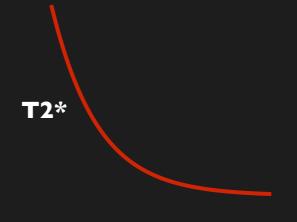


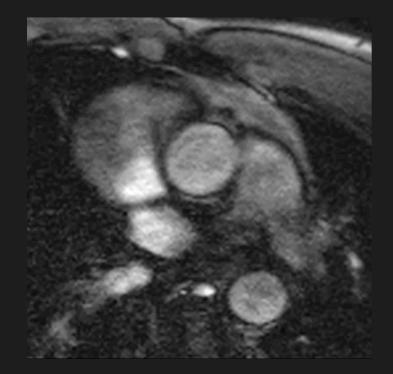


T2* not T2

Fast - cardiac

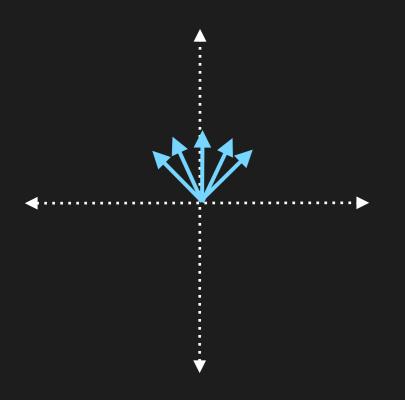
Bright blood





Saturated blood



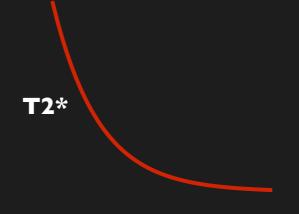




T2* not **T2**

Fast - cardiac

Bright blood



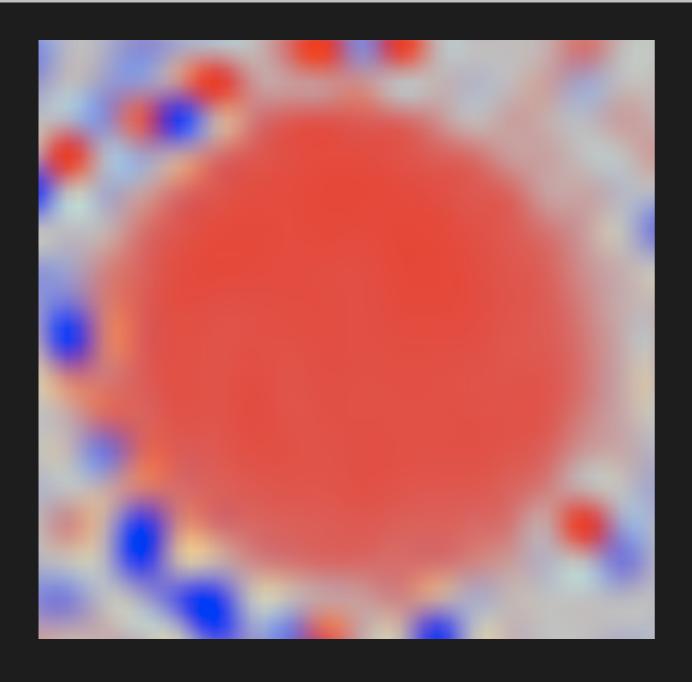


Saturated blood

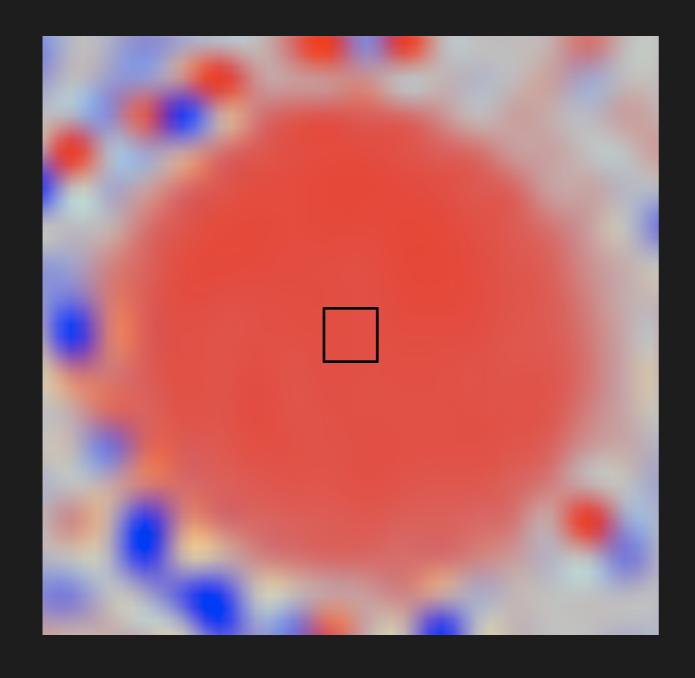
In-flow enhancement

Spatial resolution

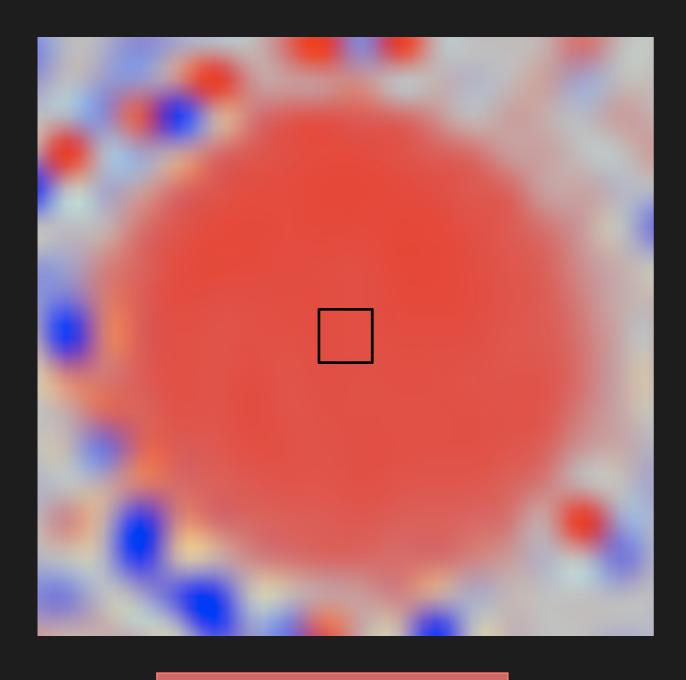






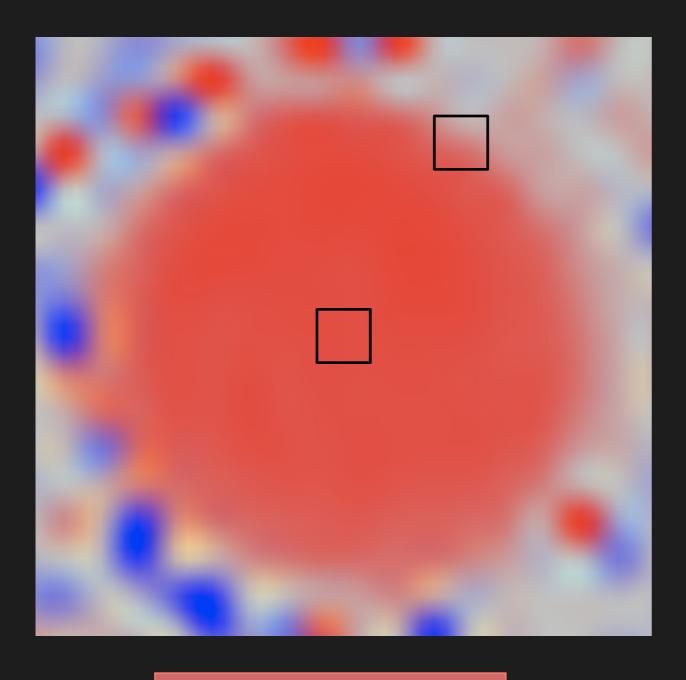






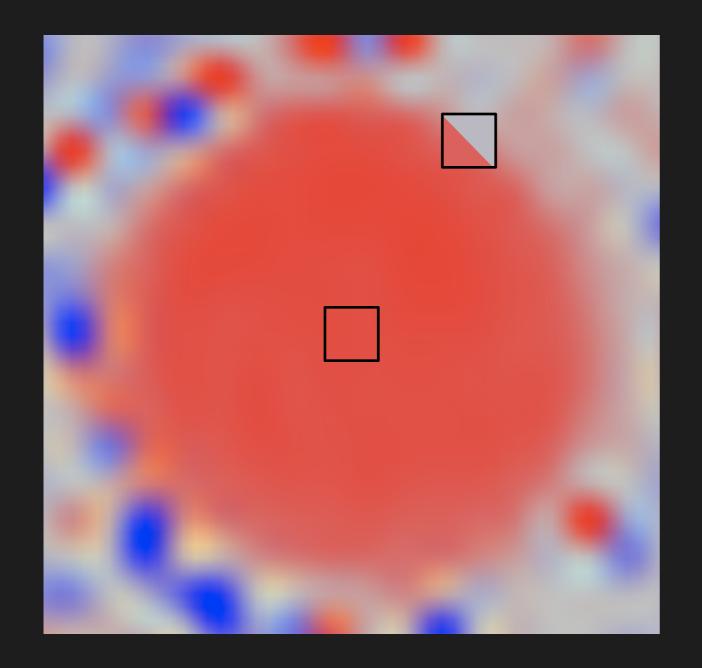
 $Q = V \times A$





 $Q = V \times A$

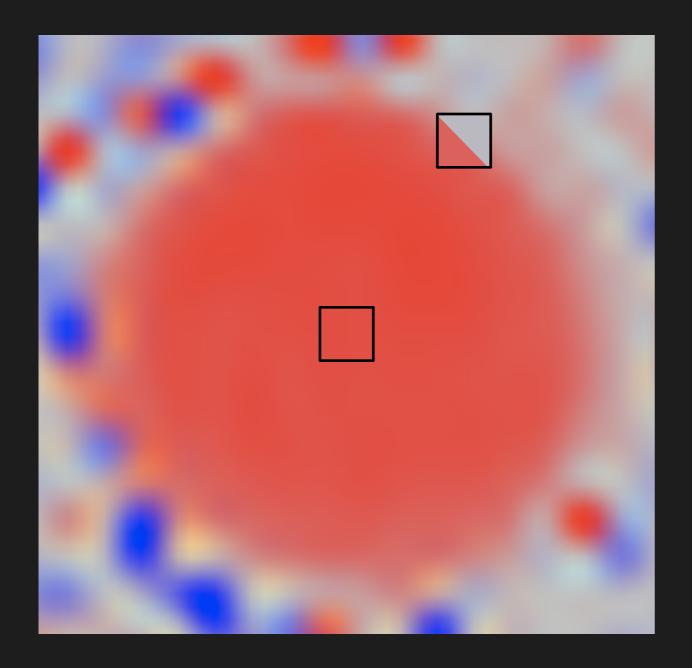




 $Q = V \times A$

Half pixel moving





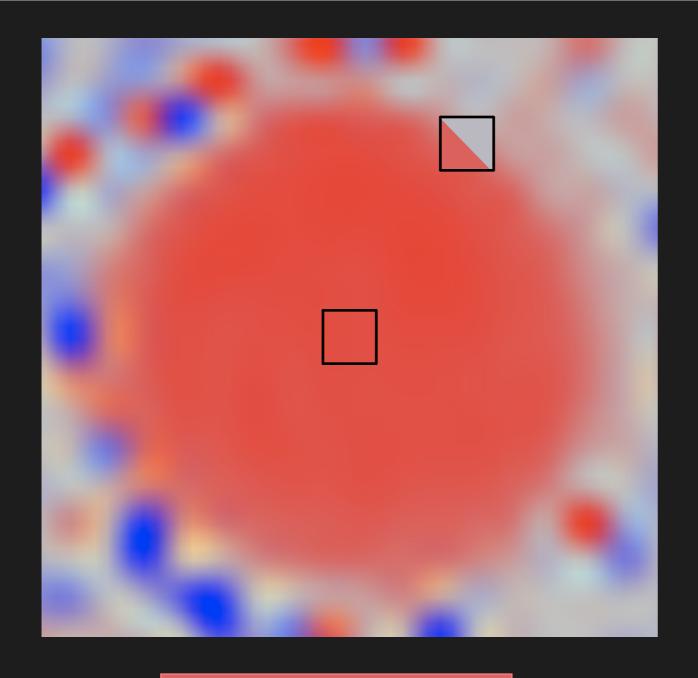
 $Q = V \times A$

Half pixel moving

Half pixel stationary

Whats the flow





Whats the flow

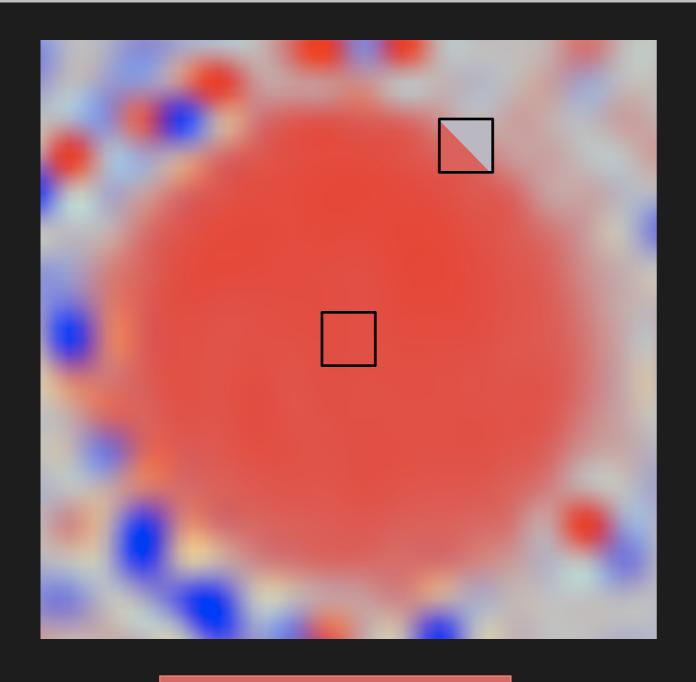


Simple average

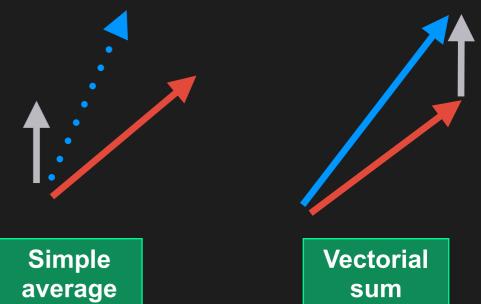
 $Q = V \times A$

Half pixel moving





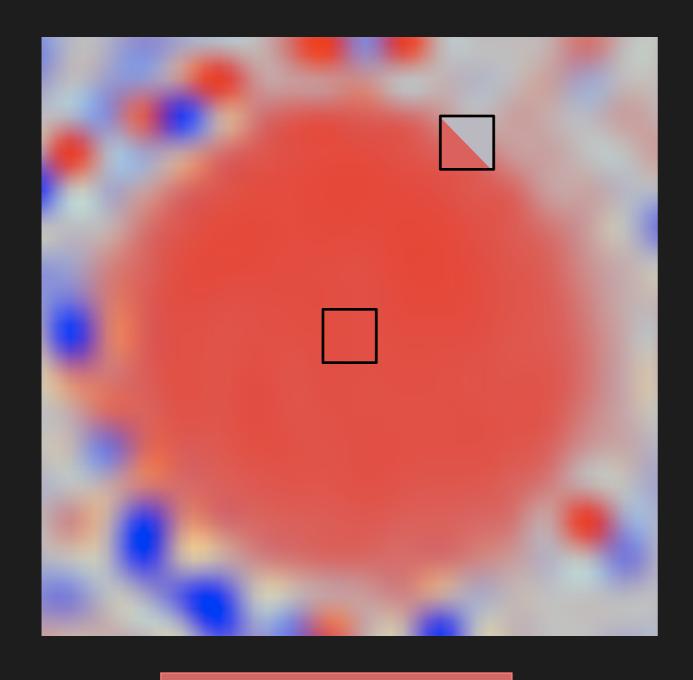
Whats the flow



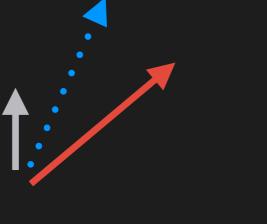
 $Q = V \times A$

Half pixel moving



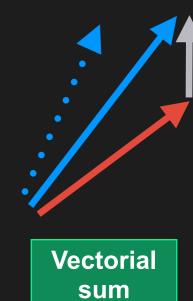


Whats the flow



Simple

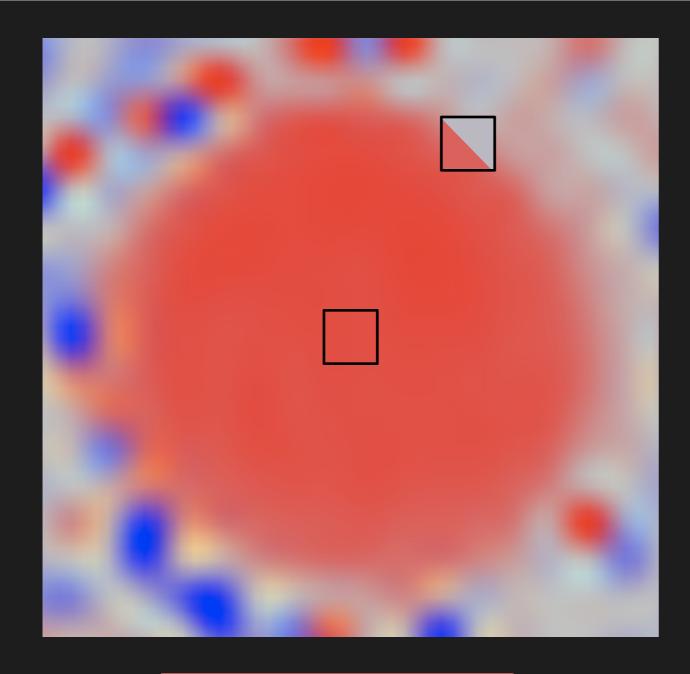
average



 $Q = V \times A$

Half pixel moving



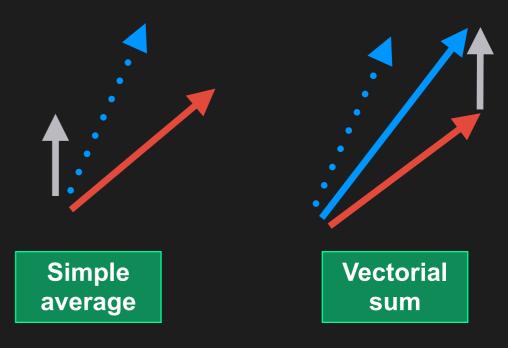


 $Q = V \times A$

Half pixel moving

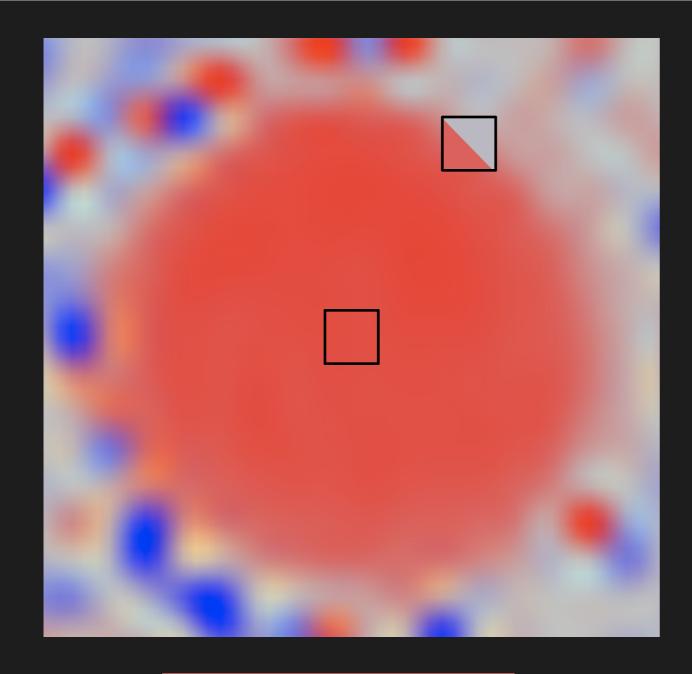
Half pixel stationary





Edge pixels



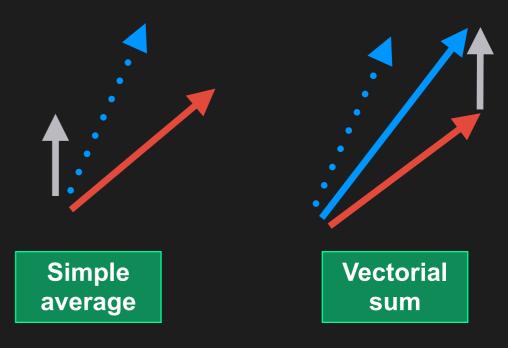


 $Q = V \times A$

Half pixel moving

Half pixel stationary

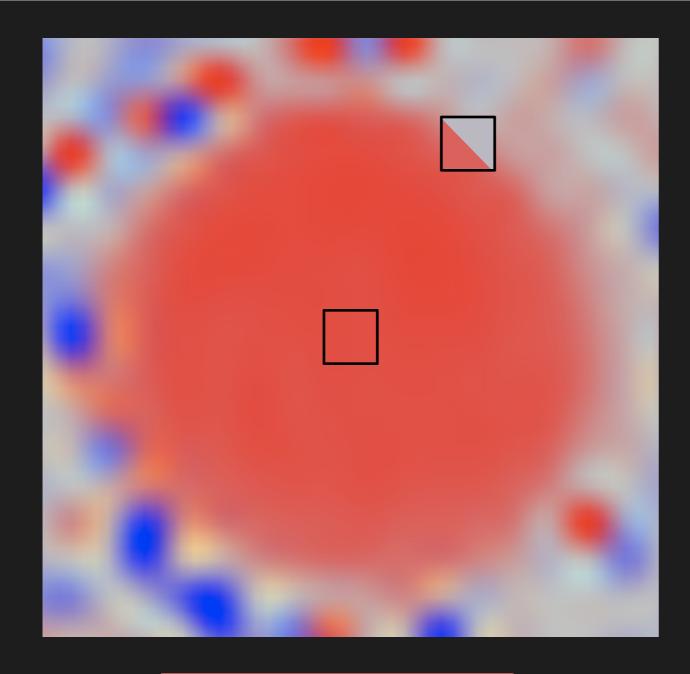




Edge pixels

Overestimate flow



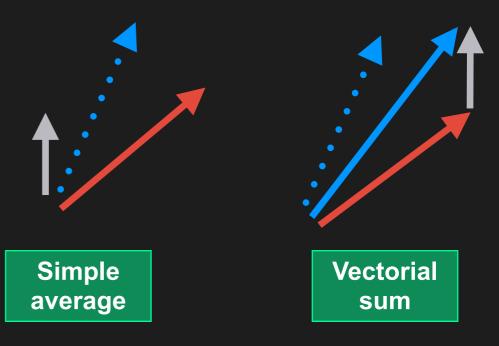


 $Q = V \times A$

Half pixel moving

Half pixel stationary

Whats the flow

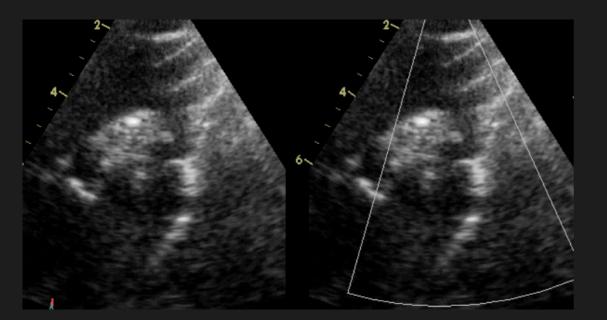


Edge pixels

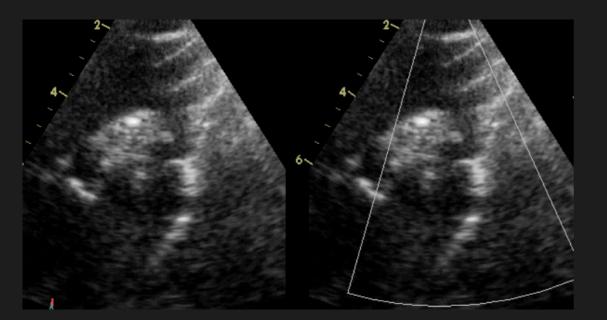
Overestimate flow

16 pixels minimum

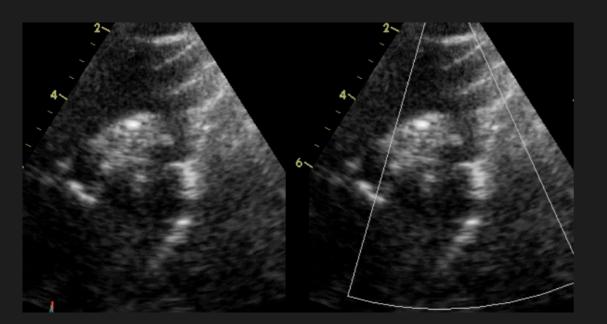


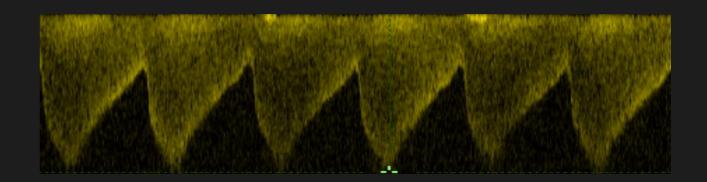






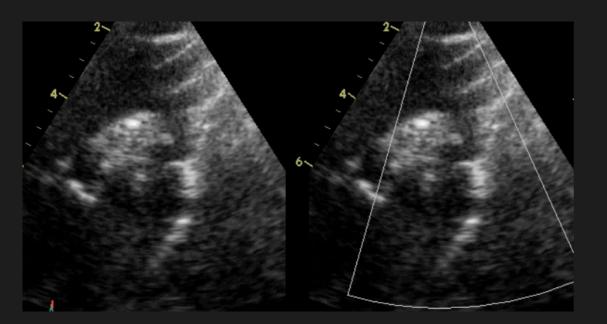


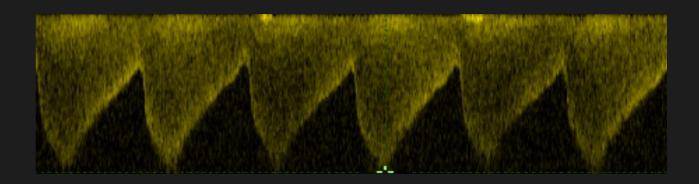




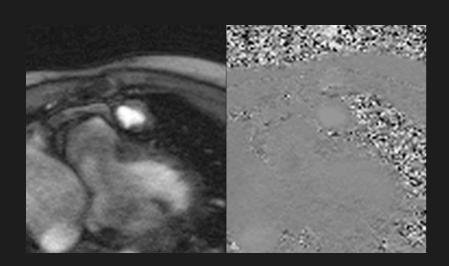
Doppler Reference



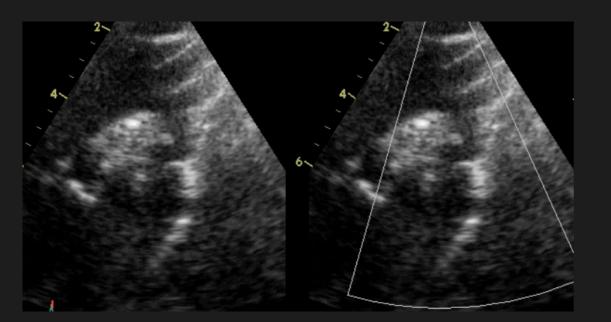


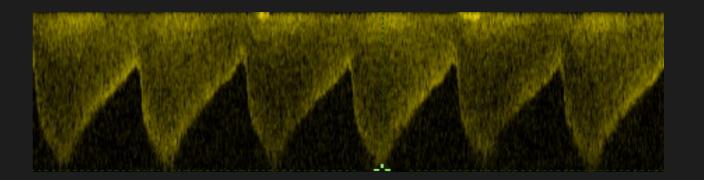


Doppler Reference

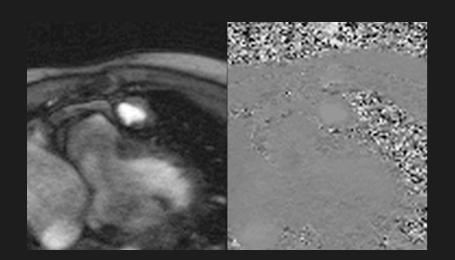


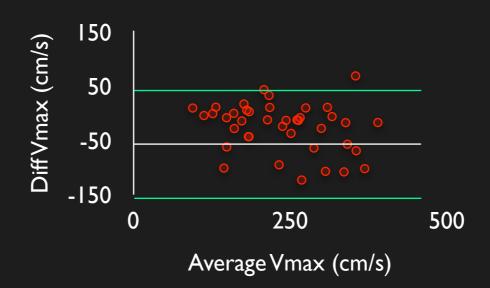






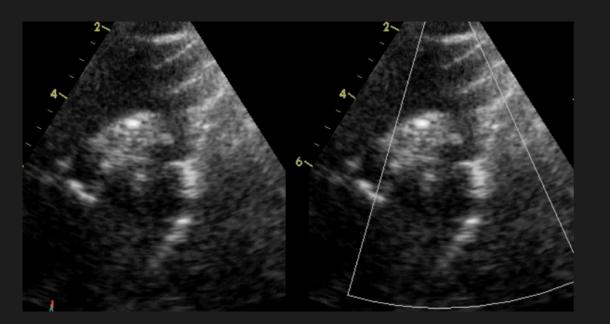
Doppler Reference

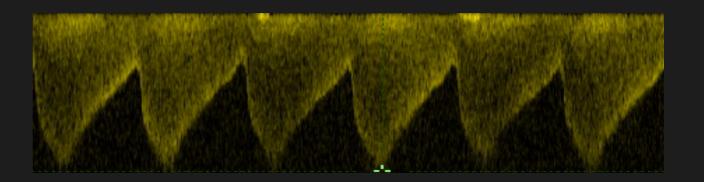




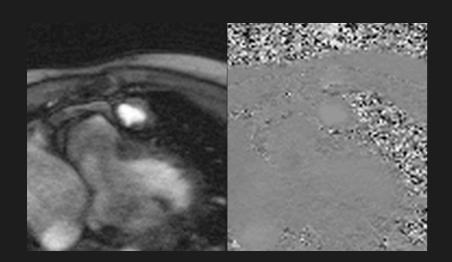
Bias 0.4m/s

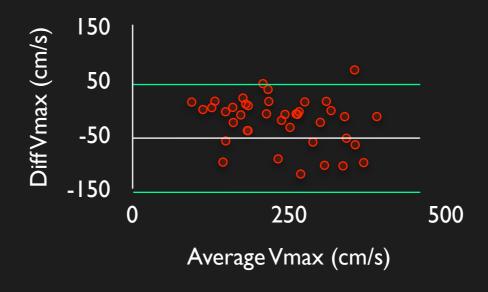




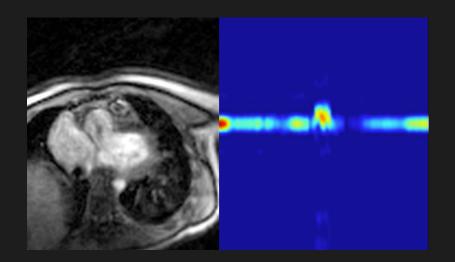


Doppler Reference

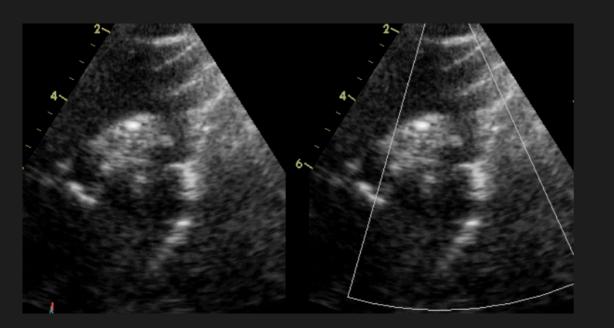


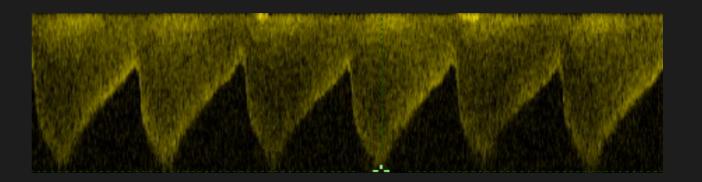


Bias 0.4m/s

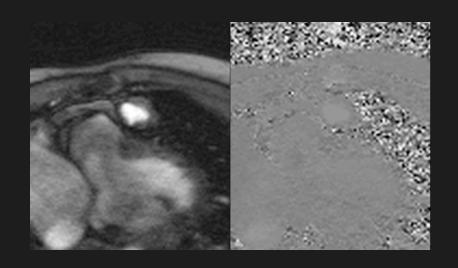


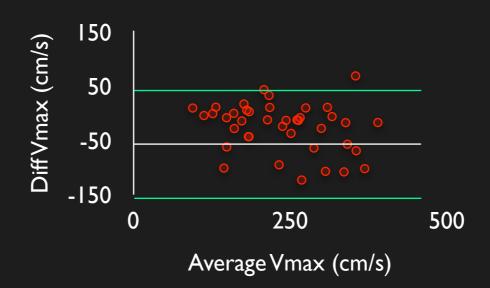




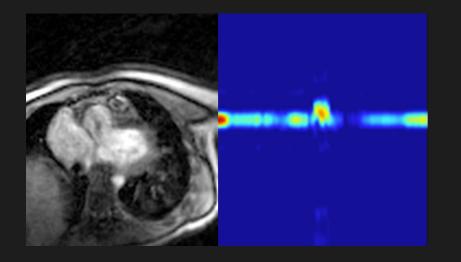


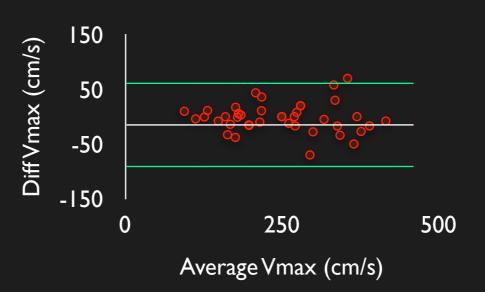
Doppler Reference





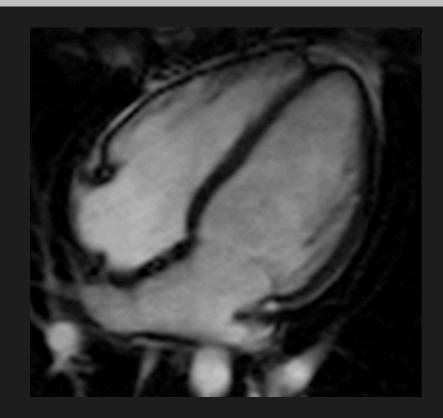
Bias 0.4m/s



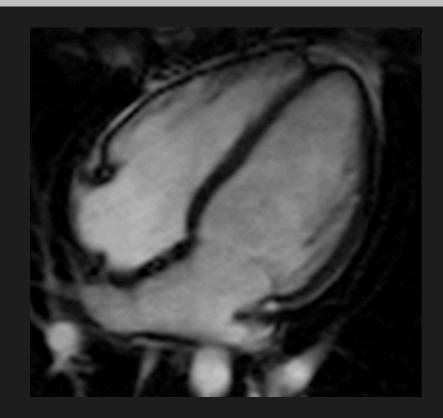


No bias

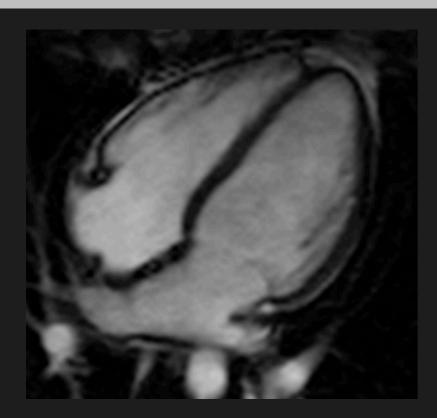






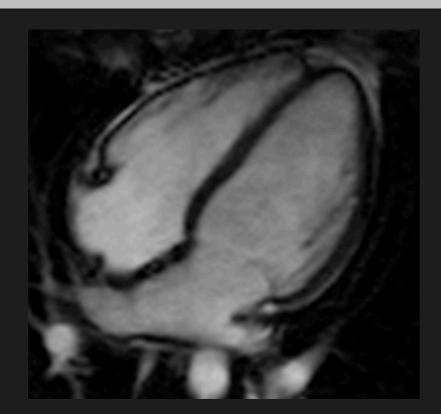






Type of GRE

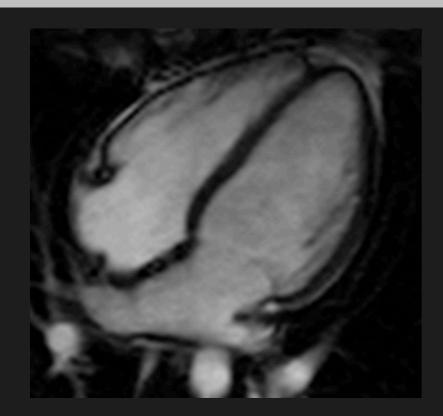




Type of GRE

Flow indépendant



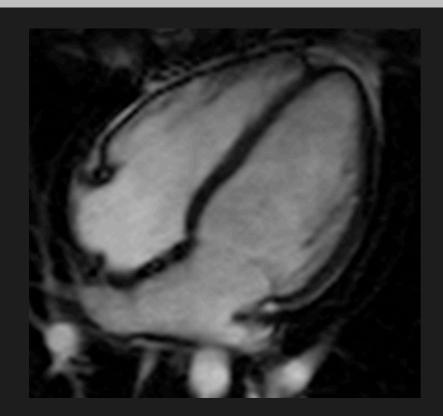


Type of GRE

Flow indépendant

High contrast





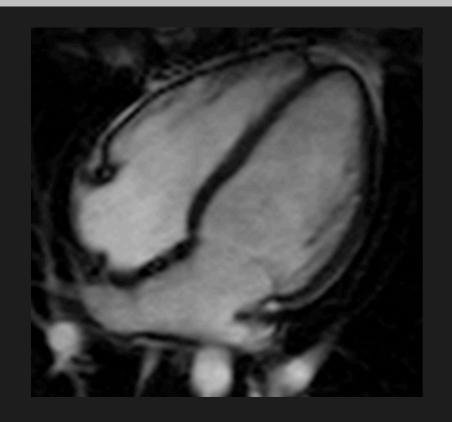
Type of GRE

Flow indépendant

High contrast

Work horse



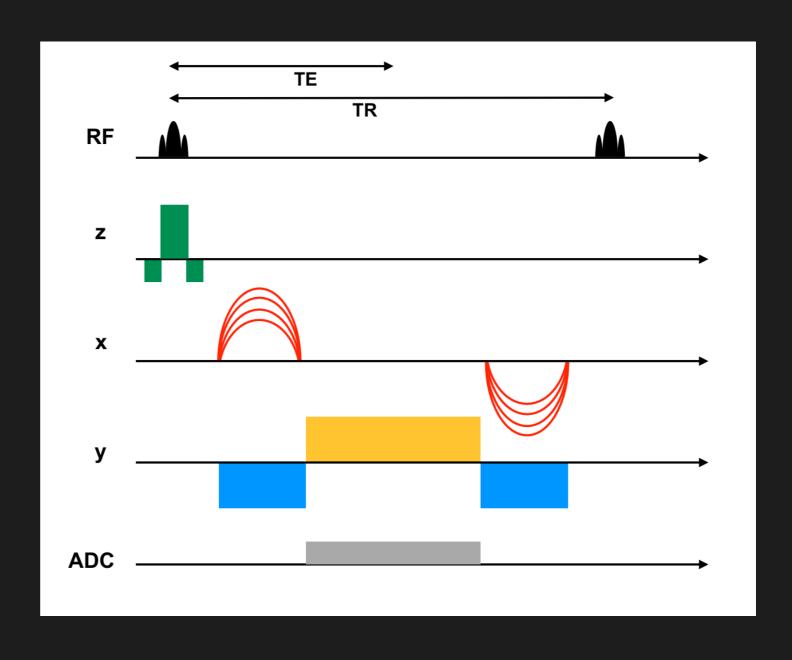


Type of GRE

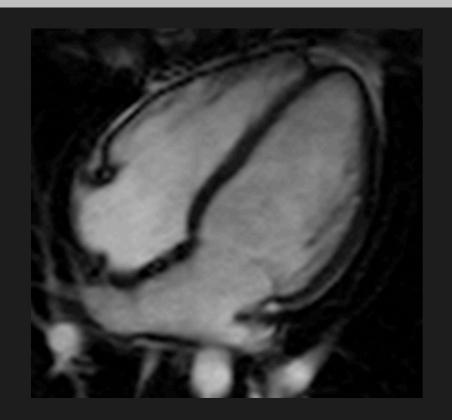
Flow indépendant

High contrast

Work horse





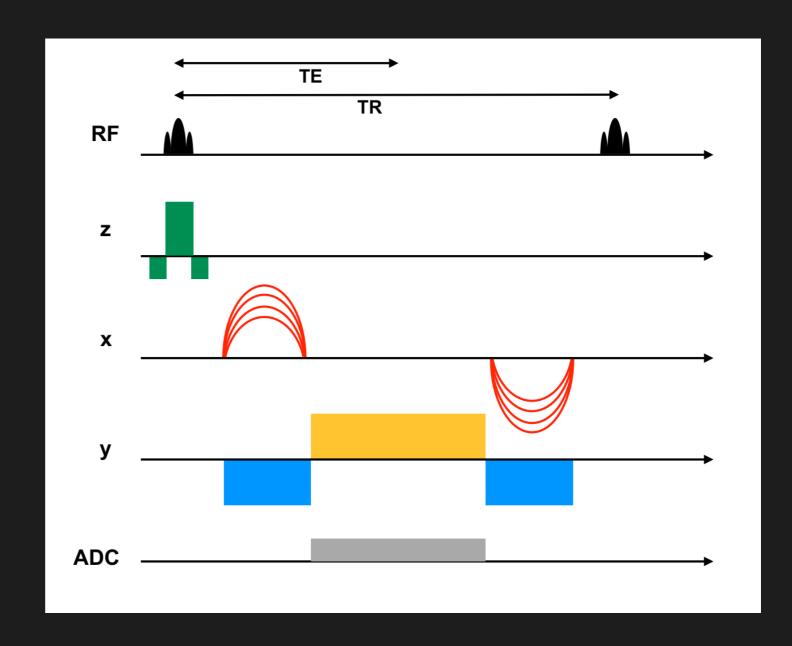


Type of GRE

Flow indépendant

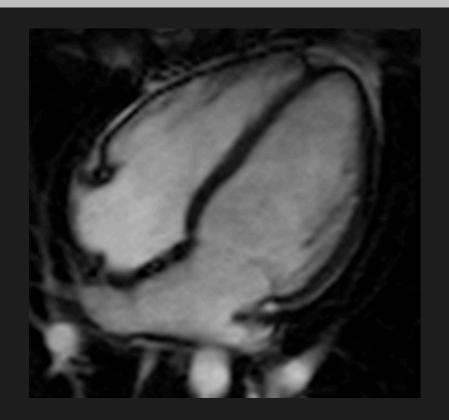
High contrast

Work horse



Gradients balanced



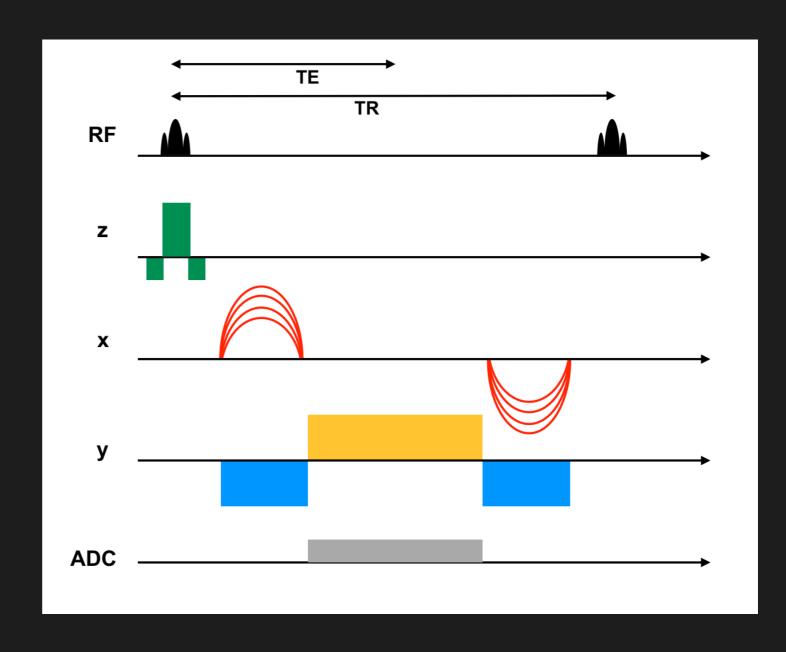


Type of GRE

Flow indépendant

High contrast

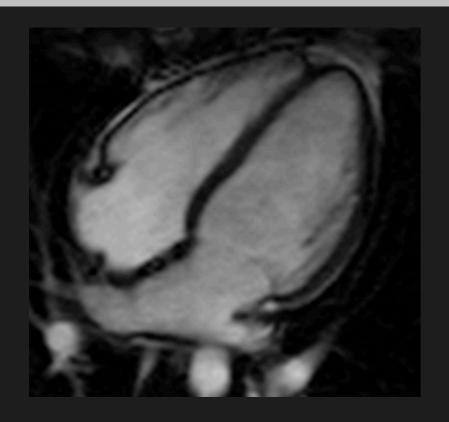
Work horse



Gradients balanced

Flipping magnetisation



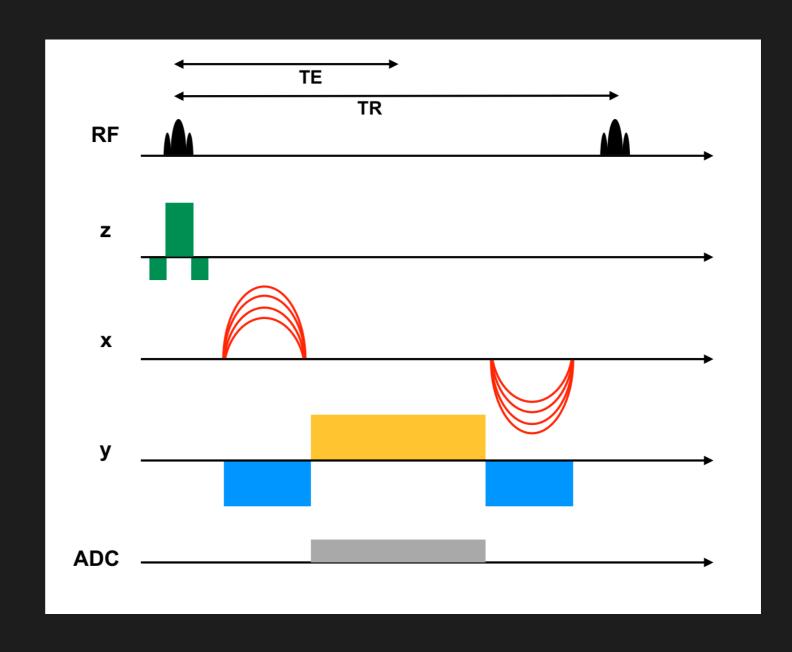


Type of GRE

Flow indépendant

High contrast

Work horse



Gradients balanced

Flipping magnetisation

T2 weighted not T2*





Sensitive to off resonance



Sensitive to off resonance

Magnetic field inhomogeneity



Sensitive to off resonance

Magnetic field inhomogeneity

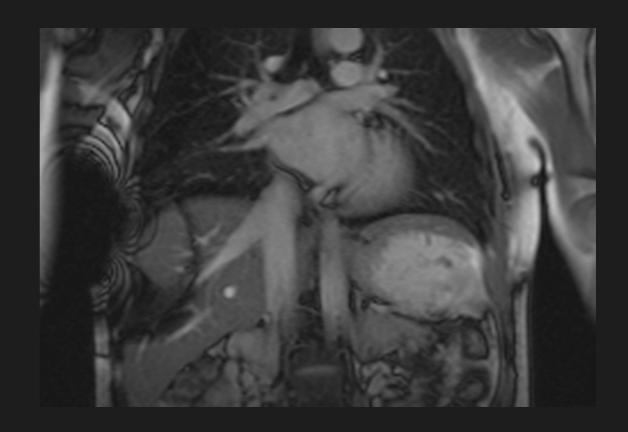
Time is a factor = TR



Sensitive to off resonance

Magnetic field inhomogeneity

Time is a factor = TR

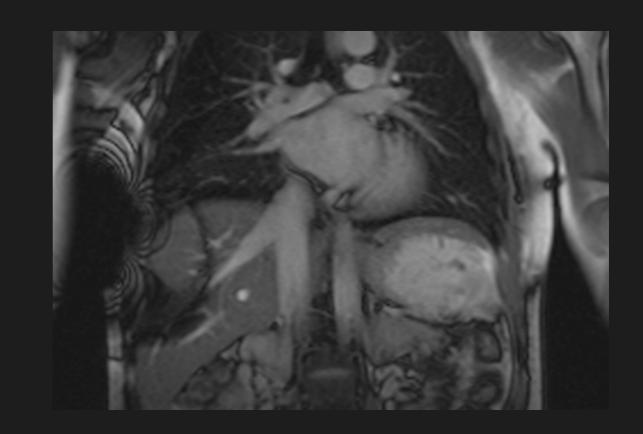


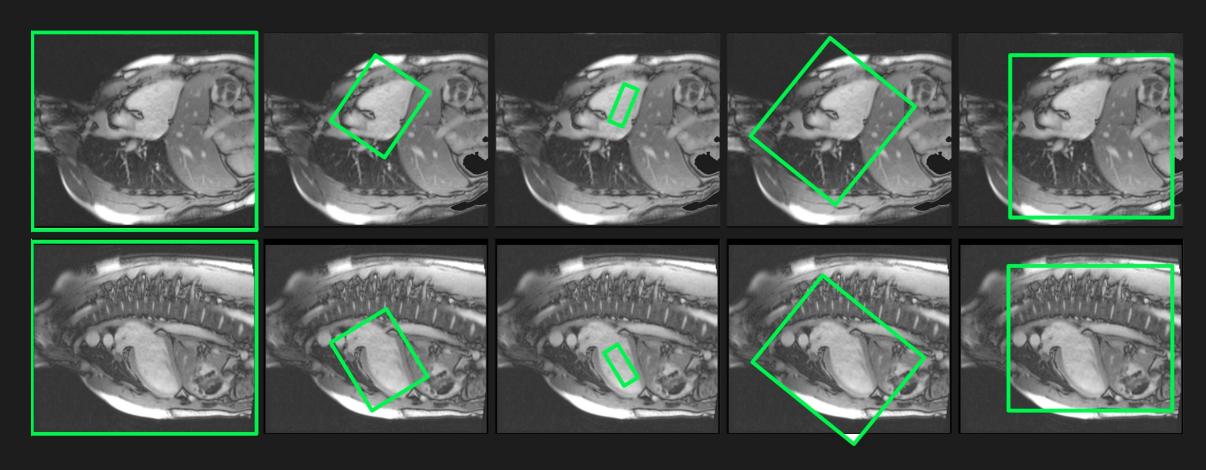


Sensitive to off resonance

Magnetic field inhomogeneity

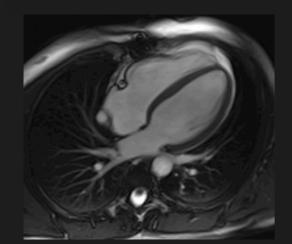
Time is a factor = TR

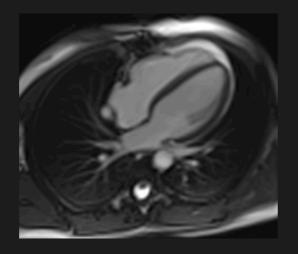




Sharp edges - spatial resolution

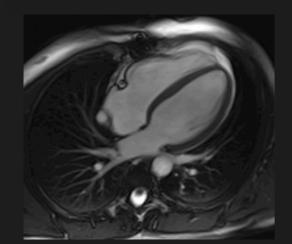


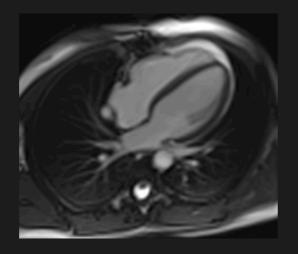




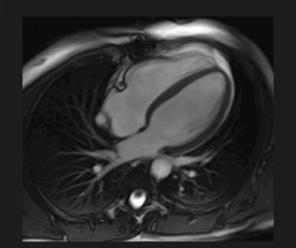
Sharp edges - spatial resolution

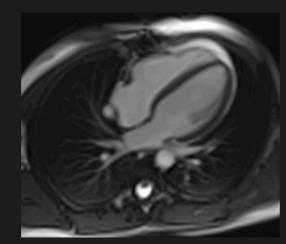






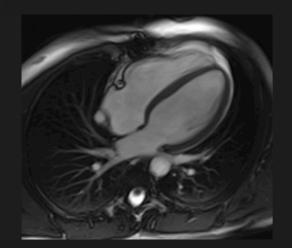






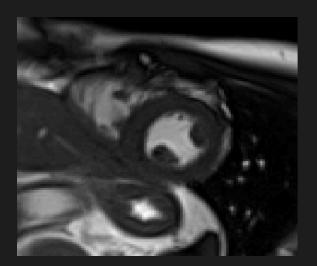
Does it effect volumes



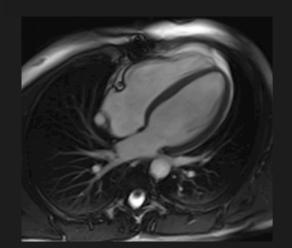


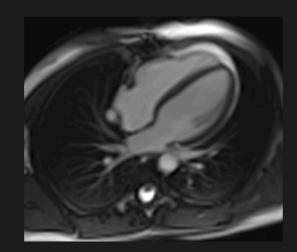


Does it effect volumes

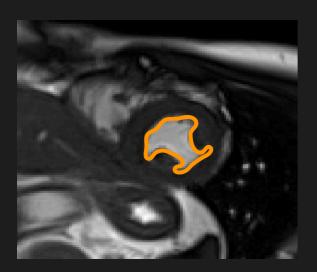




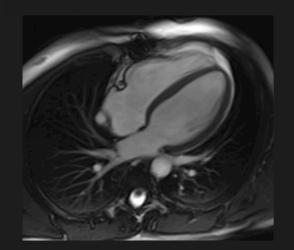


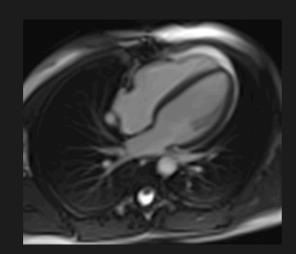


Does it effect volumes

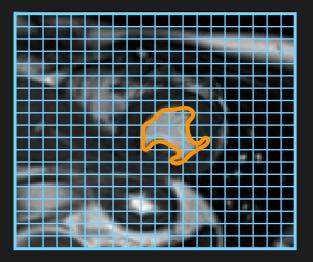




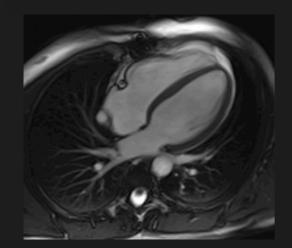


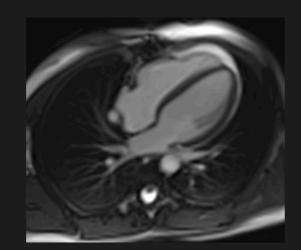


Does it effect volumes

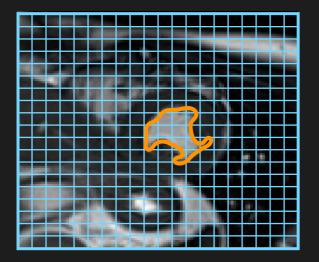


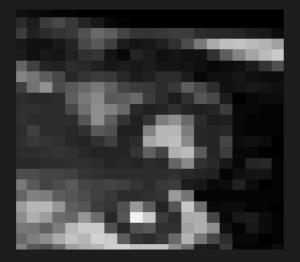




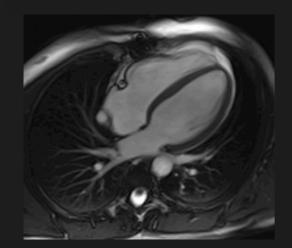


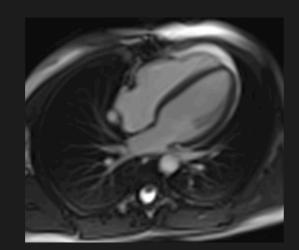
Does it effect volumes



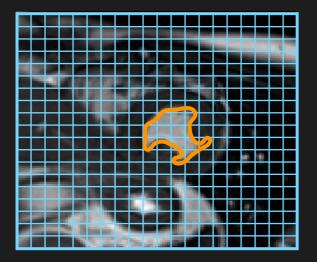


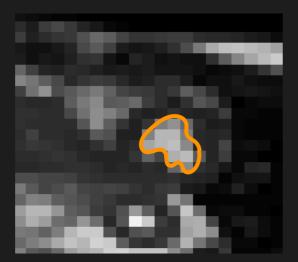




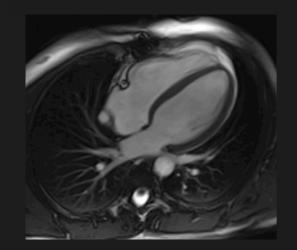


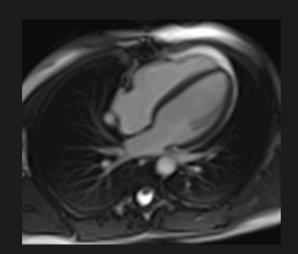
Does it effect volumes



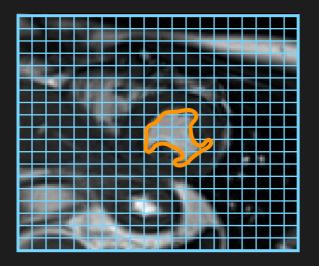








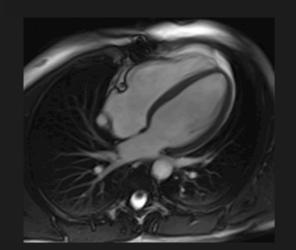
Does it effect volumes

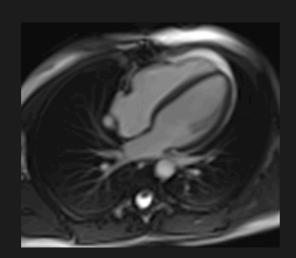




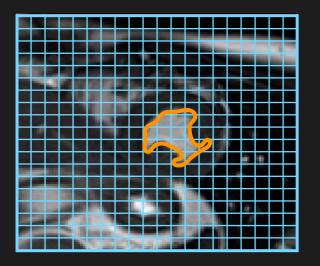
Error - segmentation

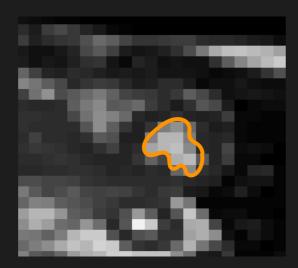






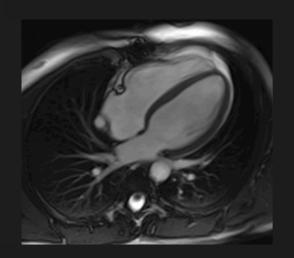
Does it effect volumes

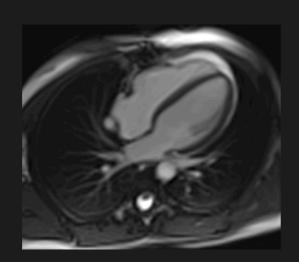


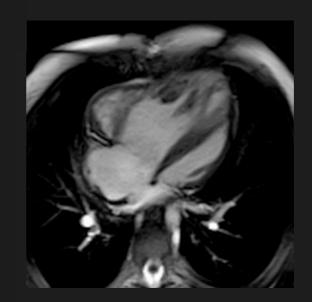


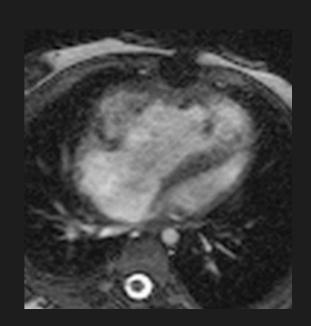
Error - segmentation



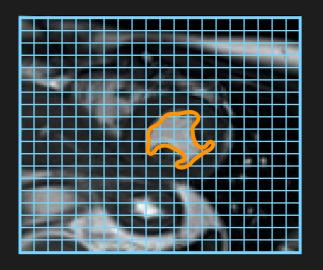


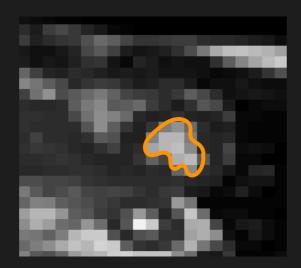






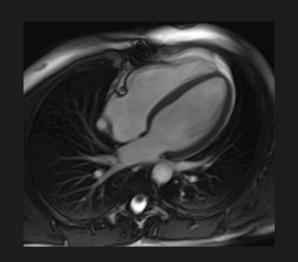
Does it effect volumes

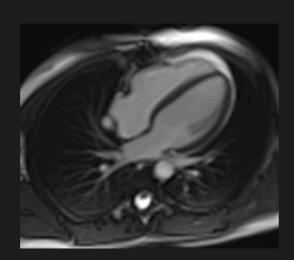


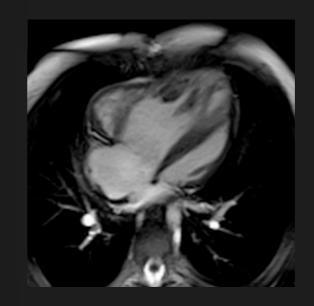


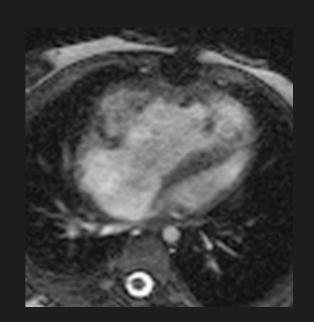
Error - segmentation





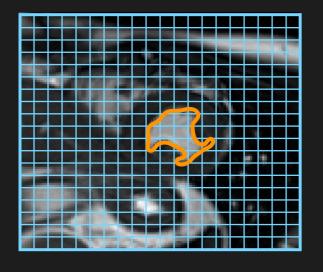


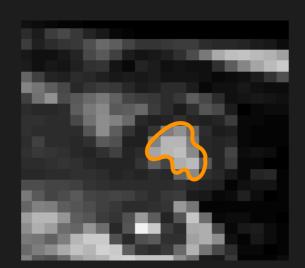




Does it effect volumes

Low Res

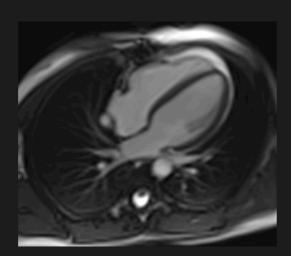


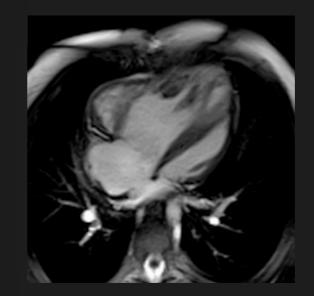


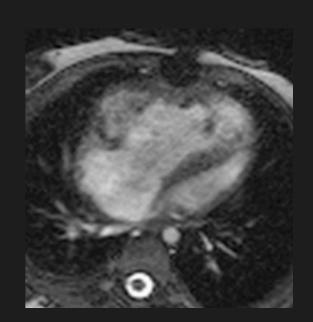
Error - segmentation







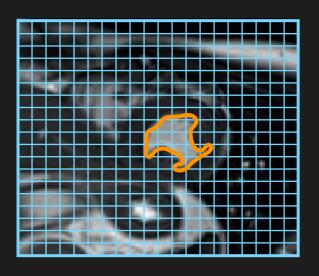


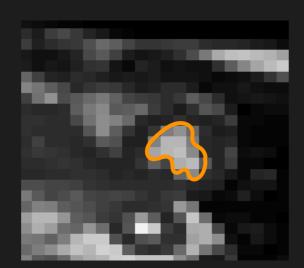


Does it effect volumes

Low Res

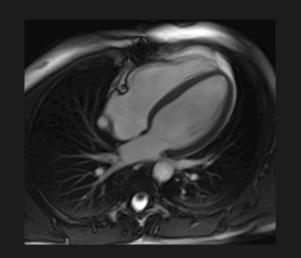
High Res

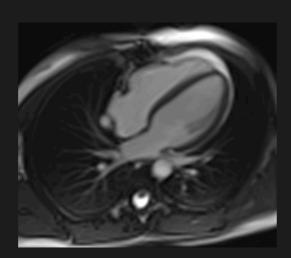


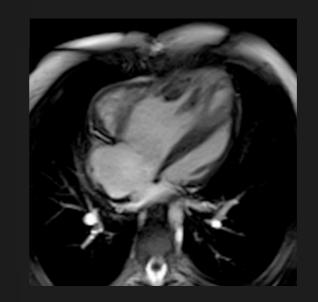


Error - segmentation







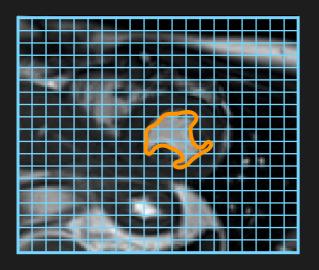


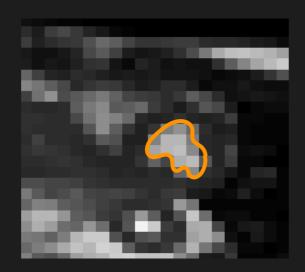


Does it effect volumes

Low Res

High Res

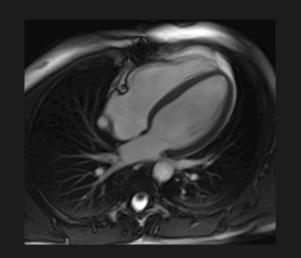


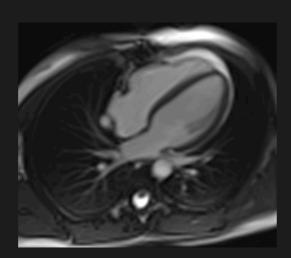


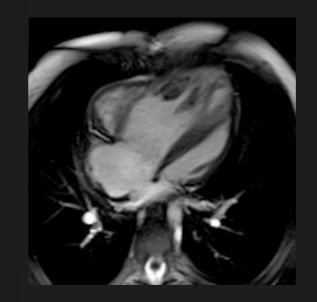
Low SNR

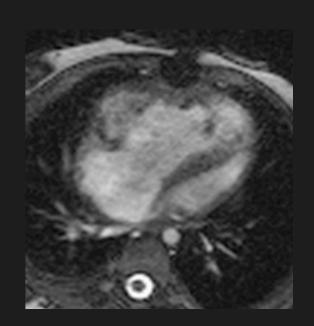
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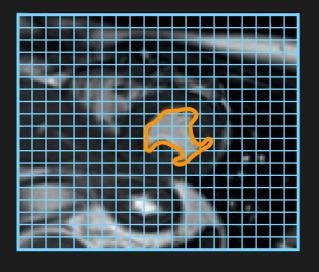


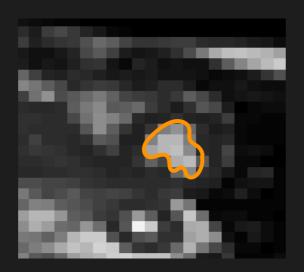


Does it effect volumes

Low Res

High Res



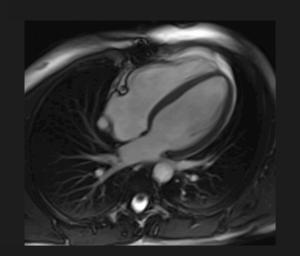


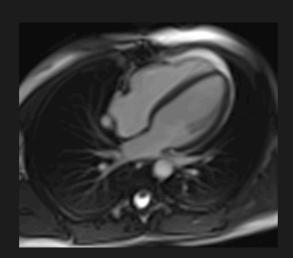
Low SNR

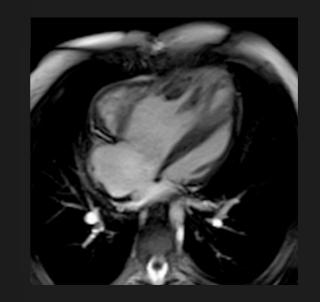
Long TR's - dark band

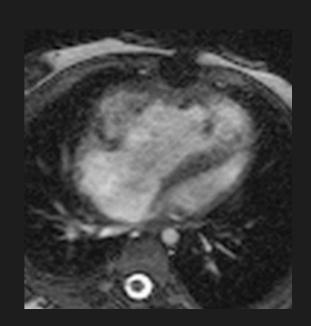
Error - segmentation







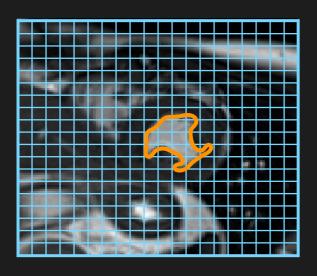


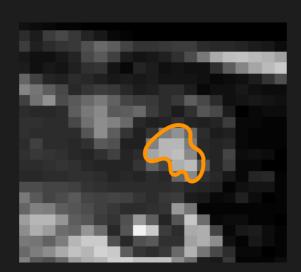


Does it effect volumes

Low Res

High Res





Low SNR

Long TR's - dark band

1.2 - 2.0mm

Error - segmentation

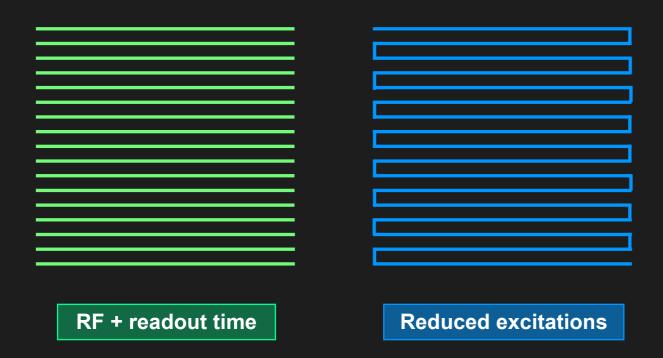






RF + readout time





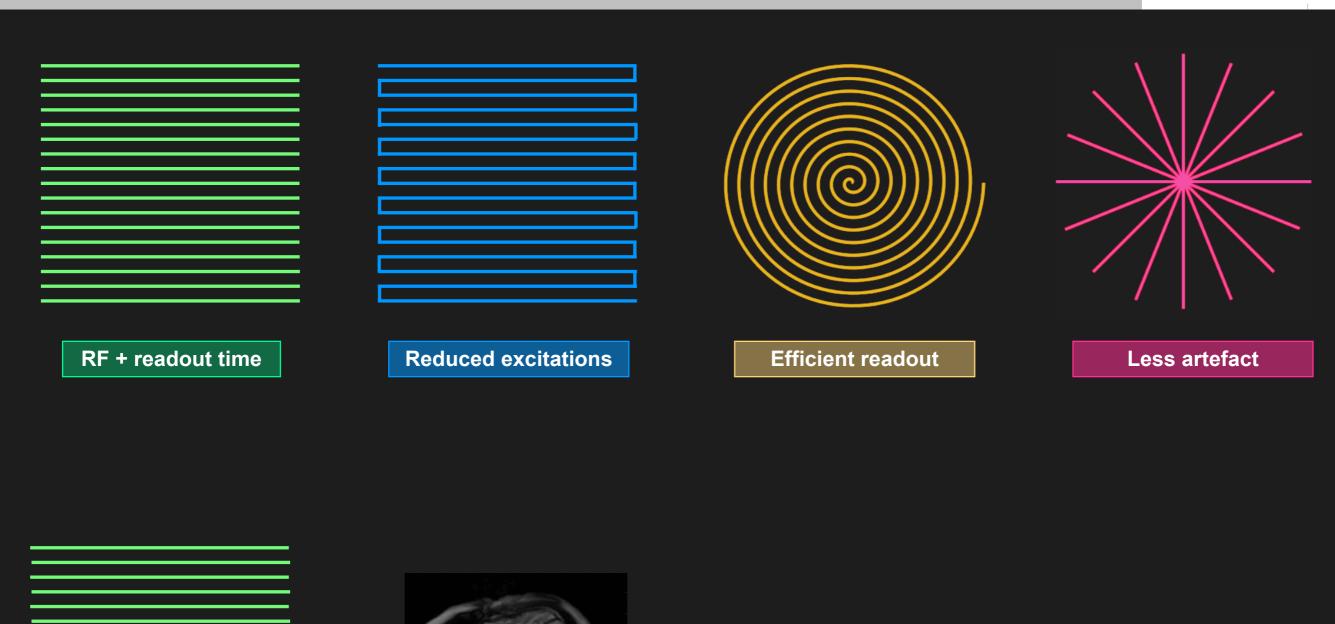




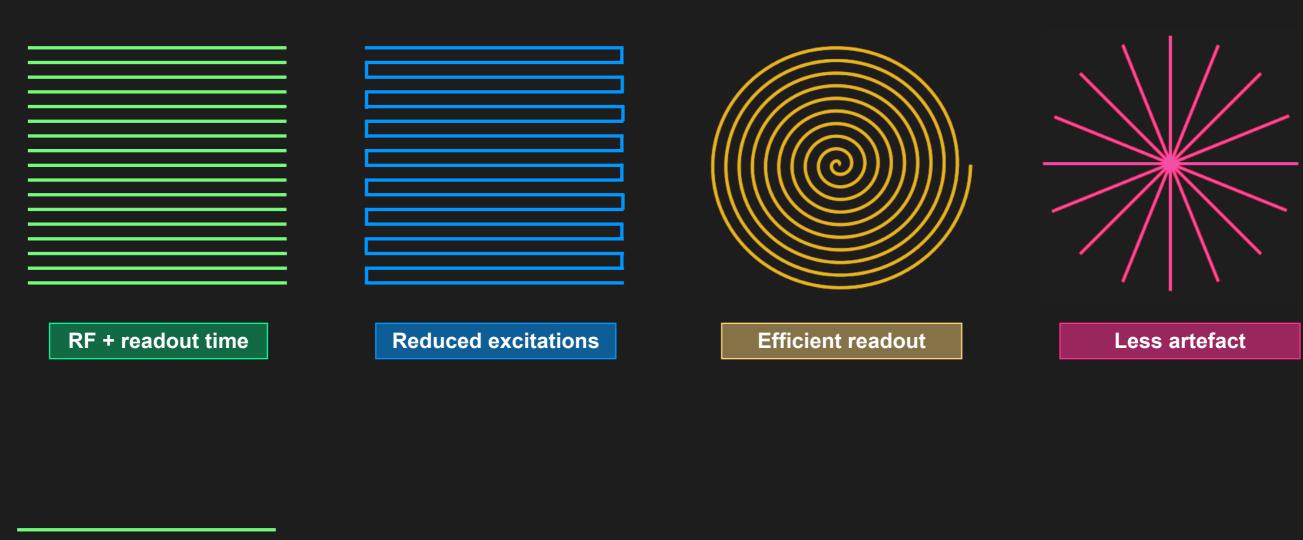


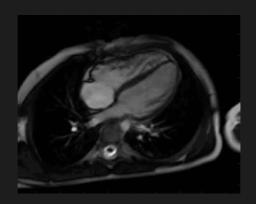




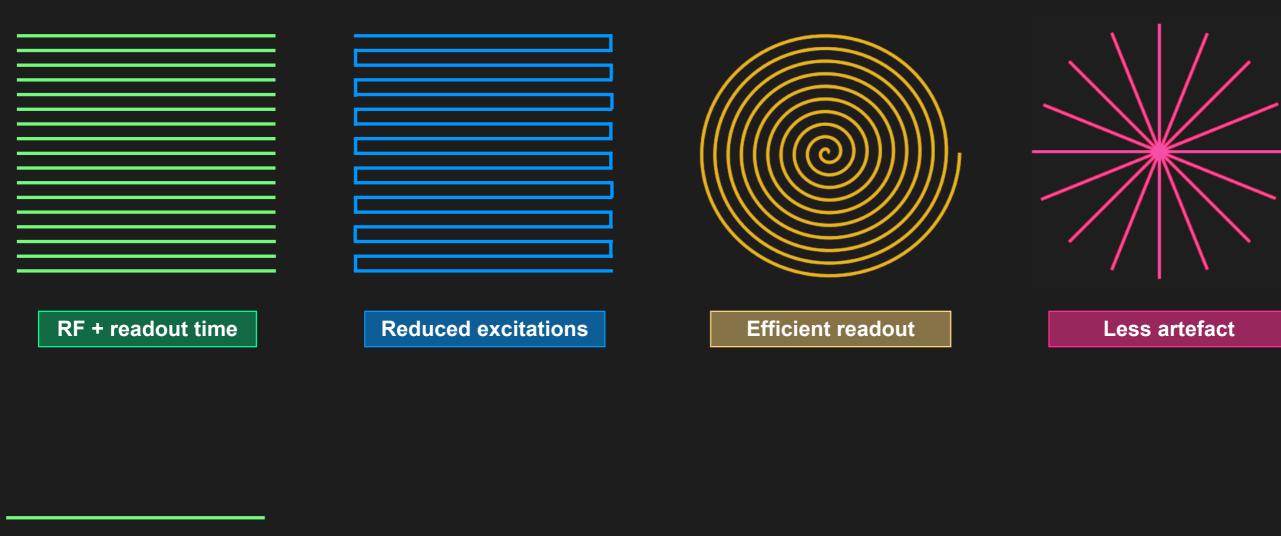


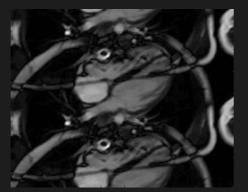




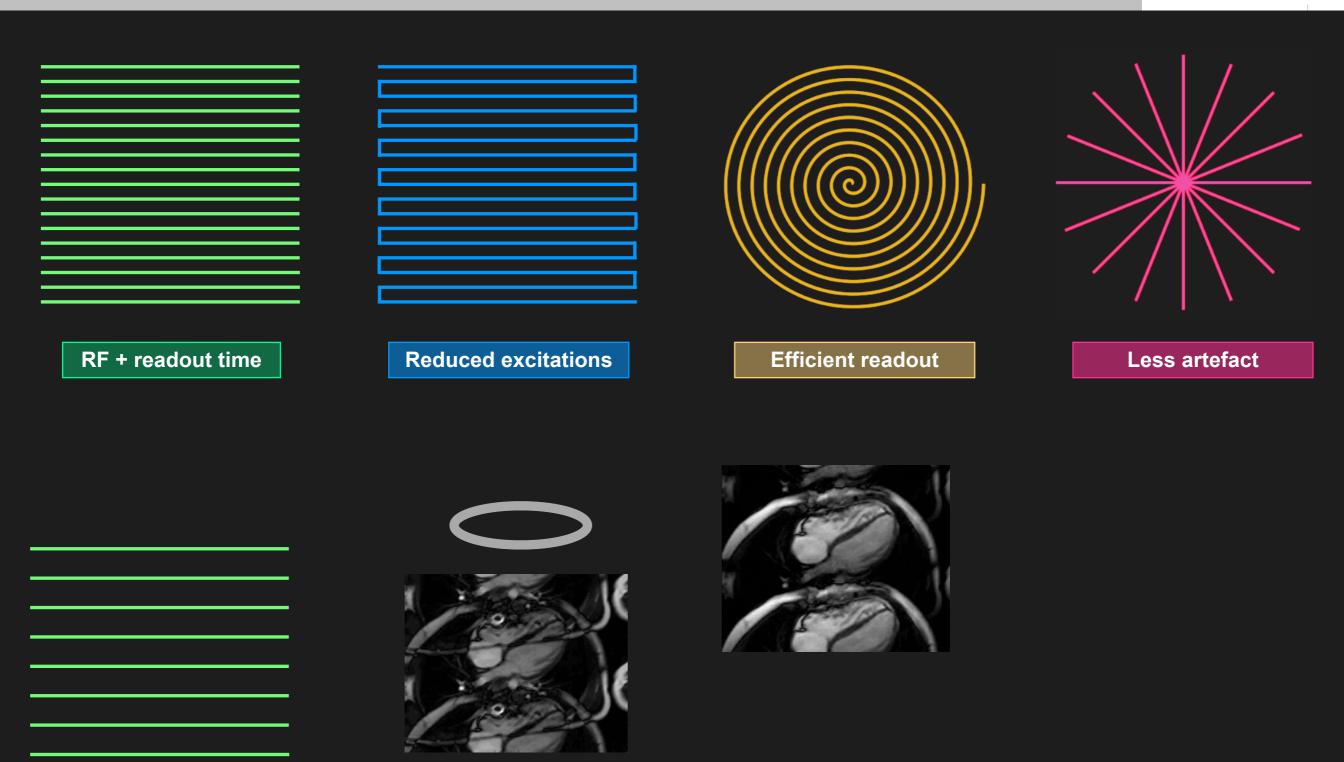














Less artefact

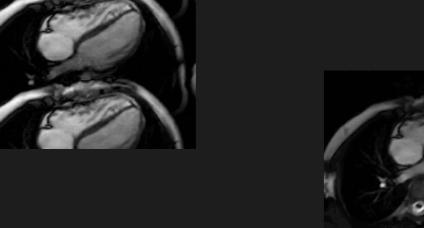
RF + readout time Reduced excitations **Efficient readout**

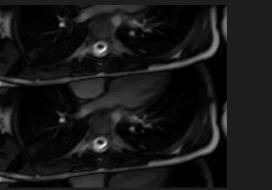


RF + readout time **Reduced excitations**















MRI physics



Takes time



MRI physics



Ask someone



Takes time



MRI physics



